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# abstracts book

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On behalf of the Organizing Committee, we take great pleasure in welcoming you to Barcelona (Spain) for the NanoBio&Med2019 International Conference.

This event, after successful editions organized within ImagineNano in Bilbao 2011 & 2013, and in Barcelona in 2014, 2015, 2016, 2017 & 2018, is going to present the most recent international developments in the field of Nanobiotechnology and Nanomedicine and will provide a platform for multidisciplinary communication, new cooperations and projects to participants from both science and industry. Emerging and future trends of the converging fields of Nanotechnology, Biotechnology and Medicine will discussed among industry, academia. be governmental and non-governmental institutions. NanoBio&Med2019 will be the perfect place to get a complete overview into the state of the art in those fields and also to learn about the research carried out and the latest results. The discussion in recent advances, difficulties and breakthroughs will be at his higher level.

As in previous editions, an industrial forum will be organized to promote constructive dialogue between business and public leaders and put specific emphasis on the technologies and applications in the nanoBioMed sector.

We are indebted to the following Companies and Scientific Institutions for their support: Institute for Bioengineering of Catalonia (IBEC), NANOMED Spain and American Elements.

We would also like to thank the following entities for their participation as exhibitors: Mecwins and the Distributed Biomedical Imaging Network (ReDIB).

In addition, thanks must be given to the staff of all the organising institutions whose hard work has helped planning this conference.

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# Vesicle chemotaxis at the nanoscale: principles and applications.

#### Giuseppe Battaglia<sup>1,2,3</sup>

<sup>1</sup>Department of Chemistry, Institute of Physics of Living Systems, University College London, 20 Gordon Street, London WC1H 0AJ, United Kingdom <sup>2</sup>Institute for Bioengineering of Catalonia (IBEC), The Barcelona Institute of Science and Technology, Baldiri Reixac 10-12, 08028 Barcelona, Spain <sup>3</sup>Catalan Institution for Research and Advanced Studies (ICREA), Passeig Lluís Companys 23, 08010 Barcelona, Spain

G.battaglia@ucl.ac.uk (Arial 9)

#### Abstract

Directional locomotion or taxis is possibly one of the most important evolutionary milestones, as it has enabled many living organisms to outperform their non-motile competitors [1]. In particular, chemotaxis (i.e. the movement of organisms either toward or away from specific chemicals) is the most common strategy adopted by many unicellular organisms to gather nutrients, escape toxins and help coordinate formation of colonies. Recently, we demonstrated that chemotaxis can be achieved by creating a nanoscopic vesicle loaded with enzymes, whose membrane have an asymmetric distribution of permeable domains [2]. When placed in the presence of a chemical gradient that act as substrate for the enzyme, the asymmetric distribution of flow across the vesicle membrane create a biased slip velocity around the vesicles and a consequent propulsion.

This, in turn, allows the vesicles to move chemotactically toward higher concentration of the substrate allowing long-ranged targeted delivery. Here, I will expand this concept using uniquely biological molecules with the final aim to demonstrate that a minimal organization of biomolecules can create the conditions for complex behavior such as chemotaxis. I will briefly present the physics associated with chemical gradient and how these create convective drifts and how these depend on both density gradient as well as diffusophoresis process associated with chemical interaction with wall surfaces.

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#### PHYSICAL PROPERTIES OF PARTICLES CAN CONTROL CELL SPECIFICITY

#### Brill-Karniely Y., Dror, D., Benny O.

Institute for Drug Research, School of Pharmacy, Faculty of Medicine, The Hebrew University, Jerusalem, Israel

ofrab@ekmd.huji.ac.il

#### Abstract

Growing evidence shows correlation between cancer aggressiveness and the mechanical properties of tumor cells. For many cancer diseases it was found that the deformability of the cells is higher in cancer compared to normal cells, and further raises with the degree of cell malignancy.

The goal of our multidisciplinary research is to investigate how physical properties of particles affect their internalization into non-cancer and cancer cells of varying malignancy potential, from the same origin. Such insight can promote specificity in uptake of drug delivery systems and can potentially be applied in diagnostic schemes. For that aim we used inert rigid colloids of different sizes, as well as nano particles of varying rigidity. Uptake of these particles was tested in non-cancer and cancer cells, including cells of increasing malignant potential. A wide range of biological and physical schemes was used and mechanistic insights were provided by a physical model.

A microfluidic based methodology to produce highly controlled nanoparticles was developed (1) followed by cell assays. We found that flexible particles are less internalized into the cells due to increased contact area that requires massive cell deformation in their engulfment (2).

A non-monotonic dependence on colloid size was found, explained by the energetic interplay between adhesion and cancer cell deformation. Importantly, uptake capacity of colloids was significantly higher in cancer compared to non-cancer originated cell lines, and also higher the more invasive the cancer cells were. The phagocytic capability of cells was found to correlate with the malignancy potential as well as with the mechanical deformability of the cells. Our study provides new mechanistic insights related to cancer progression that can potentially be applied in the rational design of drug delivery systems.

#### References

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#### **Figures**



**Fig. 1.** Example of mechanical tuned particulate system, Illustration of soft ("wet") polymeric micelles compared to semi-solid stiffer ones.



**Fig. 2.** An example of highly tunbnable polymer particles produced by a microfluidic device. A single chip can produce nano to micro range particles.



Fig. 3. Physicalmodel. **A**. A scheme of the model geometry, with definition of the flattening state, $\vartheta$ , and the contact area, a. **B**. Free energy plots as a function of  $\vartheta$  and a for different values of the rim constants,  $\kappa r$ , with  $\epsilon \frac{1}{4}$  0:1 kBT. nm2 and c=20kBT.

#### Paper-based nanobiosensors: diagnostics going simple

#### Arben Merkoçi

<sup>1</sup>Catalan Institute of Nanoscience and Nanotechnology (ICN2), CSIC and The Barcelona Institute of Science and Technology, Campus UAB, Bellaterra, 08193 Barcelona, Spain. <sup>2</sup>ICREA - Institucio Catalana de Recerca i Estudis

Avançats, 08010 Barcelona, Spain

arben.merkoci@icn2.cat

#### Abstract

Biosensors field is progressing rapidly and the demand for cost efficient platforms is the key factor for their success. Physical, chemical and mechanical properties of cellulose in both micro and nanofiberbased networks combined with their abundance in nature or easy to prepare and control procedures are making these materials of great interest while looking for cost-efficient and green alternatives for device production technologies. Both paper and nanopaper-based biosensors are emerging as a new class of devices with the objective to fulfil the "World Health Organization" requisites to be ASSURED: affordable, sensitive, specific, userfriendly, rapid and robust, equipment free and deliverable to end-users. How to design simple paper-based biosensor architectures? How to tune their analytical performance upon demand? How one can 'marriage' nanomaterials such as metallic nanoparticles, quantum dots and even graphene with paper and what is the benefit? How we can make these devices more robust, sensitive and with multiplexing capabilities? Can we bring these low cost and efficient devices to places with low resources, extreme conditions or even at our homes? Which are the perspectives to link these simple platforms and detection technologies with mobile phone communication? I will try to give responses to these questions through various interesting applications related to protein, DNA and even contaminants detection all of extreme importance for diagnostics, environment control, safety and security.

#### Creating a Bidirectional Bypass for Spinal Cord Injuries with Nanotechnology

#### Rodolfo Miranda<sup>1</sup>,

T. González, L. Pérez, J. Camarero, L. Mechin, E. L. Dolado, C. Serrano and L. Ballerini<sup>2</sup>

<sup>1</sup>IMDEA Nanociencia, Cantoblanco, Madrid, Spain <sup>2</sup> By-Axon Team

#### rodol fo.mir and at@imdea.org

After a Spinal Cord Injury (SCI), the communications between the brain and the spinal circuits that dictate movement are interrupted. Innovative equipment has been developed to help patients regain control of limbs. The current strategies to remediate SCI based on computer-brain interfaces [1, 2], however, require the use of bulky devices, not implantable and without sensorial feedback.

We aim at developing a new generation of magnetic sensors and electrodes based on nanotechnology for neural interfacing with improved sensitivity and low tissue disturbance thanks to their nanostructure. The nanodevices are suitable for chronic implantation. It will be focused on restoring the transmission of electrical signals in the injured SC, acting as a bi-directional local bypass.

I will first describe the nanofabrication and performance of high-resolution magnetic field sensors working at room temperature, based on anisotropic magnetoresistive (AMR) LSMO films epitaxially grown on vicinal substrates. Then I will report on the production of nanowire-coated electrodes for neural excitation by template-assisted electrochemical growth (metallic) or nanoimprint technology (conductive polymer).

Finally I will show real-time measurements of both the pharmacologically induced activity of neural cord slices and the subsequent actuation on neural cord slices.

#### References

- [1] E. Formento et al, Nature Neuroscience (2018)
- [2] F. Wagner et al, Nature 563 (2018) 65



**Figure 1.** Scheme of the active By-pass for neural reconnection including magnetic sensing and nanoelectrodes for neurostimulation.



**Figure 2.** Real time measurements of the activity of a neural cord slice. The data have been taken at room temperature without any magnetic shielding.

# Nanomagnets for biomedical applications: from spherical shapes to planar geometries

R. Morales<sup>1,2</sup>, B.Mora<sup>3</sup>, A. Perez-Valle<sup>4</sup>, C. Redondo<sup>3</sup>, M.D. Boyano<sup>5</sup>.

<sup>1</sup>Department of Physical-Chemistry & BCMaterials, University of the Basque Country UPV/EHU, 48940 Leioa, Spain

- <sup>2</sup>IKERBASQUE, Basque Foundation for Science, 48011 Bilbao, Spain
  - <sup>3</sup>Department of Physical-Chemistry, University of the

Basque Country UPV/EHU, 48940 Leioa, Spain

<sup>4</sup>Department of Cell Biology and Histology, University of

the Basque Country UPV/EHU, 48940 Leioa, Spain <sup>5</sup>Department of Cell Biology and Histology UPV/EHU, and Biocruces Health Research Institute 48903 Barakaldo, Spain

rafael.morales@ehu.eus

Magnetic nanomaterials have risen the expectation to develop novel biomedical applications. Their unique properties and physical effects under external fields have attracted their interest in several areas; among them, cell manipulation through the remote action, diagnosis through high sensitive magnetic sensors or contrast enhancement in magnetic resonance imaging, and therapy through the heating effect under high-frequency fields.[1, 2] Magnetic nanoparticles (MNP) are chemically synthesized in compact forms like nanocubes, nanowires, and more conventionally spherical shapes.[3, 4] These nanomagnets are in a superparamagnetic state to be suitable for medical applications. Therefore, their size must be smaller than few tens of nanometers.

On the contrary, magnetic nanostructures (MNS) are fabricated using lithography techniques.[5] This approach produces planar geometries like disks or ellipses (Figure 1). This planar shape confers them new properties for magnetic actuation. However, MNS do not present superparamagnetic behavior due to their dimensions around hundreds of nanometers. Consequently, they must be designed with special magnetic configurations to achieve the zero remanence required in biomedical applications.[6]

We will discuss these special configurations and cost-effective routes to fabricate suitable planar nanomagnets. Magnetic properties and toxicity studies *in-vitro* models of tumor cells will be presented. We will also state the expected advantages of MNS in novel diagnostics and therapeutic applications.

This work was supported by AEI-MINECO FIS2016-76058, UE FEDER "Una manera de hacer Europa", the European Union's Horizon 2020 research and innovation programme under the Marie Sklodowsks-Curie grant agreement No 734801, and the Basque government grant IT970-16, IT1162-19, and PIBA 2018-11.

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#### **Figures**



Figure 1. Magnetic nanostructures of NiFe fabricated by interference lithography

#### nanoBiomaterials for Neurology: one (powerful) tool, many applications

#### Ana Paula Pêgo<sup>1,2,3,4</sup>

 <sup>1</sup> INEB - Instituto de Engenharia Biomédica, Universidade do Porto, Portugal
 <sup>2</sup> i3S – Instituto de Investigação e Inovação em Saúde, Universidade do Porto, Portugal
 <sup>3</sup> ICBAS - Instituto de Ciências Biomédica Abel Salazar, Universidade do Porto, Portugal
 <sup>4</sup> FEUP - Faculdade de Engenharia, Universidade do Porto, Portugal

Nervous system problems are common and encompass a large spectrum of traumatic injuries, diseases or iatrogenic lesions. The poor regenerative capacity, particularly in the case of the central nervous system (CNS), cannot be attributed to an intrinsic inability of neurons to sprout and regrow after injury, as axons are able to regenerate in the presence of a permissive growth environment. One of the challenges facing the neuroscience field is the development of effective therapies that can enhance the regenerative capacity of the nervous system based on the advances achieved in basic research.

We have been dedicated to using nano-enabled solutions to the design of new therapeutic approaches based on biomaterials to promote neuroprotection and neuroregeneration. In this talk, two main strategies will be presented that represent two of the main lines of research of my group:

i) the design of biomaterial-based nanoparticles for targeted nucleic acid delivery to neurons [1];

ii) the design of bioactive hydrogels for neural stem cell delivery in the spinal cord[2].

Emphasis will also be given to the application of novel strategies proposed to assess the potential of the developed systems[3-5].

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#### Novel DNA-Based Molecules and Their Charge Transport Properties

#### Danny Porath,

Institute of Chemistry and Center for Nanoscience and Nanotechnology, The Hebrew University of Jerusalem, 91904 Israel

danny.porath@mail.huji.ac.il

#### Abstract

Charge transport through molecular structures is interesting both scientifically and technologically. To date, DNA is the only type of polymer that transports significant currents over distances of more than a few nanometers in individual molecules. Nevertheless and in spite of large efforts to elucidate the charge transport mechanism through DNA a satisfying characterization and mechanistic description has not been provided yet. For molecular electronics, DNA derivatives are by far more promising than native DNA due to their improved charge-transport properties.

In recent years we have invested great efforts to address the above issues. Measuring the charge transport in DNA was elusive due to great technical difficulties leading to various results. We recently devised an experiment in which double-stranded DNA is well positioned between metal electrodes. Electrical measurements give surprisingly high currents over 100 base-pairs (~30 nm) elevated from the surface. The temperature dependence indicates backbone-related band-like transport. In collaboration with the Kotlyar group, We were also able to synthesize and measure long (hundreds of nanometers) DNA-based derivatives that transport significant currents when deposited on hard substrates. Among the molecules, metal containing DNA, which is true metal-organic hybrid, a smooth and thin metal coated DNA and G-quadruplex DNA. Step by step we improve the synthesized constructs and the measurement methods of single DNA-based molecules. I will present new and surprising results on dsDNA molecules. I will present new DNA-based molecules and report on our measurements of their properties.

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#### Detection of particles, microorganisms and biomarkers using CMOS image sensors

#### Valerio Pruneri,

R. Camphausen, R. Hussain, , R. Terborg, L. Duempelmann. A. Cuevas, E. Wajs, S. Diefenbach ICFO; Spain

Valerio.Pruneri@icfo.eu

We will present recent developments in using images sensor arrays to detect minute quantities of transparent materials, small particles, microorganisms and biomarkers. The designs of the large-field of view imagers are novel and exploit scattering and phase (interferometric) effects in the classical and quantum regime.

#### **Medical Nanoparticles: Principles of Design**

#### Victor Puntes<sup>1</sup>

Catalan Institute of Nanoscience and Nanotechnology (ICN2), CSIC and BIST, Campus UAB, Bellaterra, 08193 Barcelona, Spain Vall d'Hebron Institut de Recerca (VHIR), 08035, Barcelona, Spain Institució Catalana de Recerca i Estudis Avançats (ICREA), P. Lluís Companys 23, 08010 Barcelona, Spain

#### Contact@E-mail (victor.puntes@vhir.org)

From last two decades of intense research at the nanobiointerface a series of conclusions can be drawn with respect a general set of rules for inorganic nanoparticle design for medical applications. This includes, not only purity, sterility and monodispersity but also feasibility and traceability, metabolization and excretion. In this context, safety is paramount and efficacy has to be developed in a context of a real pressing and precise medical need. Safety is mandatory not only in the development of medical tecyhno9logies but indeed any new technology has to be introduced safely, nanoparticles also. Finally, therapeutic doses has to be achieved, that may be high for colloidal NP stability (always at ease at low concentrations). Similarly, when thinking on dosing, persistency of NPs and potential accumulation has to be carefully controlled to avoid long term damage. This implies to develop a full nanoADME (administration, distribution, metabolization and excretion) model to enable NPs to be used in medicine.





t: 15 min



#### **Figures**

Figure 1. Concentration of AuNPs to reach theraputical dose of the conjugate.

Figure 2: Dark Field Confocal microscopu pm A549 exposed to AuNP-CisPt for 24 hours

Fig.3. CeO2NPs Tumor enhanced Computer Tomography Xray images.

#### Bio-Inspired Peptide-Based Functional Coating

#### **Meital Reches**

Institute of Chemistry and the Center for Nanoscience and Nanotechnology, The Hebrew University of Jerusalem, Edmond Safra campus, Jerusalem, Israel

#### Meital.reches@mail.huji.ac.il

The lecture will present bio-inspired functional coatings that are spontaneously formed by short peptides. These peptide-based coatings selfassemble on metals, oxides and polymers under mild conditions without any need for a curing step. The coating can serve in many functions. One application is preventing biofouling - the undesirable adhesion of biomolecules and organisms to surfaces. [1-2] This process leads to numerous adverse phenomena including hospital-acquired infections, blockage of water desalination facilities and food contamination. We showed that this coating prevents the first step of biofouling, which involves the adsorption of bioorganic molecules to the substrate. Moreover, the coating significantly reduces the attachment of various organisms such as bacteria and fungi to surfaces. Another function that these peptide-based coatings can mediate is the adhesion of mammalian cells to implants. [3] This function is important for the integration of implants into the human body. Finally, we showed that these peptides self-assemble in solution into particles that adsorb and release active compound that synergistically reduce the number of bacteria on the surface. [4]

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Figure 1. Peptide-based antifouling particles on surface release antimicrobial agents.

#### Force pathway to synaptic clustering at the neuromuscular junctions of embryonic flies

**Taher Saif**<sup>1</sup>, Anthony Fan, Saddam Joy<sup>1</sup>

<sup>1</sup>Mechanical Science and Engineering University of Illinois at Urbana-Champaign 1206 West Green St, Urbana, IL 61822, USA

saif@illinois.edu

#### Abstract (Arial 10)

Memory and learning in animals are mediated by neurotransmitters that are released from vesicles clustered at the synapse. Vesicle clustering has been believed to result primarily from biochemical signaling processes that require the connectivity of the presynaptic terminal with the cell body, the central nervous system, and the postsynaptic cell. We show, using embryonic Drosophila motor neurons. that vesicle clustering at the neuromuscular presynaptic terminal depends on mechanical tension within the axons [1]. Neurons generate this tension within the first two hours of synaptogenesis, and actively maintain the tension of about 1 nN by employing acto-myosin machinery. If the rest tension is perturbed mechanically, axons restore the rest tension either by relaxing or by contracting over a period of about 15 min. Vesicle clustering vanishes upon severing the axon from the cell body, but is restored when mechanical tension is applied to the severed end of the axon. Clustering increases when intact axons are stretched mechanically. We finally reveal the underlying mechanism by which tension and vesicle clustering are linked [2]. The role of mechanical force in vesicle clustering is a new paradigm in the understanding of synaptic functions. This force paradigm may lead to new treatments for neurological diseases.

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#### Figures

**Figure 1.** Nervous system of an embryonic Drosophila (left). The axons of motor neurons emanate from the Central Nervous System (CNS) to form Neuro Muscular Junction (NMJ) with muscle. One of the axons is resected by a laser beam. The neurotransmitter vesicles de-cluster after resection. But if the cut end is pulled by a pipette, vesicle clustering is restored.



## Nanomotors: Artificial active matter for nanomedicine

#### Samuel Sánchez<sup>1,2</sup>

<sup>1</sup>Institute for Bioengineering of Catalonia (IBEC), The Barcelona Institute for Science and Technology (BIST), Barcelona, Spain

<sup>2</sup>Catalan Institute for Advanced Studies (ICREA),

Barcelona, Spain

#### ssanchez@ibecbarcelona.eu

Engineering nanomotors which convert chemistry into motion is of fundamental relevance and interesting for specific applications. Self-propelled micro- and nano-motors are opening many avenues in fields such as nanomedicine, robotics, biosensing, microfluidics, and environmental field [for reviews see 1-3]. Due to the versatility of fabrication techniques available nowadays, we can synthesize nano- and micromotors of different shapes and materials almost on demand, from nanoparticles, microcapsules to nano- and microtubes.

The combination of biological components and artificial ones emerges into what we call hybrid machines/bots. Alike bacteria or small swimmers found in nature, artificial nanobots convert bioavailable fuels to generate propulsion force to swim at the nanoscale. One of the dreams in nanotechnology is to engineer small vehicles which can eventually be applied in vivo for medical purposes. Major advances have been demonstrated towards that end, however, questions like -how to swim at the nanoscale, how to achieve motion control and how to image these nanobots- need to be properly addressed.

Here, I will present our recent developments in the field of nanomotors that can autonomously swim and perform complex tasks in vitro. Our hybrid "bots" combine the best from the two worlds: biology (enzymes) and (nano)technology (nano- micro-particles) providing swimming capabilities, remote control, multifunctionality and actuation.[4]

I will present some of the fundamental aspects that we have studied for enzyme nanomotors such as the role of asymmetry, catalysis and enzyme quantity [5]. Moreover, I will show some proof-ofconcept applications such as the efficient transport and the enhanced release of drugs into cancer cells [6] and spheroids [7], sensing [8].

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#### **Figures**

Figure 1. Micro-and nanomotors, from fundamentals to applciations





ACS Publications

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#### From basic principles of protein self-assembly to rational design of multifunctional fibers

#### Ulyana Shimanovich <sup>1</sup>,

<sup>1</sup>Department of Materials and Interfaces, Weizmann Institute of science, Rehovot, 76100, Israel.

Ulyana.shimanovich@weizmann.ac.il

Self-assembly is the autonomous organization of components into patterns or structures without human intervention. A number of different assemblies can be formed by proteins. A particularly interesting example of protein self-assembly is a formation of highly ordered, nearly one-dimensional fibrilar structures. This high-level, long-range ordering is relatively independent of the molecular identity of the protein monomers. Interestingly, in nature, such structures can perform either beneficial roles or appear as aberrant protein aggregation, which is in a latter case results in the development of neurological disorders. The main objective of our research is to understand the evolution of protein complexes in the context of both biological function and malfunction as well as to draw the links between structure and properties of self-assembling materials based on natural polypeptides.

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Figure 1. Microgels made of protein nanofibrils

#### Glycosylated amphiphilic polymeric nanoparticles in active drug targeting

#### Alejandro Sosnik,

Laboratory of Pharmaceutical Nanomaterials Science, Department of Materials Science and Engineering, Technion-Israel Institute of Technology, Haifa, Israel

#### sosnik@technion.ac.il

The overexpression of energy-dependent and independent glucose receptors and transporters has been identified in different cell populations (e.g., macrophages). For example, in pediatric sarcomas, overexpression of glucose transporter 1 (GLUT-1) is associated with the more efficient uptake of this vital energy source and faster proliferation and metastasis. Nanotechnology has made sound contributions to treat disease due to the ability to target drug-loaded nanomaterials by the enhanced permeation and retention effect (passive targeting). Furthermore, the design of nanocarriers surfacemodified with ligands recognized by receptors overexpressed in specific cell types is an extensively investigated (though still unrealized in the clinical practice) strategy for active targeting and reduce offtarget accumulation and toxicity. Among the platforms, polymeric micelles with core-corona nanostructure and amphiphilic polymeric nanocarriers displaying more complex self-assembly patterns have gained great attention owing to their ability to encapsulate and target hydrophobic cargos and the chemical versatility to modify their surface. Aiming to confer them with active targeting features, in recent years, we designed a plethora of glycosylated amphiphilic polymeric nanocarriers and demonstrated that by tuning their composition and size, they undergo selective accumulation in solid tumors [1-3]. In this presentation, I will overview the strategies developed in my laboratory to improve the efficacy of the pharmacotherapy in cancer and also tune the phenotype of immune cells by using this unique type of nanoparticle.

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#### Nanomechanics and Nanomechanical Systems for Biology and Medicine

#### J. Tamayo,

O Malvar, J.J. Ruz, S. García-López, M.L. Yubero, A. Cano, V. Puerto, A. Sanz, E. Gil-Santos, D. Ramos, A. San Paulo, P.M. Kosaka & M. Calleja

Instituto de Micro y Nanotecnología(IMN-CNM), CSIC, Tres Cantos, Madrid, Spain.

jtamayo@imm.cnm.csic.es

Millions of people dies of cancer or infection every year in the first world and developing countries, respectively. Most of these lives could be saved if patients had timely access to early detection. Mass spectrometry and multiplexed immunoassays have rapidly developed during last years with improved limits of detection. Still these technologies can hardly probe the deepest region of the plasma, at concentrations below the pg/mL level in the case of cancer protein biomarkers or below 1000 virions per mL in the case of viral infections. Overcoming these detection limits is required for early detection [1]. This clearly indicates the need of implementing novel ultrasensitive techniques can cover the inaccessible regions of the plasma. We here propose biological detectors based on nanomechanical svstems for discoverv and detection of cancer protein biomarkers and pathogens in plasma. We review the modes of operation of these devices [2], putting our focus on recent developments on nanomechanical sandwich immunoassays [3] and nanomechanical spectrometry [4]. The first technique enables reproducible immunodetection of proteins at concentrations well below the pg/mL level, with a limit of detection on the verge of 10 ag/mL as well as the detection of one pathogen in 10 mL of plasma. The second technique enables the identification of individual pathogens by two physical coordinates, the mass and stiffness, instead of the mass-tocharge ratio of the protein constituents. This technology can enormously simplify the identification of pathogens such as virus and bacteria that are not accessible to current mass spectrometry detectors (http://viruscanproject.eu/). Finally, I will show some of our most recent developments for deciphering the role of the cell stiffness in cancer.

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## DNA-nanoparticle hybrids for single-molecule sensing

#### Peter Zijlstra<sup>1</sup>,

<sup>1</sup>Eindhoven University of Technology, Eindhoven, The Netherlands

p.zijlstra@tue.nl

Biofunctionalized nanoparticles are promising constructs for molecular sensing and drug delivery. Plasmonic nanoparticles are particularly attractive because the plasmon resonance enables single molecule detection by measuring shifts of the plasmon resonance [1,2], or by exploiting the fact that the fluorescence intensity of nearby fluorophores is strongly enhanced by the plasmon [3].

The functionality of such particle-based sensors is governed by their chemical interface, specifically by the number of functional groups per particle and particle-to-particle differences. The latter can only be resolved by single-particle and single-molecule approaches, so I will first show how we use correlative microscopy to characterize the number of functional groups on single particles.

We use a combination of super-resolution microscopy, single-particle spectroscopy, and atomic force microscopy to characterize and optimize functionalization protocols. I will then show the application of such biofunctionalized particles toward single-molecule sensors that can be applied biomedical and environmental for sensing applications.

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#### Dynamic systems mimicking the systemic complexity in biology

#### Loai K. E. A. Abdelmohsen<sup>1</sup>

<sup>1</sup>Eindhoven University of Technology Institute for Complex Molecular Systems P.O. Box 513 (STO3.41), 5600MB Eindhoven, the Netherlands

#### l.k.e.a.abdelmohsen@tue.nl

#### Abstract

One of the most inherent and interesting features of living systems is their adaptability to show complex behavior, in response to a variety of signals. Among these behaviors, autonomous motion has been an important source of inspiration for scientists who, over the years, have created a variety of synthetic motor systems, imitating biological motility[1]. For example, molecular motors[2], micro- and nanoscale sized Janus self-assembled polymeric motors[4], motors[3], movable tubules and rods[5] have been developed. Regardless of the excellent performance of these motor systems, there is a fundamental difference in the way movement is regulated in synthetic and natural systems. Cellular autonomous motion (e.g., vesicular transport and motility), displays adaptive features as a result of competing transient activation and deactivation processes, which are governed by enzyme-mediated energy input and consumption, and molecular interactions. Such dynamic processes are also referred to as out-of-equilibrium or dissipative; mimicking these behaviors in synthetic systems has recently drawn much attention from the scientific community. Introducing transient behavior into synthetic molecular or nanoscaled systems has been demonstrated for active materials with unique properties such as dissipative fibres[6], transient peptide hydrogels, vesicles or microcapsules[7], and non-equilibrium molecular recognition and colloidal systems[8]. In a stepwise fashion, we couple motility to a dynamic process, which is maintained by transient events[9]. This lecture will therefore focus on how we translate dynamic processes into motion - on both nano and micro scale.

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Figure 1. Schematic representation of the transient deactivation and activation of a stomatocyte nanosystem mediated by ATP.

#### Wound care and smart bandage technology based on Graphene monolayers

#### Vincent Bouchiat<sup>1</sup>,

<sup>1</sup>GRAPHEAL, 38042 GRENOBLE Cedex 09 France

Contact vbouchiat@grapheal.fr

After a decade and thousands of publications, graphene produced by CVD on copper foils remains at the sweet spot for quality and cost-effective production of large size, high-mobility graphene transferred on insulators. Use of these monolayers has been so far scarce in industrial applications. I will present the use of this technology for biological (1) and medical applications from both the academic and industrial point of view.

We have first explored the use of graphene-on polymer for biosensing and tissue engineering. I will show results of in-vitro cellular growth (neurons and skin fibroblasts) on graphene-covered substrate which shows the stimulation of growth (2) and migration of cells promoted by the graphene substrate together with the possibility of probing their electrical activity down to the sub-cellular scale (3).

We are also developing a novel technology platform that exploits the features of monolayer graphene, for woundcare. The first-generation of our system is a graphene-based scaffold that looks like a very thin, transparent plaster. Based on that material, we are building an innovative bandage technology platform based on graphene-on -insulator film in order to better support chronic wounds.

In particular, I will insist on the possibility to combine therapeutics (bio electrostimulation & healing) with diagnostics (biosensing) features in the same Following these properties, we have device. elaborated a graphene-based scaffold that looks like a very thin, transparent plaster integrated in commercial bandage that is indented to be applied in direct contact with an open wound. We believe these films will have some impact in healthcare, as they target some important and poorly addressed diseases such as pressure ulcers and diabetic foot ulcers I will present the preclinical results on animal studies and the perspectives of their commercial (3) use for wound-care, in particular in the treatment and diagnostics of chronic wounds that affect the diabetics and elderly.

Our bandage platform (4) is based on the integration of a monolayer graphene polycrystalline layer backbonded onto a biocompatible polymer layer (figure 1°. The resulting film can directly be applied onto the bed-wound and is inserted in a commercial bandage. Graphene surface combines healing (speed-up of wound closure) and antibacterial action. optical transparency and electrical conductivity. It is obtained by integrating a large uniform graphene monolayer into a bandage in order to provide a bio- stimulating and electrically-active platform directly applied in contact with the wound. It allows the development of a range of intelligent dressings that combine on the same product both therapeutic and diagnostic actions. -Therapeutic action: graphene functions as a growth matrix, promoting healing but at the same time acting as an electrode in close contact with the wound. This allows the application of electrical pulses whose actions promote faster healing and reduce pain. -Diagnostic action: Graphene it plays at the same time the role of a biosensor to monitor the wound evolution and early stage detection of infection by

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pH and biomarker sensing.



**Figure 1.** Principle of the graphene-coated bandage platform: a single monolayer of polycristalline, CVD Graphene is assembled onto a biocompatible polymer and integrated in a bandage.

#### Scanning probes for enzyme nanopatterning and for the spatial mapping of collagen micro-stiffness in tissue sections

#### Annalisa Calò<sup>1</sup>

<sup>1</sup>Department of Electronic and Biomedical Engineering of University of Barcelona, Carrer de Martí i Franquès 1 08028 Barcelona

annalisa.calo@ub.edu

Scanning probe microscopy makes use of small probes, with size from tens of nanometers to few micrometers, scanned over the sample surface to obtain topographical and mechanical information with spatial resolution and force sensitivity. In a different application, scanning probes can be used as nanometric pens to locally modify the sample surface in contact with the probe. This second approach provides lithographic capabilities and it is called scanning probe lithography (SPL)<sup>1</sup>. In SPL, different inputs are used to generate the desired surface modification. In particular, when heatable cantilevers are employed to locally induce chemical reactions, the technique is called thermochemical nanolithography (tc-SPL)<sup>2</sup>. Both approaches can be of great interest for biological applications, to provide functional (nano and micro-mechanical) markers in biological surfaces (AFM) or for patterning purposes (tc-SPL). In my presentation, I will show the use of force volume AFM for the spatial mapping of collagen distribution in mammalian tissues with affordable timescales. This study points to the use of AFM as a routine tool in the biomedical research, to provide micromechanical data that correlate with outputs from other (optical, biochemical, histological) techniques<sup>3</sup>. I will also describe tc-SPL for the fabrication of nanoscale patterns in polymer films. These patterns can be used for enzymes anchoring with high throughput, high reproducibility and spatial control, till the single molecule level. Tc-SPL allows for the fabrication of 3D surfaces with independent control of topography and chemistry, and in my work it is employed to generate pockets (< 10 nm in size) that accomodate single enzymes<sup>4,5</sup>.

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#### **Figures**



Figure 1. Enzyme patterning through tc-SPL.

Reference section Adjacent, non-stained section for IT-AFM

Figure 2. Force volume AFM in tissue sections from human liver.

#### Nanoneedle Arrays for Intracellular Sensing and Delivery

#### Ciro Chiappini<sup>1,2</sup>

<sup>1</sup>Centre for Craniofacial and Regenerative Biology, King's College London, London, United Kingdom <sup>2</sup>London Centre for Nanotechnology, London, United Kingdom

#### ciro.chiappini@kcl.ac.uk

Nanoneedles are rapidly emerging as a tool to interact with the intracellular environment of a large number of cells simultaneously, with limited perturbation of their physiological processes. This interaction provides characteristic advantages for minimally invasive cell and molecular biology investigations, as well as progression of biomedical translation of regenerative and precision medicine approaches.

A quick string of several successful proofs of principles have established nanoneedles' potential to efficiently deliver impermeant molecules and nanoparticles directly to the cell cytosol, and to sense the intracellular milieu across biological systems ranging from cells in culture to living organisms.

This talk presents an overview of our recent research advances in leveraging the nanoneedle biointerface to enable intracellular sensing and delivery in the context of diagnostics and tissue engineering.

High aspect ratio nanostructures provide a unique biointerface [1] that stimulates multiple mechanosensory elements within the cell, inducing non-canonical regulation of the YAP and Lamin A mechanosensors.[2] This interfacing also enhances payload delivery across the cell membrane and the harvesting of biomolecules from the intracellular space through a combination of enhanced endocytosis and increased membrane permeability [3].

Using nanoneedle arrays as a delivery vector for nucleic acids enables highly efficient transfection in localised delivery vitro and with minimal invasiveness in living organisms [4]. In particular the nanoneedle-mediated delivery of a plasmid coding for the vascular endothelial growth factor (VEGF) to the muscle of a mouse stimulates neovasculature formation driven by exogenous VEGF expression, in the first example of nanoneedle mediated gene therapy. This method of delivery does not impact on the structure of the tissue, induce cell death or elicit an immune response.

Nanoneedles can also sense the intracellular environment [5]. Nanoneedle sensors can map the activity of cancer biomarkers across cell cultures and tissues, with the potential to identify tumour margins and detect cancerous dissemination beyond the margin [6].

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Figure 1. False-colored SEM micrograph of a human cell in the early stages of adhering to a nanoneedle array.

#### Membrane tension and domains: New method of measurement and visualization

#### Adai Colom Diego 1,2,3,

Pau Guillamat<sup>1,3</sup>, Naomi Sakai<sup>2,3</sup>, Stefan Matile<sup>2,3</sup>, Aurélien Roux<sup>1,2,3</sup>

<sup>1</sup>Biochemistry Department, University of Geneva, Geneva, Switzerland.

 <sup>2</sup>Swiss National Centre for Competence in Research Programme Chemical Biology, Geneva, Switzerland
 <sup>3</sup>School of Chemistry and Biochemistry, University of Geneva, Geneva, Switzerland

#### adai.colom@unige.ch

Organelles and cells are delimited by a lipid bilayer, which is highly deformable, a property essential to many cell processes such as motility, endocytosis, cell division. During these deformations, lipid membranes experience stretch causing membrane tension. Membrane tension is therefore a main regulator of the cell processes that remodel membranes, albeit, it is difficult to measure in vivo. FliptR (for Fluorescent LIPid Tension Reporter) can monitor changes of membrane tension by changing its fluorescence lifetime as a function of the twist between its fluorescent groups. We show that fluorescence lifetime depends linearly on membrane tension<sup>1-3</sup>, allowing for an easy quantification of membrane tension by fluorescence lifetime imaging microscopy (FLIM) and Fast-FLIM.

Given that **FliptR** tremendously facilitates membrane tension measurements, we are currently studying membrane tension on the organelles<sup>4</sup>, plasma membrane and tissues during different cell processes.

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**Figure 1.** A) Twisted and planar conformation structure of FliptR based in the lateral pressure. B) Cell membrane domain related with tension during cell migration. C) FLIM images of mitochondria and ER organelles, D) cell adhesion surface on pattern and E) zebrafish embryo.

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#### Characterization of the immunomodulatory properties of graphene-based materials and their application as novel biomedical nanotools

Lucia Gemma Delogu<sup>1,2</sup>,

Laura Fusco<sup>2,3,4</sup>, Marco Orecchioni<sup>5</sup>, Valentina Bordoni<sup>5</sup>, Alberto Bianco<sup>6</sup>

<sup>1</sup>Department of Biomedical Science, University of Padua, Via Ugo Bassi, 58/B, 35131, Padua, Italy <sup>2</sup>Istituto di Ricerca Pediatrica, Fondazione Città della Speranza, Corso Stati Uniti 4, 35127 Padua, Italy. <sup>3</sup>Department of Chemical and Pharmaceutical Sciences, University of Trieste, Via L. Giorgieri 1, 34127 Trieste, Italy;

 <sup>4</sup>Sidra Medical and Research Center, Doha, Qatar;)
 <sup>5</sup>University of Sassari, Sassari, Italy; <sup>6</sup>CNRS, Institut de Biologie Molèculaire et Cellulaire, Laboratoire d'Immunologie et Chimie Thérapeutiques, France;

luciagemma.delogu@unipd.it

#### Abstract

Graphene-based materials (GBMs) are promising nanotools for biomedical application. However, a critical step for any clinical translation of GBMs is represented by the assessment of their impact on the complexity of the immune system.

Encouraged by our previous findings, demonstrating the dramatic impact exerted by the different physicochemical properties of GBMs on the modulation of their immune effects [1-4], here we evaluated the effects of graphene oxide (GO) and amino-functionalized GOs with different lateral size dimensions on a large variety of human immune cells (unpublished data).

Exploiting innovative approaches, such as single-cell mass cytometry, we revealed that the amino decoration of GO increased its immune compatibility and was also able to induce a specific M1 like activation of monocytes and the secretion of interleukin-4 and Granzyme-B from B cells, skewing a cytotoxic-like response.

Moreover, thanks to the combination of GO with inorganic quantum dots containing indium, the detection of GO cell uptake was enabled using single cell mass cytometry. Our results highlighted that monocytes and, intriguingly, B cells, were the main immune cell subpopulations able to internalize GO.

We finally exploited the immune modulatory proprieties of a specific GO on monocytes in

combination with the osteoinductive capacity of calcium phosphates (CaP) for the design of a novel biocompatible nanomaterial called maGO-CaP (monocytes activator GO complexed with CaP) [5]. Our *in vitro* and *in vivo* results demonstrated maGO-CaP ability to induce osteoinductive stimuli increasing bone regeneration thanks to its modulation of the immune cell functionality.

Overall, our investigations suggest that well designed and functionalized GBMs allow the modulation of immune cells exploitable for the treatment of several pathologies, paving the way for their future biomedical applications.

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#### **Figures**

CTRL





Figure 1. In vivo bone formation. Microcomputed tomography ( $\mu$ CT) image of untreated tibia (left, CTRL) and after one month of maGO-CaP treatment (right, GO-CaP).

#### Electrochemical nanoreactors and nanomotors for potential biomedical applications

**M.J. Esplandiu**<sup>1</sup>, K. Zhang<sup>1</sup>, J. Fraxedas<sup>1</sup>, D. Reguera<sup>2</sup>, B. Sepulveda<sup>1</sup>,

<sup>1</sup>Catalan Institute of Nanoscience and Nanotechnology (ICN2), CSIC and BIST, Campus UAB, Bellaterra, 08193 Barcelona, Spain <sup>2</sup>Departament de Física de la Matèria Condensada, Universitat de Barcelona, C/Martí i Franguès 1, 08028

Mariajose.esplandiu@icn2.cat

Barcelona, Spain

One of the aspirations of nanotechnology is to become true the long-awaited development of nanomachines which can autonomously move and perform different tasks from sensing to repairing and thus to emulate the complex functionalities of biological systems. Such achievement is expected to have a revolutionary impact in fields such as medicine. Under this context, the engineering of artificial self-propelled micro/nanomachines with multitasking capabilities has become a research line of growing interest since the pioneering studies at the beginning of this millennium.

These self-propelled micro/nanomachines generate local physicochemical gradients to drive their own motion, which is harnessed to perform multi-tasking activities in different locations. Self-propulsion generated by gradients from local electrochemical reactions is a very interesting strategy for autonomous motion. Although there have been many proofs of concept of chemical machines performing different activities, the progress on the comprehension of the physicochemical fundamentals behind the self-generated actuation has been more moderate. In many cases, the precise motion mechanism is still not unambiguously identified, and the key physicochemical parameters are not well-characterized. A complete and deep understanding of such issues would help to improve the control levels for applications and to better assess perspectives and challenges of these selfpropelled machines. In this presentation, we will review a combined set of techniques that we have chemically implemented to study propelled micro/nanomotors using pumps as the immobilized motor counterparts (Fig. 1). These techniques have turned out to be very useful for mapping chemical reactions and for extracting physicochemical parameters (e.g. electric fields, fluid flows) and thus to achieve a more complete characterization of the mechanisms driving fluid motion [1-3]. Moreover, the chemical reactions in these motors can not only be used to produce the self-propulsion but also to generate reactive products that can in turn chemically modify the immediate environment on the fly. In this context, we will introduce some promising

active micro/nanomachines that could have potential impact on biomedicine.

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#### Chemical reaction Pumps Pumps Tracking E and V H<sup>+</sup> H<sup>+</sup> H<sup>+</sup> H<sup>+</sup> Napping chemical gradients Swimmers Chemical reaction

**Figure 1.** Understanding chemically propelled motors using pumps as the immobilized motors counterparts.

#### *In silico* study of proteinnanoparticle assembly and protein aggregation in crowded environments

#### Giancarlo Franzese<sup>1</sup>

<sup>1</sup>Secció de Física Estadística i Interdisciplinària– Departament de Física de la Matèria Condensada, Facultat de Física,

& Institute of Nanoscience and Nanotechnology (IN2UB), Universitat de Barcelona, Martí i Franquès 1, 08028 Barcelona, Spain

#### gfranzese@ub.edu

A pristine nanoparticle (NP) in a biological fluid is covered spontaneously by absorbed biomolecules forming a corona. Proteins, in particular, are one of the main components of it and can be part of the 'hard' or the 'soft corona', remaining for a relevant time on the NP or dynamically exchanging with those in solution, respectively [1]. Experiments debate if the irreversible protein adsorption can cause loss of specificity in targeting of prefunctionalized NPs [2] or not [3]. Other data show that a minority of the protein's epitopes are appropriately arranged for receptor bindina. consistent with a stochastic and irreversible adsorption process in which proteins are, at least partially folded in their native state even when adsorbed in the hard corona [4]. Therefore, the details of the protein-NP assembly are essential to understand the possible nanoMedical applications [5]. Here we perform in silico studies to understand how the presence of interfaces or crowding affect the stability of the native state of a protein and its aggregation rate.

We consider several cases of proteins, from those with a unique native state to those intrinsically disordered, by means of a coarse-grain protein model in explicit solvent [6-9]. By Monte Carlo calculations, we show how relevant is the water contribution to protein denaturation and folding [10, 11] and to protein design [12]. We reveal that the hydropathy profile of proteins is a consequence of evolutionary pressure exerted by water in simplified geometries [12] and in bulk [13]. We find that a hydrophobic interface destabilizes the protein native state but can allow it to fold even if adsorbed onto a surface [14].

Furthermore, we study the proteins in a crowded environment, where the aggregation is tuned in a

way that enable them to be functional at the concentrations required for optimally efficient performance [15]. We show how the increase of the concentration of individual protein species can induce a partial unfolding of the native conformation without the occurrence of aggregates. A further increment of the protein concentration results in the complete loss of the folded structures and induces the formation of protein aggregates (Fig. 1). We discuss the effect of the protein interface on the water fluctuations in the protein hydration shell and their relevance in the protein-protein interaction [16]. These results can lead the way for engineering proteins and drugs that would be functional at extreme conditions and it is potentially relevant in protein-NP assembly for nano-Medicine applications [17, 18].

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**Figure 1.** Protein unfolding vs aggregation. Color map of the free energy profile of a selected protein, as function of the native contacts and inter-protein contacts, for different protein concentration *c*. Native contacts and inter-protein contacts have been normalized to 1. Adapted from [16].
# Nanomechanical properties of the cytoskeleton influence neuronal function in C. elegans

### Michael Krieg<sup>1</sup>,

<sup>1</sup>ICFO, Av CF Gauss 3, Castelldefels, Spain michael.krieg@icfo.eu

### Abstract

The millimeter scale mechanics of biological tissues is an emergent character originating from the material properties of the constituent cells and their mutual adhesive interactions. Likewise, the cell is an inhomogenous, non-isotropic and non-linear material composed of thousands of different components that interact transiently and/or permanently. Despite this complexity, previous research has shown that a few dominating elements of the cytoskeleton are largely responsible for the cellular strain response to mechanical stress. Thus, it is plausible that these mechanoresponsive molecules also endow some functionality to the cell - a property that has been largely investigated decoupled from the cellular physiology[1].

During my talk, I will highlight recent progress to understand the interplay between cellular and molecular nanomechanics and their role in regulating cellular physiology[2]. I focus on work on the nervous system of the roundworm Caenorhabditis eleaans. which is а popular experimental system to combine engineering, biophysics and cell biology, due to its stereotyped body plan, known structural connectome and amenable genetics. C elegans uses a set of different sensory neurons to navigate its habitat which endow the animals to process chemical and mechanical stimuli in a changing environment. Some of these neurons respond to minute mechanical forces delivered to the skin of the animal, while others respond to stresses generated within the animals that originate from muscle contraction during locomotion. How these stresses are borne by molecular mechanics, transmitted within biological tissues and activate biochemical pathways is one of the last challenges in mechanosensory biology[2]. This lack of understanding is largely due in part to the absence of appropriate techniques to investigate the effect of mechanical properties of cells and neurons within living organisms at the level of a single molecule. With a combination of genetically encoded reporters for mechanical stress and together with piconewton force calcium. measurements. we investigate the pathways mechanotransmission leading to physiological response to mechanical stress. To our surprise, a single point defect in cytoskeletal proteins can have a large consequence on the

stability of neurons against mechanical stresses, leading to a functional deficit[3].

We also introduce novel microfluidic devices (Ref [4] and in prep.) that enables the delivery of precise stresses to immobilized animals while reading out mechanical deformations and physiological functions. Using these technologies, we showed that a ubiquitously expressed protein of the cortical actin cytoskeleton, called β-spectrin, has neuron-specific role on mechanosensation and is subjected to mechanical stress during physiological processes. Mutations in this protein lead to a failure to properly sense forces and consequently severe uncoordination. Strikingly, similar mutations in the linker regions of b-spectrin have been shown to destabilize adjacent domains with consequences on overall cytoskeletal flexibility that lead to hemolytic diseases in humans[5]. Since the molecules are ubiguitously expressed in mammalian central nervous system and highly conserved among different species including humans, the results from our experimental paradigm bridge the gap between tissue culture and the clinics and are thus critical for our understanding of complex mechanical systems such as the brain.

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# Versatile Single Chain Polymer Nanoparticles in Drug Delivery and Targeted Imaging

### Jos M. J. Paulusse<sup>1</sup>

 <sup>1</sup> Department of Biomolecular Nanotechnology, University of Twente, Enschede, the Netherlands.
 <sup>2</sup>Department of Nuclear Medicine and Molecular Imaging, University Medical Center Groningen, the Netherlands.

### J.M.J.Paulusse@utwente.nl

As the area of controlled drug delivery is increasingly finding application in a variety of diseases, with different targeting sites and drug candidates, there is an urgent need for adjustable nanocarrier systems. Linear biopolymers folded into 3D-structures fulfill a wide array of complex functions and are omnipresent in biological systems; prime examples are proteins, in which the precise positioning of monomeric units (i.e. amino acids) largely determines protein morphology and therefore their remarkable variety of properties.

Due to their chemical diversity and highly modular nature polymers, and polymeric nanoparticles in particular, are popular drug carrier materials. Most polymeric nanoparticles are in the 50-200 nm size range, which is unfortunate, since proteins, enzymes and some viruses are considerably smaller in size.

In order to widen the existing polymeric drug carrier systems to the sub-20 nm size regime, we are investigating single-chain polymer nanoparticles (SCNPs) for controlled drug delivery and targeted SCNPs are prepared through imaging. [1] intramolecular crosslinking of individual polymer chains into individual nanoparticles and thus offer tremendous control over size and dispersity. Through exclusive intramolecular crosslinks, SCNPs are an order of magnitude smaller than conventional polymer nanoparticles, easily accessible in relevant quantities and without the requirement of complex synthetic strategies. Highly modular in nature, these sized polymer nanoparticles enable uniquely encapsulation and controlled release of drug molecules, irrespective of their hydro- or lipophilicity. [2]

Preparation of SCNPs from prepolymers containing pentafluorophenol activated esters, followed by functional amine substitution, allows for careful engineering of the nanoparticle surface, providing control over distribution behavior and enabling the mimicking of proteins in terms of shape, composition and even function. Current efforts focus on evaluation of these promising materials in vivo.

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### Figures



Polymer Nanoparticle

**Figure 1.** Intramolecular crosslinking of polymers, in the presence of therapeutics, to form single chain polymer nanoparticles for application in nanomedicine.

# Super resolution microscopy as a tool for tackling nanomedicine challenges

Sílvia Pujals<sup>1,2</sup>,

Lorenzo Albertazzi<sup>1,3</sup>

<sup>1</sup>Nanoscopy for Nanomedicine group, Institute of Bioengineering of Catalonia (IBEC), the Barcelona Institute of Science and Technology (BIST), C\ Baldiri Reixac 15-21, Helix Building 08028 Barcelona, Spain

<sup>2</sup>Department of Electronics and Biomedical Engineering, Faculty of Physics, Universitat de Barcelona, Barcelona, Spain. <sup>3</sup>Department of Biomedical Engineering, Institute for

Complex Molecular Systems (ICMS), Eindhoven University of Technology 5612AZ Eindhoven, The Netherlands

spujals@ibecbarcelona.eu

Our group uses advanced microscopy techniques to visualize and track in living cells and tissues selfassembled nanomaterials with therapeutic potential. The understanding of materials-cell interactions is crucial towards the development of novel nanotechnology-based therapies for treatment of cancer and infectious diseases.

Many biological structures are made of multiple components that self-organize into complex architectures. Here we want to mimic this phenomenon to develop novel bioactive materials such as nanoparticles or nanofibers able to build 3D self-assembled themselves (1D or nanomaterials). Having the self-assembly motif decorated with different functionalities allows a modular and tunable approach that eases sample preparation.[1]

То study the behavior of such complex nanomaterials in action we make use of a variety of optical microscopy techniques, in particular super resolution microscopy (SRM).[2,3] SRM can achieve a resolution down to 20 nm and represents an ideal tool to visualize nanosized objects in the biological environment. In particular we demonstrate how STORM Optical (Stochastic Reconstruction Microscopy) can be used to image a wide range of nanomaterials beyond diffraction the limit: nanoparticles[4], BTA fibers[5], peptidic nanostructures [6], etc.

Remarkably, STORM allows this observation in the biological environment, thus we are able to follow the journey of nanomaterials inside the body: from protein corona formation[7] to extravasation, targeting and tracking nanomaterials inside the cell.[8-10]

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# Curve and cut: membrane trafficking *in sillico*

### Anðela Šarić<sup>1</sup>,

<sup>1</sup>University College London, Gower St, London, UK a.saric@ucl.ac.uk

Cellular membranes constantly need to be cut and reshaped to sustain inter- and intracellular trafficking and enable life. The cell has developed a wide array of strategies for forming and reshaping its membrane structures, just as pathogens have evolved their own means of breaching the outer cell layer. These are at their heart physical processes, which require mechanical work and involve action across various scales.

Our group develops minimal coarse-grained models investigate membrane computer to remodeling strategies, in close collaboration with experimental colleagues [1-5]. Here I will first present our findings on the evolution of membranecrossing nanoparticles (unpublished). Then I will discuss our results on how heterogeneity of the membrane composition can increase the membrane selectivity to this nanoparticle uptake [1]. Finally, I will present our recent model on active membrane cutting from the inner side of the membrane neck, driven by ESCRT-III nanomachinery (Figure 1) [2].

The physical principles revealed by our simulations can help us understand how the nanomachinery of life operates and can guide the design of man-made structures to manipulate cell membranes and deliver materials to cells.

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Figure 1. Cargo release by ESCRT-III machinery

# Role of surface topography on adhesion of motile bacteria

### Giorgio Volpe<sup>1</sup>,

<sup>1</sup>Department of Chemistry, University College London, 20 Gordon Street, WC1H 0AJ London, UK

### g.volpe@ucl.ac.uk

Only two decades ago, bacteria were considered as well-characterized biophysical entities, which offered little room for new discoveries. We now know that this picture is truly wrong and naïve. In recent years, bacterial cells have come back to the spotlight due to many bacterial species developing antimicrobial resistance (AMR) even to last-resort drugs. In particular, the way bacterial cells localize near a surface is key to the emergence of several phenomena of biological, ecological and medical relevance, including biofilm formation. Here, I will show how microfeatures on a surface have a nonnegligible effect in shaping the propagation and localization dynamics of bacterial cells on the same. Beyond demonstrating the critical role played by surface defects on the near-surface motion of bacterial cells, these results can inspire novel routes to control microbial ecology in natural habitats and devise engineered materials for the control and prevention of bacterial adhesion to surfaces

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Figure 1. Trajectories of *E. coli* bacteria in complex porous environments.



# Complex Nanoporous Anodic Alumina Photonic Structures for Sensing: Design, Fabrication and Application

### Laura K. Acosta

Elisabet Xifre-Perez, Josep Ferré-Borrull, and Lluis F. Marsal Departament d'Enginyeria Electrònica, Elèctrica i Automàtica, Universitat Rovira i Virgili, Avinguda Països Catalans 26, 43007 Tarragona, Spain

#### lluis.marsal@urv.cat

Nanoporous anodic alumina (NAA) is a promising material formed by the electrochemical anodization of aluminum, a cost-effective and fully scalable process compatible with conventional micro and nanofabrication approaches that allow the precise control over the geometry and distribution of the pores [1-2]. NAA has high chemical and physical stability, provides stable optical signals without further passivation; and its surface chemistry can be easily modified with a broad range of molecules.[3] Moreover, the optical properties of NAA rely intrinsically upon its nanoporous architecture. Therefore, to engineer the nanoporous structure of NAA provides novel means of modulating its refractive index in a multidimensional fashion to fabricate advanced materials with unique optical properties to guide, reflect, transmit, emit incident light [4]. Furthermore, the pore geometry can be varied by different methods to obtain different functionalities such as funnels [5], branched pores and even structures with remarkable optical properties such as Distributed Bragg Reflectors, Rugate filters, etc [6-7]

Photonic structures (PS) can be obtained by NAA pore engineering. NAA-PSs are obtained by applying a sinusoidal anodization current, which results in a continuous modulation of the pore diameter along its length. The application of this modulation results in a one-dimensional photonic crystal with a periodic variation of the refractive index along the pore direction and a photonic stop band.[8]. Previous studies have also developed NAA-PSs with different anodization current profiles such as sawtooth-like pulse anodization [9], and square wave [10] to achieve better control over the oxide growth rate and porosity of NAA.

In this work, we propose novel methods to obtain NAA-PSs applying different current profiles. Our study establishes a better understanding of the effect that the different anodization parameters have on the optical properties of NAA-PSs such as their characteristic reflection bands across UV-visible-NIR spectrum. We present a comprehensive study of different NAA-PSs based on single and multiple structures with sinusoidal profiles in an overlapped and stacked configuration. The stacked configuration consists of multiple currents are applied sequentially and the overlapped configuration consists of the average sum of multiple sinusoidal waves into a single complex waveform. Each sinusoidal wave determines the position and the reflectance amplitude of a forbidden band. In this case, the different periodic structures are stacked or overlapped on the same structure. The effective medium of the resulting photonic structures (PSs) is demonstrated to be optimal for the development of optical bio-sensing platforms.

All these photonic structures were prepared by anodization of a high-purity aluminum foils in 0.3 M oxalic acid electrolyte at 5 °C. Figure 1 shows ESEM top view (a) and cross-section (b) picture in a stacked configuration. The straight pores can be recognized in the cross-section, Figure 2 shows the reflectance spectrum of the sample after removing the remaining aluminum. Figure 2a shows the reflection spectrum of a sample in overlapped configuration with  $I_0 = 4 \text{ mA}, I_1 = 2 \text{ mA}, T1 = 100 \text{ s},$ T2= 150 s and T3= 200 s. In figure 2b we can observed the reflectance spectrum in stacked configuration wit  $I_0 = 4 \text{ mA}$ ,  $I_1 = 2 \text{ mA}$ , T1 = 125 s, T2 = 125 s150 s and T3= 175 s. The application of stacked sinusoidal current profile gives rise to the formation the three photonic stopbands. The height of these stop bands reaches 18-37 % while its width was 10-23 nm and the position of the photonic band corresponding central wavelength,  $\lambda = 330-500$  nm.

In order to evaluate the suitability of these complex NAA-PSs, we assessed shifts in the position of the reflectance band filling the nanopores with different concentrations of aqueous solutions of D-Glucose.

We analyzed changes in the refractive index of the medium filling the pores by real-time spectroscopy. To this end, the sample is mounted in an acrylic cell with a transparent window that permits the measurement of the reflectance spectrum by a fiber mini spectrometer while different fluids are injected to cell and fill the NAA-PSs pores. Figure 3 illustrates the sensing principle of these photonic structures. The position of the reflectance band shifts to longer wavelengths when the nanopores are filled with different concentrations of D-Glucose.

In this work, we demonstrate the possibility to fabricate NAA-PSs by the application of different types current profiles. We also demonstrate the ability of structures to detect a change in the refractive index of the fluid filling the pores by means of real-time spectroscopy. With this method, it is possible to sense glucose in low concentrations. These results open up the possibility of using these complex NAA-PSs for detection of many other molecules for bio-sensing applications. Acknowledgments: This work was supported by the Spanish Ministerio de Ciencia, Innovación y Universidades (MICINN/FEDER) RTI2018-094040-B-I00, by the Agency for Management of University and Research Grants (AGAUR) ref. 2017-SGR-1527 and by the Catalan Institution for Research and Advanced Studies (ICREA) under the ICREA Academia Award.

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### **Figures**



**Figure 1.** (a) Top view (scale bar 1µm ) and (b) Cross-section (scale bar 1 µm) of NAA-PSs (stacked configuration)



Figure 2. Reflectance spectrum of NAA-PSs (a) Overlapped configuration and (b) stacked configuration



**Figure 3**. Sensing Principle of stacked NAA-PSs with Water and D-Glucose showing the red-shift in the position of de bands.

# All printed environment friendly, biocompatible, sustainable sucrose-based temperature sensor

### Junaid Ali<sup>1</sup>

Shahid Aziz<sup>2</sup>, Memoon Sajid<sup>3</sup>, Ghyas Uddin Siddiqui<sup>4</sup>, Kyung Hyun Choi<sup>2</sup>

<sup>1</sup> COMSATS University Islamabad, Pakistan <sup>2</sup>Jeju National University, Jeju, Republic of Korea, <sup>3</sup>GIKI, Topi, Pakistan <sup>4</sup>University of Karachi, Pakistan Junaid\_ali@comsats.edu.pk

### Abstract

The in-situ measurement of ambient temperature is significant in our daily life, industrial processes, and environmental monitoring. The thermistor-based temperature sensor is one of the most important candidates for temperature sensing that has advantages outstanding of immunity to electromagnetic interference, simple fabrication, cost-effectiveness, and durability against harsh environments. Thermo resistive devices are extremely sensitive to the external temperature; therefore, by applying thermo-resistive based material a temperature sensor with high sensitivity and practicability can be obtained. Organic and disposable sensors have great potential for applications such as food industry, environmental monitoring and medical industry. Various types of temperature sensors have been fabricated, which include thermocouples [1], nanogenerators based temperature sensors [2], and thermistors [3]. An all printed interdigitated electrodes (IDT) based temperature sensor has been demonstrated in this study. The IDTs were fabricated on a glass substrate by reverse offset printing. The sucrose film was fabricated by spin coating the sucrose solution on the IDTs. The sensors showed stable and close to linear response of resistance change by varying temperature in the range 0°C to 100°C. The resistance of the sensors changed from ~3200 k $\Omega$  to ~400 k $\Omega$  for the temperature change in the range 0°C to 100°C. This study provides an effective method to fabricate environment-friendly, biocompatible. sustainable and high-performance temperature sensors based on thermistor effect in the future.

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# Fundamental behaviour of nanoparticles revealed in zebrafish embryo

**G. Arias-Alpizar**<sup>1</sup>, *F.Campbell*<sup>1</sup>, *F.Bos*<sup>3</sup>, *S.Sieber*<sup>4</sup>, *BE. Koch*<sup>5</sup>, *J.Huwyler*<sup>4</sup>, *W.Jiskoot*<sup>2</sup>, *A.Kros*<sup>1</sup> and *J.Bussmann*<sup>2</sup>

 <sup>1</sup> Leiden Institute of Chemistry, Einsteinweg 55, 2333CC Leiden, The Netherlands
 <sup>2</sup> Leiden Academic Center for Drug Research, Einsteinweg 55, 2333CC Leiden, The Netherlands
 <sup>3</sup> Hubrecht Institute, Uppsalalaan 8, 3584CT Utrecht, The Netherlands
 <sup>4</sup> Pharmacenter, Klingelbergstrasse 50, 4056, Basel, Switzerland
 <sup>5</sup> Institute Biology of Leiden, Einsteinweg 55, 2333CC Leiden, The Netherlands

g.arias.alpizar@lic.leidenuniv.nl

Up to 99% of intravenously administered nanoparticles are cleared by the reticuloendothelial system (RES) cell types in the liver and spleen. The precise biological mechanisms which underpin clearance are not, however, fully understood.

Here, we use the transparent and versatile embryonic zebrafish as animal model to rapidly screen the behavior of nanoparticles *in vivo*. The ability to visualize fluorescent nanoparticles at cellular resolution and across entire living organisms has given us an unprecedented understanding of the fundamental behavior of nanoparticles *in vivo*.

In this presentation, I will demonstrate how key RES cell types of the embryonic zebrafish are genetically and functionally analogous to the mammalian liver sinusoidal endothelium. Furthermore, I will show how we identify stabilin-1 and stabilin-2 as the main receptors for scavenging anionic nanoparticles [1] by studying the distribution of various types of nanoparticles in the zebrafish in combination with CRISPR/Cas technology. The ligands that are cleared by zebrafish stabilin-1 and -2 receptors (glyco)proteins, include specific polyanionic carbohydrates, endotoxins, viruses and (in)organic nanoparticles -including liposomes used for clinical drug delivery- providing an alternative route to the nanoparticle clearance performed by macrophages.

Importantly, nanoparticle-SEC interactions can be blocked by dextran sulfate, a competitive inhibitor of *stabilin-1, stabilin-2* and other scavenger receptors. The importance of particle size in the nanomedicine field is also highlighted here, showing that small particles are the more convenient to avoid liver sequestration by scavenger receptors and to promote internalization in the cell of interest. Finally, we exploit nanoparticle-SEC interactions to demonstrate targeted intracellular drug delivery resulting in the selective deletion of a single blood vessel.

The identification of *stabilin-1* and *stabilin-2* as mediators in the uptake of anionic nanoparticles, and how to avoid such interaction, is an example of how the zebrafish embryos provides a new and powerful model system to study the mechanism that is required for the role in nanoparticle-mediated drug delivery.

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**Figure 1.** Schematic representation of liver endothelium in mice and zebrafish embryo. Nanoparticles endocytosed by receptor-mediated stab-1 and stab-2 or circulating in the absence/inhibition of stab-1 and stab-2. Modified from [1]

# Biodegradable nanofibers scaffolds containing platelet lysate for skin wound healing

### Andreu Blanquer<sup>1</sup>,

Elena Filova<sup>1</sup>, Eduard Brynda<sup>2</sup>, Johanka Kucerova<sup>2</sup>, Vera Jencova<sup>3</sup>, Barbora Koprivova<sup>3</sup>, Renata Prochazkova<sup>4</sup>, Lucie Bacakova<sup>1</sup>

<sup>1</sup>Institute of Physiology of the Czech Academy of Sciences, Videnska 1083, Prague, Czech Republic <sup>2</sup>Institute of Macromolecular Chemistry of the Czech Academy of Sciences, Videnska 104, Vestec, Czech Republic

<sup>3</sup>Technical University of Liberec, Studentska 1402/2, Liberec, Czech Republic <sup>4</sup>Regional Hospital Liberec, Husova 357/10, Liberec,

Czech Republic

andreu.blanquerjerez@fgu.cas.cz

The number of patients suffering from non-healing wounds is reaching epidemic proportions and it is estimated that 1-2% of the population will experience chronic wounds during their lifetime. The prevalence of chronic wounds increases along with vascular diseases and diabetes mellitus, and along with systemic factors such as advanced age [1]. Therefore, it is necessary to develop new drugs and medical devices to improve wound healing. In this scaffolds are nanofibrous promising regard, materials to regenerate the damaged skin, because they can act as a protective barrier against penetration of microorganisms, allow gas exchange, absorb the exudate and mimic the fibrous component of the extracellular matrix. On the other hand, platelet lysate (PL) has been considered to heal skin wounds due the accelerating effect of growth factors and bioactive molecules present in platelets [2]. In the study, polymeric scaffolds containing PL were developed as skin dressings with a controlled release of growth factors and bioactive molecules. Here, we show the in vitro effect of two types of biodegradable scaffolds on cell types involved in skin wound healing.

Both polymeric biomaterials, poly(vinyl alcohol) (PVA) and poly(L-lactide-co-ε-caprolactone) blend with poly-ε-caprolactone (PLCL/PCL), were fabricated by electrospinning in order to obtain a mesh of nanofibers. Two different strategies were used to assemble the PL according to the biodegradability of synthetic polymers. In the case of PVA, PL were introduced into the dissolvent to obtain PL-loaded nanofibers. In case of PLCL/PCL nanofibers, the nanmofibers were coated with fibrin assemblies together with PL.

Human keratinocytes (HaCaT), mouse fibroblasts (3T3) were cultured with nanofibrious scaffolds in Dulbecco's Modified Eagle Medium supplemented with 2% of fetal calf serum. Primary human saphenous vein endothelial cells were cultured in EGM-2 medium (Promocel) without growth factors. Cell metabolic activity was quantified on days 1, 3 (4), 7, and 14 days after seeding using MTS assay kit (Abcam). Cell migration was evaluated only for EC and measured by transmigration assay using Corning FluoroBlock cell culture inserts with the pore size of 8 µm. Cell differentiation were detected by immuno-fluorescence staining of specific markers. Basal cytokeratin 14 and differentiated cytokeratin 10 were analyzed for keratinocytes, whereas von Willebrand factor and platelet endothelial cell adhesion molecule (CD31) were analyzed for endothelial cells. For fibroblasts, type I collagen was analyzed.

For PVA samples, cell metabolic activity of keratinocytes, fibroblasts and endothelial cells was increased when PVA contained PL compared with pure PVA. In addition, images of cytokeratin 10 and 14 immunostaining on keratinocytes showed an increased number of differentiated cells positive for cytokeratin 10 on PVA containing PL. Cytokeratin 10 was detected on cells which grew on the upper layers in agreement with other authors that evaluated the presence of different types of cytokeratin according to the stratified layer of skin [3]. Endothelial cells were positively stained for von Willebrand factor and CD31. 3T3 fibroblasts started to produced type I collagen.

Similar results were obtained for PLCL/PCL scaffolds. The higher values of metabolic activity of keratinocytes and endothelial cells were observed on samples containing PL. The number of cells positively stained for cytokeratin 10 was higher on scaffolds with PL. Well-developed cytoskeleton of cytokeratin 10 and 14 can be observed in cells growing on samples (Fig. 1A). Endothelial cells staining for von Willebrand factor and CD31 indicated the presence of both differentiated markers (Fig. 1B). Moreover, endothelial cells migration towards the scaffold was significantly increased when samples contained PL.

The *in vitro* results indicate that both polymers could be considered as candidates for biomedical applications. However, the potential therapeutic application of each scaffold is different due to their physical and chemical properties and biodegradation rate. PVA nanofibers do not allow cells to migrate and grown on samples, so they can be used as dressing for wound healing. On the other hand, PLCL/PCL nanofibres could be used as scaffolds for skin regeneration with cells colonization.

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**Figure 1.** Immunofluorescence staining of cytokeratin 10 (green) and cytokeratin 14 (red) in HaCaT cells 14 days after seeding (A); and immunofluorescence staining of CD31 (green) in endothelial cells 7 days after seeding in medium with PLCL/PCL nanofibers scaffolds containing PL.

# Model membranes interfaced with optical tweezers: a versatile microfluidics platform for nanomanipulation and mechanical characterization

Aurora Dols-Perez<sup>1</sup>,

Guillermo J. Amador <sup>1,2</sup>, Victor Marin<sup>1</sup>, Roland Kieffer<sup>1</sup>, Daniel Tam<sup>2</sup> and Marie-Eve Aubin-Tam<sup>1</sup>

<sup>1</sup>Department of Bionanoscience, Kavli Institute of Nanoscience, Delft University of Technology. Van der Maasweg 9, Delft 2629 HZ, The Netherlands. <sup>2</sup> Laboratory for Aero and Hydrodynamics, Delft University of Technology, 2628 CD Delft, The Netherlands

### a.dolsperez@tudelft.nl m.e.aubin-tam@tudelft.nl

Membranes are the site of vital biological processes. such as sensing, communication and trafficking, involving many of them mechanical forces. But to elucidate the relationship between these membrane processes and mechanical forces it is required the use of tools able to apply and to measure picoNewton-level forces, like optical tweezers. Here, we introduce the combination of optical tweezers with free-standing lipid bilayers, which are fully accessible on both sides of the membrane [1]. In the vicinity of the lipid bilayer, optical trapping would normally be impossible due to optical distortions caused by pockets of solvent trapped within the membrane. We solve this by drastically reducing the size of these pockets via tuning of solvent and flow cell material. In the resulting flow cells, lipid nanotubes are pushed or pulled, and reach lengths above half a millimeter. Moreover, the controlled pushing of a lipid nanotube with an optically-trapped bead provides an accurate and direct measurement of important mechanical properties. In particular, we measure the membrane tension of a free-standing membrane composed of a mixture of DOPC and DPPC to be 4.6 x 10-6 N/m. We demonstrate the potential of the platform for biophysical studies, by inserting the cell-penetrating TAT peptide in the lipid membrane. The interactions between the TAT peptide and the membrane are found to decrease the value of the membrane tension to  $2.1 \times 10-6$ N/m. This method is also fully compatible with electrophysiology measurements, and presents new possibilities for the study of membrane mechanics and the creation of artificial lipid tube networks of great importance in intra- and intercellular communication.

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# Figures



**Figure 1.** Schematic representation of an optical tweezers (red) pulling a lipid nanotube from a free-standing lipid membrane. The system consists of an artificial lipid bilayer (yellow) assembled on a rectangular aperture (blue) allowing free access to both sides of the membrane.

# Lipid-composite particles by liquid-CO<sub>2</sub> cryospraying technology: advantages, challenges and pharmaceutical applications

### Pierandrea Esposito<sup>1</sup>

Hana Danan<sup>1</sup>, Jesús Caramés Bueno <sup>1</sup>

<sup>1</sup>SiTec PharmaBio , Carrer Baldiri Reixac 4-8, Barcelona (Spain)

p.esposito@sitec-pharmabio.com

In recent years, a new generation of CO<sub>2</sub>-based technologies has gained considerable interest in pharmaceutical and biotech industries, offering innovative, organic solvent-free, scaleable and economically viable solutions to address critical issues related to biopharmaceutical properties and drug product development.

Dense or liquid CO<sub>2</sub> has been applied in several processes as an atomization medium for the production of micro- and nanoparticles systems, by exploiting the thermal and mechanical properties of carbon dioxide rapid phase changes [1,2]. Variosol® cryospraying is one of these processes, based on the dynamic interaction between two spraved fluids in different thermodynamic conditions. A liquid or pasty fluid can be converted into a micro or nano solid by the combined thermodynamical sized (Joule-Thomson effect) mechanical and (atomization) actions resulting from liquid-CO<sub>2</sub> rapid expansion. These properties can be advantageously applied to several classes of excipients, especially lipids or lipids-polymers composite, facilitating in some cases the formation of eutectic blends at low temperatures. Applying appropriate operating conditions, CO<sub>2</sub> expansion allows to eliminate water during spraying at low Tº [3], thus making it possible to spray disperse systems, such as emulsions or microemulsions, to obtain very fine dry particles combining hydrophilic and hydrophobic materials in the same matrix.

Lipid-based formulations (LBF) offer nowadays a wide range of possibilities, from e.g. enabling drugs intestinal solubilization and absorption of oral products [4], to controlling drug release, or improving facilitating drug efficacy in dermal products, interaction with skin components. However, most LBF are liquid or semisolid at room temperature, which may present a disadvantage in terms of processability, product dosing stability. (e.g. necessity of soft gel capsules) and high production costs. In fact, the development of solid forms (especially micro- or nanoparticulates) has been the focus of recent innovation in the field of LBF [4].

The cryogenic effect obtained during liquid-CO<sub>2</sub> expansion can be used to process composites, containing excipients or active molecules in liquid form, and still obtain LBF as fine, solid

microparticles. The appropriate choice of materials and processing conditions are key factors to develop micronized and possibly nanosized LBFs for specific application such as improved drug solubilization and bioavailability, controlled or delayed release, drug stabilization, helping to address specific patients needs and targeting different routes of administration.

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Figure 1. Scheme of CO<sub>2</sub> cryospraying technology



**Figure 2.** Optical Microscopy Images of dry (a) and water-suspended (b) drug- containing microspheres

# Nano harvesting energy applied to cell biology

Carolina Vargas-Estevez<sup>1</sup>,

Gonzalo Murillo<sup>1</sup>, Andreu Blanquer<sup>1,2</sup>, Marcos Duque<sup>1</sup>, Lleonard Barrios<sup>2</sup>, Elena Ibañez<sup>2</sup>, Carme Nogués<sup>2</sup>, Jaume Esteve<sup>1</sup>

<sup>1</sup> IMB-CNM(CSIC), Campus UAB, 08193 Bellaterra, Spain <sup>2</sup> Departament de Biologia Cel·lular Fisiologia i Immunologia, UAB, 08193 Bellaterra, Spain

jaume.esteve@imb-cnm.csic.es

### Abstract

Our bodies are complex machines whose functioning depends on multiple electrical signals controlled mainly by the nervous system. Afterwards, it is not illogical to think that one day artificial electrical impulses would replace those signals offering support to medical treatments. Nowadays electrical stimulation is used in many therapeutic applications to modulate cellular activity, restore biological lost functions or even improve the performance of certain tissues. However, these systems still carry side effects link to the surgical interventions to place them or place their electrodes, their inherent bulkiness or lack in specificity to target only the cells involved in the condition to treat. The future to transcend these constrains would be possible in the extent that technology ease the path to improve precision, autonomy and miniaturization of the actual therapeutic tools. In this context, micro/nanogenerators play a key role as selfpowered devices with high spatial resolution and acute cell specificity.

This work aims to provide micro/nanogenerators to stimulate single cells in its own liquid media. This work explored two technological branches based on photovoltaic and on magnetoelastic (piezoelectric/magnetostrictive) devices to harvest energy. Their fabrication was accomplished through micro/nanosystems technologies and their performance was characterized through several tests to ensure their correct power generation. As these devices were intended to interface biological media, direct cytotoxicity studies were conducted to guarantee their safety. Both branches were biologically validated with in vitro models of excitable cells (human osteoblast-like cells) analyzing the electrostimulation effects through morphological changes and through instantaneous ionic responses as calcium signaling.

Here, we demonstrate that the interaction of human cells with piezoelectric nanogenerators (NGs) based on two-dimensional ZnO nanosheets (NSs) induces a local electric field that stimulate and modulate their cell activity. When cells were cultured on top of the NGs, the electromechanical NG-cell interactions stimulated the motility of macrophages and triggered the opening of ion channels present in the plasma membrane of osteoblast-like cells inducing intracellular calcium transients, (activated cells over 62%). In addition, excellent cell viability, proliferation and differentiation were validated [1,2,3].

We will present the technology for microphotodiodes fabrication and the characterization of single microphotodiode characteristics under in vitro conditions. We also demonstrate their capability to harvest energy from light and instantaneously convert it to an electric stimulus. These devices provide a stimulation tool of single cells without the limitation of external cables and electrodes. The electrical stimulation triggered intracellular calcium transients as a response in 46% of the cells. Furthermore, induction of cytosolic Ca2+ transients triggered by the electrical stimuli generated by the microphotodiodes, on which osteoblasts cells were grown, shows the feasibility of this approach towards localized activation of excitable cells in a simple way [4,5].

The results gathered in this research demonstrate the feasibility of these micro/nanogenerators as selfpowered electrical stimulators. Furthermore, their reduce size and capability to be suspended in liquid media open the door to further developments towards injected or ingested minimally invasive medical tools.

(Partial abstract from PhD Thesis of Carolina Vargas-Estévez, Universitat de Barcelona 2019).

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**Figure 1.** Morphology and NG-cell interaction, assessed by scanning electron microscopy showed that cells were firmly adhered to the nanosheets (NSs) [1]



Figure 2. Quantification of Saos-2 cells undergoing changes in Ca2+ concentration (activated cells). Asterisks above the columns indicate significant differences (Kruskal-Wallis test and  $\chi 2$  test) [1]



Figure 3. Fabrication process of suspended microphotodiodes [4]



Figure 4. SEM image of neuron with photodiodes attached to soma [4]



Figure 5. SEM image of Saos-2 cells growing on microphotodiodes array (PVMA). [5]



**Figure 6.** Percentage of activated Saos-2 cells on PVMA and on glass coverslip/bare silicon control for the same light stimulation. [5]

# "Three-Bullets" Loaded Mesoporous Silica Nanoparticles for Combined Photo/Chemotherapy

#### Aurore Fraix<sup>1</sup>,

André Luiz Tessaro<sup>1,2</sup>, Ana Claudia Pedrozo da Silva<sup>3</sup>, Elena Gazzano<sup>4</sup>, Chiara Riganti<sup>4</sup>, Salvatore Sortino<sup>1</sup>

<sup>1</sup> Laboratory of Photochemistry, Department of Drug Sciences, University of Catania, Viale A. Doria, 6, 95125 Catania, Italy,

<sup>2</sup>Department of Chemistry, Federal University of Technology – Paraná, R. Marcílio Dias, 635 - Jardim Paraíso, 86812-460, Apucarana, Paraná, Brazil <sup>3</sup>Department of Chemistry, Universidade Estadual de Maringá, Av. Colombo, 5.790, 87.020-900, Maringá, Paraná, Brazil.

<sup>4</sup>Department of Oncology, Via Santena 5/bis – University of Torino, I-10126 Torino, Italy.

#### fraix@unict.it

Multimodal cancer therapy involves the use of two or more treatment modalities with the aim to attack tumour on different sides by acting either on a single oncogenic pathway through different mechanisms or across parallel pathways without amplification of side effects.

In this frame, the combination of conventional chemotherapeutics with light-activated therapeutic treatments is revealing a very appealing approach to therapeutic outcome potentiate the through synergistic/additive anticancer effects. Liaht represents in fact as suitable and minimally invasive tool that permits the introduction of therapeutic species in biological environments with superb spatiotemporal control [1]. Among the light triggered therapeutic treatments, photodynamic therapy (PDT) is so far one of the most promising to combat cancer diseases [2]. This treatment modality exploits mainly the cytotoxic effects of the highly reactive singlet oxygen (1O2), catalytically generated by energy transfer between the long-lived excited triplet state of a photosensitizer (PS) and the nearby molecular oxygen.

Another emerging light-activated approach is based on the photoregulated release of nitric oxide (NO) through the use of NO photodonors (NOPD) [3]. Although still confined to the research area, this NObased PDT, namely NOPDT, has come to the limelight in recent years and holds very promising features in cancer treatment. In fact, apart from playing multiple roles in the bioregulation of a broad array of physiological processes, NO has also proven to be an effective anticancer agent [4]. If generated in an appropriate concentration range this diatomic free radical can act not only as a cytotoxic agent but also as inhibitor of the ATP Binding Cassette (ABC) transporters responsible of most chemotherapeutic efflux and inducing multidrug resistance (MDR) in cancer cells [5]. Noteworthy, both  ${}^{1}O_{2}$  and NO are multitarget species that has not a reduced efficacy in multidrug resistant cells due to their short lifetimes, confine their action to short distances from the production site inside the cells (< 20 nm for  ${}^{1}O_{2}$  and < 200 µm for NO), reducing systemic toxicity issues common to many conventional drugs. Besides, since NO photorelease is independent of O<sub>2</sub> availability, it may successfully complement PDT at the onset of hypoxic conditions, typical for some tumours, where PDT may fail.

The significant breakthroughs in nanomedicine permit nowadays the development of multifunctional platforms in which more therapeutic agents are entrapped in a single nanocarrier. This offers an unprecedented opportunity to devise a better scheme for precise and controlled delivery of multiple therapeutics in the same area of the body and at predefined extra/intracellular level. In this context, nanoplatforms combining PDT and NOPDT are opening new horizons towards more effective and less invasive cancer treatments entirely based "non-conventional" chemotherapeutics on [6]. increasing large Besides, an number of nanoconstructs in which PDT has been combined with chemotherapy in the management of several cancer types has been reported in literature [7]. In contrast. onlv recently NOPDT has been used in successfully combination with chemotherapeutics [8]. Based on this scenario, the achievement of a trimodal nanoplatform able to generate <sup>1</sup>O<sub>2</sub> and NO and, simultaneously, to deliver a conventional chemotherapeutic is a very challenging objective to pursue. Mesoporous silica nanoparticles (MSNs) as very suitable scaffolds to this end due to their high loading capacity, ease of surface functionalization, good biocompatibility and satisfactory light transparency. These inorganic scaffolds have been extensively used as excellent carrier for conventional drugs. Furthermore, it has been used as carrier for PDT agents alone and in combinations with chemotherapeutics, and recently our group demonstrated its versatility using MSNs as carrier for NOPD [9].

In this contribution, we report an engineered MSNs able to deliver "three bullets" for potential anticancer therapy. These MSNs covalently integrate in their molecular scaffold Erythrosine and a nitroaniline derivative as suitable PS and NOPD, respectively, and encapsulate the chemotherapeutic Doxorubicin (DOX) in a non-covalent fashion (figure 1) [10].

These MSNs bind the NOPD mainly in their inner part and the PS in their outer part in order to judiciously exploit the different diffusion radius of the cytotoxic NO and <sup>1</sup>O<sub>2</sub>. We demonstrate that the photochemical properties of the PS and NOPD are preserved in an excellent manner in the MSNs containing all active components. This silica nanoconstuct has been devised in such a way to permit the selective excitation of the NOPD and the PS with light sources of different energy in the visible range window. As a result, the spontaneous release of DOX under physiological conditions can be combined with the photoregulated generation of <sup>1</sup>O<sub>2</sub>, NO or both by using light stimuli of appropriate energy in the visible light range (figure 2).

Preliminary biological results performed by using A375 cancer cell lines expressing ABC transporters show a good tolerability of the functionalized MSNs in the dark and a potentiated activity of DOX incorporated in our "three bullets" nanoconstruct upon irradiation with blue light, due to the effect of the NO photoreleased.



**Figure 1.** Schematic for the "three-bullets" PS-MSNs-NOPD/DOX and their working principle.



Figure 2. A. Normalized absorption spectra in PBS (10 mM , pH 7.4) of NOPD and PS. B. Representative TEM image of the PS-MSNs.

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# Mesoporous silica nanoparticles as dual delivery platform for the efficient drug delivery and CRISPR-Cas9 editing machinery to one-shot treatments

**Alba García-Fernández**<sup>1,3,4</sup>, Gema Vivo-Llorca<sup>1,4</sup>, Mónica Sancho<sup>4,5</sup>, Alicia García-Jareño<sup>4,5</sup>, Félix Sancenón<sup>1,2,3,4</sup>, José Ramón Murguía<sup>1,3,4</sup>, Mar Orzáez<sup>4,5</sup> and Ramón Martínez-Máñez<sup>1,2,3,4</sup>

<sup>1</sup>Instituto Interuniversitario de Investigación de Reconocimiento Molecular y Desarrollo Tecnológico (IDM), Universitat Politècnica de València, Universitat de València. Spain.

<sup>2</sup>Departamento de Química, Universitat Politècnica de València, Spain.

<sup>3</sup>CIBER de Bioingeniería, Biomateriales y Nanomedicina (CIBER-BBN) Spain.

<sup>4</sup>Unidad Mixta UPV-CIPF de Investigación en Mecanismos de Enfermedades y Nanomedicina, UPV-CIFP, València Spain.

<sup>5</sup>Centro de Investigación Príncipe Felipe (CIPF), Laboratorio de Péptidos y Proteínas, València, Spain

algarfe4@etsia.upv.es

### Abstract

The new CRISPR-Cas9 technology has been established quickly as an easy genome-editing This system presents two method. main components; the non-specific CRISPR associated endonuclease (Cas9) and the guide RNA (gRNA). The Cas9 targets the specific sequence in the genome to be edited guided by the gRNA. The most extended CRISPR application is for knocking out genes, being a potential technology to correct genetic defects in diseases [1]. To take advantage of this technology in therapeutic applications, the development of carriers to deliver the CRISPR-Cas9 system efficiently to human cells represents an important challenge.

Among the delivery protocols to introduce the CRISPR-Cas9 into the cells, the current non-viral used methods are lipofection, microinjection and electroporation.

However, these protocols are complex to apply in in vivo settings and the use of nanoparticles for CRISPR-Cas9 efficient delivery has become a research area of great interest. At this respect, new methods deliverv has been described using nanomaterials based on polymers, lipid nanoparticles, peptides and cell-penetrating

inorganic nanoparticles to deliver the CRISPR-Cas9 machinery [2-4].

From another point of view, several studies showed the use of surface-functionalized mesoporous silica nanoparticles (MSNs) as an efficient and safe carrier for bioactive molecules [5]. Indeed, previous published works described the use of MSNs to deliver nucleic acids into the cells [6]. In this scenario, MSNs could be a potential platform for the efficient co-delivering of the CRSIRP-Cas9 technology, as well as, to deliver an entrapped payload at the same time.

Based on these premises, we described here a novel vehicle that simultaneously delivers the CRISPR-Cas9 technology and an entrapped cargo. As a proof of concept, we used MSNs to edit GFP in human cells and, simultaneously, deliver an entrapped dye. The MSNs were loaded with a dye and then its external surface coated with a polyethylenimine (PEI) layer. Finally, CRISPR-Cas9 adsorbed, through system is electrostatic the PEI layer. This interactions, onto work demonstrated the possible use of MSNs as dual platforms to gene editing and drug delivery. MSNs represent a potential tool in the preparation of advanced nanodevices for one-shot treatments to simultaneously edit genes and release drugs by double-hit strategies, in particular to combine synergistic therapies or to overcome drug resistance in tumours.

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**Figure 1.** MSNs for the efficient co-delivery of CRISPR-Cas9 editing machinery and an entrapped cargo.

# Mesoporous magnetic nanorods for theranostics

Jan Grzelak<sup>1</sup>, Martí Gich<sup>1</sup>, Anna Roig<sup>1</sup>

<sup>1</sup>Institut de Ciència de Materials de Barcelona (ICMAB-CSIC), Carrer dels Til·lers s/n, Campus de la UAB, Bellaterra (Barcelona), Spain

jgrzelak@icmab.es

### Abstract

The presented work involves developing mesoporous silica nanorods as a platform for production of multimodal agents for diagnostic and therapeutic purposes. The main aim is to demonstrate that such materials can exhibit improved properties compared to the current state of the art, mainly focused on spherical particles.

In this work mesoporous silica nanorods (Figure) have been synthesized and characterized in terms of size, shape, pore size and surface area. In a second step, silica was functionalized by inserting iron oxide nanoparticles into the pores by an in-situ method.

The magnetic properties of the silica nanorods have been investigated and their performance as MRI contrast agents has been studied.

Future work will focus on in vitro and in vivo performance tests as well as on using the nanoplatforms for ultrasound (US) imaging and computerized tomography (CT) imaging.

# References

# **Figures**



**Figure 1.** (Top) Scanning electron microscopy (SEM) image of mesoporous silica nanorods synthesized using a templated sol-gel method. (Bottom) Transmission electron microscopy (TEM) image of a silica rod filled with iron oxide nanoparticles.

# Polymeric NPs as efficient tool for gene delivery

Clara Guido<sup>1,2</sup>.

Stefania D'Amone<sup>2</sup>, Barbara Cortese<sup>3</sup>, Giuseppe Gigli<sup>1,2</sup> and Ilaria E. Palamà<sup>2</sup>

1 Dep. of Mathematics and Physics, University of Salento, via Monteroni, Lecce, Italy 2 Nanotechnology Institute, CNR-NANOTEC, via Monteroni, Lecce, Italy 3 Nanotechnology Institute, CNR-NANOTEC, Piazzale A. Moro, Roma, Italy clara.guido@nanotec.cnr.it; ilaria.palama@nanotec.cnr.it

clara.guido@nanotec.cnr.it; ilaria.palama@nanotec.cnr.it

#### Abstract

Gene therapy is described as the direct transfer of genetic material to cells or tissue for the treatment of inherited disorders and acquired diseases, such as cancer. The base of this therapeutic method is to introduce a gene encoding a functional protein altering the expression of an endogenous gene or possessing the capacity to cure or prevent the progression of a disease, or to introduce systems of gene silencing (such as siRNA, etc.) which has the ability to specifically silence target proteins that are crucial for modulating cellular pathways inducing an inhibitory effect on cancer proliferation. There are two types of gene delivery based on the carrier's nature: viral delivery and non-viral delivery. Gene delivery using viral vectors have long been proven to be the most efficient and stable transgene vectors into the cell. In addition, viruses are able to use the host cell machinery for protein synthesis, and some of them are able to stably insert into the host cell genome and provide a long-term transgene expression in transduced cells. Thus, viral gene carriers possess higher gene transfection efficiency than non-viral vectors. Despite some successes in clinic trials, viral vector gene transfer still has some safety issues. In order to limit the use of viral vectors, recent advances in vector technology have improved gene transfection efficiencies of non-viral carriers.

Nanoparticle (NP)-based therapeutic systems developed in recent years have shown efficient delivery of nucleic acids with low toxicity and sustained cargo release.

For gene delivery application, NPs can accommodate large DNA plasmids, RNA or proteins and may be produced at low cost on a large scale. NP-based systems overcome safety problems and limitations of viral vectors. FDA-approved polymers are particularly attractive for *in vivo* drug/gene delivery applications. Recently, we have developed a polymeric system for drug and gene based on pHresponsive and enzyme-responsive, core/shell NPs using the FDA approved PCL polymer [1-4].

Another, attractive polymer for gene delivery applications is polyglycolic acid (PGA), which has been approved by the FDA. PGA degradation is quicker *in vivo* and *in vitro*, and the degradation product, glycolic acid, is non-toxic and it can enter in the tricarboxylic acid cycle.

Our PGA NPs are obtained by nanoprecipitation and desolvation method, and are composed of a core

loaded with the acid nucleic molecules and a PGA shell. Prior to particle assembly, active agent is complexed with a pH (as chitosan) or enzymatic (as protamine)-responsive polymer. By combining the sensitivity of the core polymer with the slow degradation of surface PGA, we obtained a simple and easy way to control the release of an active agent and improve its therapeutic efficiency.

The mean size of PGA nanoparticles is 100 nm, with a negative  $\zeta$ -potential of -12 mV.

Our NPs have a regular spherical shape and no aggregation as observed by AFM and SEM analysis. No cytotoxicity is observed on different cell lines tested.

In addition, our PGA NPs have showed an efficient delivery of cDNA, observing relative numbers and mean fluorescence intensity of transfected GFPpositive cells comparable to those achieved with standard reagents used to promote transfection.

PGA NPs, thanks their properties, as biocompatibility, biodegradability and a good transfection efficacy, can be used as efficient tool of transfection overcome viral vector problems.

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# Complex skeletons for improved tracking and motion of 3D printed biorobots

#### Maria Guix <sup>1</sup>,

Rafael Mestre<sup>1</sup>, Giulia Zarpellon<sup>1</sup>, Tania Patiño<sup>1,2</sup>, Samuel Sánchez <sup>1,3</sup>

<sup>1</sup> Institute for Bioengineering of Catalonia (IBEC), The Barcelona Institute of Science and Technology, 08028, Barcelona, Spain

<sup>2</sup> University of Rome Tor Vergata, 00133, Roma, Italy <sup>3</sup> Institució Catalana de Recerca i Estudis Avançats (ICREA), Barcelona, Spain

mguix@ibecbarcelona.eu

Nano and microrobots has raised great interest for its potential applications in both environmental and biomedical applications, being traditionally divided in three main categories: synthetic, biological and hybrid microrobots.[1] Among them, biohybrid robots are being explored to exploit and implement some of unique inherent capabilities, their such as adaptability, self-assembly, self-healing, or response to an external stimuli.[2] The development of 3D bioprinting techniques revolutionized the field of advanced biorobots based on living tissues, being especially remarkable the versatility of such approach when cells are directly bioprinted in a rational shape to obtain a defined functionality.

In our specific case, our biological actuator based on skeletal muscle cells is combined with an advanced 3D printed compliant skeleton useful force tracking purposes (Figure 1). Skeletal muscle cells provide a controlled contractile behavior dependent on the applied electrical stimuli, being also of interest for their self-repair capabilities, which could lead to longer operative time in the resulting biobot.[3] On the other hand, a skeleton with a controlled stiffness and a spring-like structure useful for force tracking[4] has been integrated to obtain efficient motion and provide the required stiffness for the optimal cell The resulting biohybrid maturation. roboťs capabilities also depend on the performed training protocols, which are already been stablished in the group by applying electric pulse stimulation.[5] Currently, we are not only exploring the effect of such global stimulation, but also how actuation can be modulated by integrating flexible electrodes in the system able to apply local electric field.

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# Enzyme-powered nanomotors towards biomedical applications

### Ana C. Hortelão<sup>1</sup>,

Rafael Carrascosa<sup>1</sup>, Nerea Murillo-Cremaes,<sup>1</sup> Tania Patiño,<sup>1,2</sup> Samuel Sánchez<sup>1,3</sup>

<sup>1</sup>Institute for Bioengineering of Catalonia (IBEC), The Barcelona Institute of Science and Technology (BIST), Baldiri i Reixac 10-12, 08028 Barcelona Spain <sup>2</sup> Department of Chemistry, University of Rome, Tor Vergata, Via della Ricerca Scientifica 1, Rome 00133, Italy <sup>3</sup> Institució Catalana de Recerca i Estudis Avancats (ICREA), Passeig Lluís Companys 23, 08010 Barcelona, Spain

> ahortelao@ibecbarcelona.eu tpatino@ibecbarcelona.eu ssanchez@ibecbarcelona.eu

Bio-catalytic micro- and nanomotors are capable of self-propulsion in fluids due to the enzymatic conversion of substrates into products. 1,2 These structures have been focus of interest for biomedical applications, such as the active transport and delivery of cargoes to specific locations, as well as to modulate cell targeting and internalization phenomena. Here, we present fuel-dependent anticancer drug doxorubicin release and efficient delivery to cancer cells by urease powered nanomotors based on mesoporous silica nanoparticles,<sup>3</sup> as well as their potential to target bladder cancer cells in the form of 3D spheroids by anchoring anti-FGFR3 antibody on their surface. <sup>4</sup> We observed that these nanomotors propel in physiologically relevant fluids, such as PBS. Furthermore, we found a four-fold increase in anticancer drug doxorubicin release by nanomotors after 6 hours exposure to urea, compared to static particles. Moreover, active drug-loaded nanomotors present improved anti-cancer efficiency toward HeLa cells, which arises from a synergistic effect between enhanced anti-cancer drug release and generation of ammonia during bio-catalysis. We found that in the presence of urea, a higher content of anti-cancer drug is uptaken by cells after 1, 4, 6- and 24-hour incubations with active nanomotors, compared to static carriers. In addition, we anchored anti-FGFR3 antibody to the surface of urease-powered nanomotors to target 3D bladder cancer spheroids. These nanomotors are able to self-propel in both simulated and real urine. We observed that the internalization efficiency of antibody-modified nanomotors into the spheroids in the presence of urea was significantly higher compared with antibody-modified static particles or non-targeted nanomotors. Furthermore, cell proliferation studies indicated that targeted, active nanomotors induce

higher suppression of spheroid proliferation compared with non-targeted nanomotors, which could be due to a synergistic effect between the inhibition of the fibroblast growth factor pathway by anti-FGFR3 antibody and the local production of ammonia by the active nanomotors. Altogether, these results point towards the applicability of urease-powered nanomotors as tools for enhancing disease detection and simultaneous treatment, by combining improved drug release and targeting functionalities.

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# Nanomaterial Fate and Exposure Modelling

### Francisco Huertas<sup>1</sup>,

Carlos Fito<sup>1</sup>, Alfonso Gallo<sup>1</sup> and Arantxa Ballesteros<sup>1</sup>

<sup>1</sup>ITENE, C/ Albert Einstein, 1 (Paterna), Valencia, Spain

francisco.huertas@itene.com

Nanotechnology industry is a fast-growing field, but still there is not a robust legislation about how nanomaterials can affect the environment. Anticipating this need, the Biorima (BIOmaterial RIsk MAnagement) project aims at developing a reliable methodology for better risk management of engineered nanobiomaterials. We present here the fate and exposure models developed within the mentioned project.

The nanobiomaterials are engineered nanoparticles (ENP) specifically designed to interact with biological systems with a medical purpose - either in Advanced Therapy Medicinal Products (ATMP) or Medical Devices (MD).

Different fate and behavior models have been developed over the years, being SimpleBox4nano [1] and MendNano [2] two of the most representative ones. These models evaluate the nanomaterials fate from two different points of view: SimpleBox4nano is based on mechanistic formulations of the key processes, while MendNano is based on empirical partitioning of the data.

The fate model needs to know the estimated emissions as an input, coming from a Material Flow Analysis (MFA) in Biorima. As the project is based on the release of nanobiomaterials, they are liberated mainly to water via excretion, hospital waste or residuals, and accidental release. It is also needed to consider the properties of the nanobiomaterials (such as density or diameter), as well as the environmental variables (like mean temperature, volumes, diffusivities...).

From here, a full study of the fate and behavior of the nanoparticles has been done. The main approach is to calculate specific constants, such as removal and transport rates for each component, and use them to calculate the concentration of a nanobiomaterial over time. With the obtained data, it is also possible to calculate the Predicted Environmental Concentration (PEC). Figure 1 is a representation of the model.

Different processes have been taken into account: Sedimentation, resuspension, burial, dissolution and aggregation.

• Sedimentation as a transport process between water and sediment compartments,

modelled through a derivation of the Stokes' Law from gravitational settling of particles.

- Resuspension, which is the contrary process of sedimentation, involving the transport of the nanobiomaterial from sediment again to water.
- Burial is a removal process where the nanobiomaterial goes out of the system.
- Dissolution has been considered as a removal process in water and sediment compartiments. It depends on the surface of the particle and the chemical properties of the surrounding material. Noyes-Whitney equation has been applied.
- Both aggregation and attachment to larger particles have been also considered. It highly depends on collision frequencies which are described as a function of the particle size, density, number of concentrations of the particles present and characteristics of the surrounding material.

Biorima fate and behavior model implements all this information and starting from a particle emission, it can calculate the predicted environmental concentration and give it as an output of the model.

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Figure 1. Schematic diagram of the model

# Layer-by-Layer decoration of AgNPs with Aminocellulose and Quorum Quenching Acylase for Controlling Bacterial Pathogens and Their Biofilms

Aleksandra Ivanova<sup>1</sup>, Kristina Ivanova<sup>1</sup>, Thomas Heinze<sup>2</sup>, Tzanko Tzanov<sup>1</sup>

<sup>1</sup> Group of Molecular and Industrial Biotechnology, Department of Chemical Engineering, Universitat Politècnica de Catalunya, Rambla Sant Nebridi 22, 08222, Terrassa, Spain

<sup>2</sup> Center of Excellence for Polysaccharide Research, Institute of Organic Chemistry and Macromolecular Chemistry, Friedrich Schiller University of Jena, Humboldtstraße 10, 07743 Jena, German

aleksandra.asenova@upc.edu

The emergence of drug resistant bacteria and the failure of the existing therapeutics call for development novel antibacterial strategies. Furthermore, the inclusion of pathogens in highly organized biofilms causes difficult to treat infections and lead to poor treatment outcomes.<sup>1,2,3 4</sup> Whereas, the existing antimicrobials and the host immune response can eradicate the planktonic bacterial cells, they become inefficient once the cells establish biofilm structures that restrict the penetration of the antimicrobials. The process of biofilm formation is upon the phenomenon of cell-tocell communication, known as quorum sensing (QS).

Targeting QS systems in the pathogens is an emerging area of research due to the capability of the anti-QS agents to attenuate bacterial virulence and biofilm formation, making the cells more susceptible to the conventional drugs at lower concentrations. Interfering with bacterial QS may potentiate efficacy of the current antimicrobials lowering the risk of development of resistance.

Herein, we developed novel safe-by-design hybrid nano-entities of silver nanoparticles (AgNPs) decorated with layers of bactericidal aminocellulose (AC) and QS interfering enzyme acylase in a Layerby-Layer (LbL) fashion. The AC and acylase nanoshell enhanced the antibacterial activity of the AgNPs core towards the common Gram-negative pathogen *Pseudomonas aeruginosa*, lowering their minimum inhibitory concertation by 4-fold and prevented and eradicated the established biofilms with 8-fold lower AgNPs concentration. These nanosized hybrid entities were able to inhibit QS process by 45% and eliminated the drug resistant biofilms of *P. aeruginosa* from a model surface (Figure 1). Moreover, the surface modification of the AgNPs improved its biocompatibility and did not affect the viability the morphology of human fibroblast cells. In border context, the developed novel NPs could be a promising alternative to combat difficult-to-treat bacterial infections, without creating selective pressure for resistance development.

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# Acknowledgments

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Figure 1. Schematic representation of LbL decorated AgNPs and their exposure to mature biofilms

# Characterisation of key bionano interactions between organosilica nanoparticles and *Candida albicans*

Vidhishri Kesarwani<sup>1,3</sup>, Hannah G. Kelly<sup>2</sup>, Madhu Shankar<sup>3</sup>, Kye J. Robinson<sup>1</sup>, Stephen J. Kent<sup>2</sup>, Ana Traven<sup>3\*</sup>, Simon R. Corrie<sup>1\*</sup>

<sup>1</sup>Department of Chemical Engineering, Monash University, Clayton, Victoria, 3800, Australia, ARC Centre of Excellence in Convergent BioNano Science and Technology

<sup>2</sup>Department of Microbiology and Immunology, Peter Doherty Institute for Infection and Immunity, The University of Melbourne, Melbourne, Victoria 3010, Australia, ARC Centre of Excellence in Convergent BioNano Science and Technology

<sup>3</sup>Infection and Immunity Program and the Department of Biochemistry and Molecular Biology, Biomedicine Discovery Institute, Monash University, Clayton, Victoria, 3800, Australia.

### vidhshri.kesarwani@monash.edu

Candida albicans (C. albicans), a commensal microorganism in healthy individuals, is capable of causing life-threatening infections in immunocompromised patients. Known as the fourth most common hospitable-acquired pathogen, many of these infections are caused by drug-resistant biofilms on implantable devices such as a catheter, which are difficult to treat and diagnose [1, 2]. Mortality rates from systemic infections are between 10-47% despite the availability of antimicrobial therapy and current diagnostic measures [3]. Hence, novel materials need to be explored for the development of new therapeutic, diagnostic or theranostic tools in an effort to combat nosocomial infections caused by C. albicans.

Fundamental interactions between mammalian cells and silica nanoparticles focusing on cytotoxicity, cell association and imaging have been investigated for applications such as drug delivery, diagnostics and imaging [4]. While it is widely accepted that a range of inorganic nanoparticles including silver, gold and zinc oxide are inherently cytotoxic to microbial cells [5], the bio-nano interactions between silica nanoparticles and pathogenic fungi have not been well characterised.

In this study, we investigated the interactions between C. albicans and organosilica nanoparticles, which are highly tuneable and coated with the antifouling polymer, PEG, to provide an additional functional handle for drug conjugation. We found that size and PEGylation of the nanoparticles had minimal effect on the growth and viability of C. albicans. Yet, association between the nanoparticles and the pathogen was found to be size and concentration-dependent. We then employed a whole blood assay to further study how PEGylated organosilica nanoparticles of different sizes and concentrations associate with human immune cells, which are the first cell types nanomaterials are likely to encounter in vivo or during an infection. This provided us with an insight into the likely behaviour of the nanoparticles in vivo. Lastly, we attached the clinically relevant drug, caspofungin, on the surface of PEGylated nanoparticles to switch the surface interactions between C. albicans and organosilica nanoparticles from benign to antifungal, without impacting the viability of primary human neutrophils. Our results illuminate how organosilica nanomaterials could be used as scaffolds for designing biomaterials for detecting or preventing C. albicans infections.

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**Figure 1.** SEM image of ~800 nm PEGylated organosilica nanoparticles associating with *C. albicans.* Scale bar represents 5µm.

# Collagen at the solid/liquid interface: Self-assembly, supramolecular organization and interaction with inorganic nanoparticles

### Jessem Landoulsi<sup>1</sup>,

T. Degabriel<sup>1</sup>, E. Colaço<sup>2</sup>, M. Beauvais<sup>3</sup>, N. Aissaoui<sup>4</sup>, V. Dupres<sup>5</sup>, K. El Kirat<sup>2</sup>, D. Brouri<sup>1</sup>, J.-F Lambert<sup>1</sup>, C.-M. Pradier<sup>1</sup>, J. Spadavecchia<sup>1</sup>

<sup>1</sup>Sorbonne Université, CNRS - UMR 7197, LRS, 4 place Jussieu, F-75005, Paris, France. <sup>2</sup>UTC, BMBI, CNRS, UMR 7338, F-60205 Compiègne

France. 3 Alcatel-Lucent Bell Labs France, 7 route de Villejust,

91620 Nozay, France

<sup>4</sup>CIC biomaGUNE, Paseo Miramon 182, 20009 Donostia-San Sebastian, Spain

<sup>5</sup>Cellular Microbiology and Physics of Infections – Lille Center for Infection and Immunity, Institut Pasteur de Lille-CNRS UMR 8204-INSERM U1019-CHRU Lille, University of Lille, Lille, France

Jessem. landoulsi@sorbonne-universite. fr

Collagen is the most abundant structural protein in mammals, located in the extracellular matrix (ECM) of connective tissues. In vivo. collagen molecules have an outstanding ability to self-assemble and to interact with other entities to form highly organized networks surrounding cells as in hard 3D biomineralized tissues, cartilage, tendon, and skin. These architectures provide a physical support to cells and serves as transducer for biochemical signaling. Collagen is also one of the most common proteins used for the design of biomimetic materials with broad applications in drug delivery and tissue engineering. In vitro, collagen plays a pivotal role to mediate cell-material interaction during in vitro tests. It is, indeed, frequently adsorbed to cell culture substrates to provide a protein coating for cell attachment, as cells lose their normal ECM environment.

Nanostructured collagen layers may be obtained at solid/liquid interface by adjusting the adsorption procedure, the characteristics of the medium (pH, temperature, composition and ionic strength), the properties of the substrates (wettability, surface charge, topography) and collagen conformational states (triple-helix or random coil) and fibrillogenesis [1]. Even so, the self-assembly and organization of collagen at solid/liquid interface remain difficult to predict.

Understanding the behavior of collagen at solid surfaces requires coping with the complexity of the interfaces. Herein, examples are given to illustrate key considerations in situations of biomedical interest: (i) Mechanism of interaction with spheroid- and rod-shaped TiO<sub>2</sub> nanocrystals. These nanoparticles have, indeed, been the subject of a vast literature regarding their toxicity and their interaction with proteins impacting cell behavior [2], their rods being explored for enhanced photocatalytic properties, however with possible consequence on particle aggregation [3]. In solution, results show that nanoparticles do not alter the conformation of collagen (triple-helix), and slightly delay the kinetics of its fibrillogenesis. By contrast collagen layer is strongly impacted by the presence of nanoparticles in the medium (Figure 1, top).

(ii) Mechanism of interaction with hydroxyapatite (Hap) nanoparticles. А comprehensive understanding of this mechanism is a pivotal step for design of biologically relevant quiding the nanocomposites with controlled hierarchical structure. By using a variety of Hap nanoparticles differing by their shape (rod vs platelet) and their size (~30 vs ~130 nm), we showed that collagen strongly interacts with rod-shaped nanoparticles while only a weak effect was observed with platelets. Interestingly, the use of small rods, typically with ~30 nm of length, leads to the formation of assembled collagen fibrils decorated with Hap nanocrystals which, in turn, self-assemble progressively to form larger fibrillar composite (Figure 1, bottom). Through this study, we showed the possibility to design hierarchical collagen-hydroxyapatite nanostructures which may be relevant for various medical applications.

(iii) Methodological development for probing collagen layers both in the dried and hydrated phases. This includes AFM imaging, force spectroscopy, QCM-D, etc. In particular, we developed a powerful yet straightforward method to exploring the dewetting patterns of the collagen layers using AFM imaging. The method allows the extraction of quantitative parameters describing the collagen networks: density and degree of nodes, area and distribution of holes, physical distance between nodes, etc (Figure 1, top). We showed that information obtained from AFM imaging are consistent with the analysis of the protein layers in the hydrated state, regarding the elastic compliance of the film, i.e. its softness (data from QCM-D), the surface density of fibrils and their "length" (data from AFM force spectroscopy). This constitutes a step forward toward reconciling disparate views of collagen layers' characterization in the dried state and in the liquid phase.

The approaches described here offers new perspectives to examine the interactions between collagen and inorganic nanoparticles at the solid/liquid interface, particularly at the stage of *in vitro* cell culture.

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**Figure 1.** (Top) Schematic representation describing (i) the supramolecular organization of collagen on PS-coated substrate in the hydrated and the dried state in solution containing  $TiO_2$  nanoparticles and (ii) network extraction from AFM images of collagen layers with the degree of nodes (blue = 1; grey = 2; red > 2). (Bottom) AFM height image showing the formation of collagen-hydroxyapatite composite, and well-defined collagen fibrils (see arrows) remain clearly visible.

# Control of particle size and drug release of PLA/PLGA microspheres

#### Albert Lorenzo Sanz<sup>1</sup>,

Gemma Sanjuan Gómez<sup>1</sup>, Manuel Jose Lis Arias<sup>2</sup>, Vanesa Martínez Rodríguez<sup>1</sup>

<sup>1</sup>The Forest Next S.L., Prat de la Riba 88, Terrassa, Spain <sup>2</sup>ESEIAAT-UPC, Colom 1, Terrassa, Spain

alorenzo@theforestnext.com

Poly (D,L-lactic-co-glycolic acid) (PLGA) and poly (lactic acid) (PLA) are well known by its biocompatibility and biodegradability in biomedical solutions [1]. The PLGA/PLA microspheres are one of the most successful drug delivery systems (DDS) in lab and clinic [2]. In the present study, microspheres based on blend of PLGA and PLA with ibuprofen as drug and with poly(vinyl alcohol) as emulsifier were prepared by a developed double emulsion oil-in-water-in-water solvent evaporation method and characterized. The blend of PLA and PLGA is formed only by physical interactions between them. This can be seen from the FTIR spectrum which shows both PLA and PLGA component (Figure 1). The effect of added surfactant, PVA [poly (vinyl alcohol)] and PLA/PLGA concentration and emulsion speed stirring on the size of the resultant PLGA/PLA microspheres has been studied. Ibuprofen release profile from PLGA/PLA microspheres with PVA as emulsifier within a phosphate buffer solutions (PBS) is determined and compared to drug release profile of microspheres with different concentrations of PLGA and PLA. This experiment involves the use of PBS as the release medium to regulate the drug release. It was prepared using 0,2 M monobasic and 0,2 M dibasic sodium phosphate to achieve pH 7.4 at 37 °C [3]. A centrifugation process followed by a drying process at 40 °C during 4 h was carried out to obtain microspheres ready for drug release experiments. The PLA/PLGA microspheres were characterized by Zeta-sizer Nano ZS to assess their size. FT-IR analysis was used to assess the functional groups present in the PLA/PLGA microspheres. SEM was used to observe the shape and to corroborate the microspheres formation. Thermogravimetric analysis (TGA) was performed from 30 to 700 °C under nitrogen atmosphere on ibuprofen, PLA/PLGA microspheres-Ibuprofen, PLA/PLGA microspheres-Ibuprofen after the drug release experiment in PBS media and PLA/PLGA without ibuprofen. It was found that the particle size of microspheres could be easily controlled by varying the different parameters ([PVA], [PLA/PLGA] and emulsion speed stirring). It was also proved that drug release could be controlled by varying the particle size. Figure 2 shows the variability of the size distribution with different emulsion speeds (12.000 and 16.000 rpm). Likewise, the comparation of the size distribution by

varying the PVA and PLA/PLGA concentration were studied. The overall results of this study showed that the formula using 25 wt.% PLA and 75 wt.% PLGA, 1% w/v of PVA and 12.000 rpm of stirring speed produced the microspheres with the most uniform size distribution of 450-550 nm. Figure 3 shows drug PLA/PLGA-Ibuprofen release profiles determined by UV-Vis spectroscopy. Three types of microspheres were prepared for this study by the same method but with different concentrations of PLA and PLGA. Results indicate that if the size distribution is controlled, better release profiles are obtained. The microspheres with the most uniform size distribution (25 wt.% PLA and 75 wt.% PLGA, 1% w/v of PVA and 12.000 rpm of stirring speed) exhibit lower release rate achieving its full release at about 60 min. Instead, the drug release profile of 50 wt.% PLA and 50 wt.% PLGA microspheres and 75 wt.% PLA and 25 wt.% PLGA microspheres, which have a worse size distribution, achieve its full release at about 10 and 15 min, respectively. In Figure 4, first derivative of TGA (DTG) was applied to obtain degradation curves, which state that after drug release, the ibuprofen degradation stage disappears, which indicates that drug release was completed while PLA/PLGA microspheres with PVA remains stable and exhibits a similar curve to blank PLA/PLGA microspheres. Figure 5 shows the SEM images of PLGA/PLA microspheres with ibuprofen after the drug release experiment in PBS media and the blank PLGA/PLA microspheres, which help us to corroborate that PLA/PLGA microspheres with PVA remains stable after the drug release.

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Figure 1. FTIR of PLA/PLGA microspheres

**Figures** 



Figure 2. Comparation between the size distribution of two similar PLA/PLGA microspheres with different emulsion speed stirring. (A) 16.000 rpm. (B) 12.000 rpm.



**Figure 3.** Comparation between the ibuprofen release profiles of PLA/PLGA microspheres with different PLA and PLGA concentrations. **(A)** 25%PLA and 75%PLGA. **(B)** 75%PLA and 25%PLGA. **(C)** 50%PLA and 50%PLGA.



Figure 4. DTG of Ibuprofen, PLA/PLGA microspheres-Ibuprofen, PLA/PLGA microspheres-Ibuprofen after drug release experiment in PBS media and blank PLA/PLGA microspheres.



**Figure 5.** SEM image of blank PLGA/PLA microspheres (left) and SEM image of PLGA/PLA microspheres with ibuprofen after the drug release experiment in PBS media (right).

# Magnetite Nanoparticles a Key player in Alzheimer's Disease

Mònica Mir<sup>1,2,3\*</sup>

Josep Samitier

<sup>1</sup> Centro de Investigación Biomédica en Red en Bioingeniería, Biomateriales y Nanomedicina (CIBER-BBN), Monforte de Lemos 3-5, Pabellón 11, 28029 Madrid, Spain

<sup>2</sup> Nanobioengineering group, Institute for Bioengineering of Catalonia (IBEC) Barcelona Institute of Science and Technology (BIST), 12 Baldiri Reixac 15-21, Barcelona 08028, Spain

3 Department of Electronics, University of Barcelona, Martí i Franquès 1, 08028 Barcelona, Spain

mmir@ibecbarcelona.eu

### Abstract

The accumulation of iron in form of magnetite nanoparticles with amyloid peptide is a key process in the development of Alzheimer's disease (AD) [1]. However, the origin and role of magnetite inside the AD brain is still unclear [2].

We have investigated the interaction between these important players in AD with superconducting quantum interference, scanning electron microscope, surface plasmon resonance, and magnetic force microscopy [3]. The results support the notion that the magnetite-Amyloid  $\boldsymbol{\beta}$  complex is created before the synthesis of the magnetic nanoparticles, bringing a highly stable interaction of this couple. The capacity of amyloid peptide to bind and concentrate iron hydroxides, the bases for the formation of magnetite, benefits the spontaneous synthesis of these nanoparticles thanks to the catalysis of amyloid peptide [4]. This symbiotic interaction between amyloid and magnetite helps in the Fe2+ stabilization as well contributes to the aggregation of amyloid monomers to fibrils. A neuronal culture model was used to monitor the changes in spontaneous activity and effective connectivity in amyloid-magnetite affected cultures. The activity of controls was compared in parallel with magnetite, amyloid and magnetite-amyloid complex. A clear spontaneous degradation of neuronal activity is only observed with the amyloid-magnetite dose, disrupting neuron network communities [5].

Our results demonstrate that magnetite nanoparticles have a more prominent role in this disease, than the previously assigned in the literature, which could help in a better understanding of this neurodegenerative disease and in the development of new AD treatments.

Single-spaced and a single paragraph

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### **Figures**



Figure 1. Image from Magnetic Atomic Force Microscope of Amyloid fibril grown up with the generated magnetite nanoparticles [3]

# Polyethyleneimine as a versatile coating/reducing cationic polymer for metallic nanoparticle-based cancer theranosis

<u>Vladimir Mulens-Arias</u><sup>1\*</sup>, José Manuel Rojas Carrasco<sup>2</sup>, Alba Nicolás-Boluda<sup>2</sup>, Sonia Pérez-Yagüe<sup>1</sup>, María del Puerto Morales<sup>3</sup>, Alice Balfourier<sup>2</sup>, Florence Gazeau<sup>3\*</sup>, and Domingo F. Barber<sup>1\*</sup>

<sup>1</sup>Nanomedicine, cancer immunotherapy and autoimmune diseases, Department of Immunology & oncology, National Center for Biotechnology, Darwin 3, Campus Cantoblanco, 28049, Madrid, Spain; <sup>2</sup>Laboratoire Matière et Systèmes Complexes, UMR 7075, CNRS & Université Paris Diderot, 10 Rue Alice Domon et Léonie Duquet, 75205 Paris Cedex 13, France; <sup>3</sup>Institute for Material Science of Madrid, Sor Juana Inés de la Cruz 3, Campus Cantoblanco, 28049, Madrid, Spain

E-mail vladimirmascience@gmail.com

Polyethyleneimine has been long known for its efficient DNA/RNA molecule delivery intracellularly due to the so-called 'sponge effect'. However, the potential of PEI as coating and reducing agent in nanoparticle synthesis/stabilization and its implication in nanomedicine in terms of intrinsic biological activities has only been addressed in the last years. Within this scenario, we have thoroughly characterized the chemical, physical, and biological contributions of PEI when coating iron oxide and gold nanoparticles. First, we studied the biological implications of the polymer as coating layer of superparamagnetic iron oxide nanoparticles (SPIONs) by assessing the effect that PEI-coated SPIONs have on mononuclear cells (macrophages), tumor cells, and endothelial cells [1-2]. PEI-coated SPIONs activated macrophages (pro-inflammatory pro-inflammatory cytokine secretion, gene expression, cytoskeleton modulation) mediated by TLR-4 engagement and ROS production, as proinflammatory response was inhibited when macrophages were pre-treated with TLR-4 inhibitor and ROS scavengers. In addition, PEI-coated SPIONs skewed endothelial cells gene expression profile toward an activated status. Surprisingly, PEI-coated SPIONs also exhibited anti-migratory effect on

pancreatic tumor cells by modulating invadosome dynamics and, thereby, extracellular degradation ability, altogether suggesting an anti-metastatic potential [3]. Likewise, PEI-coated SPIONs impaired endothelial cell migration and invasion by affecting cytoskeleton dynamics, both in vitro and in vivo, suggesting their use as anti-angiogenic agent in cancer therapy. We then characterized the potential of the cationic polymer as a template for Au<sup>3+</sup> reduction into gold nanoparticles (AuNPs) with a promising theranostic potential for colon carcinoma treatment [4]. PEI did also proved efficient in reducing and further stabilizing colloidal gold nanoparticles (AuPEI) into guasi-fractal nanoassemblies. These quasi-fractals showed a good plasmon-coupling facilitating NIR photothermal therapy and photo-acoustic imaging of colorectal carcinoma. In summary, PEI proved to be a versatile and promising tool in cancer therapy endowing metallic nanoparticles with intrinsic properties, e.g., anti-migratory/invasion, pro-inflammatory, and anti-angiogenic features.

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Figure 1. Synthesis routes for polyethyleneimine-based iron oxide and -gold nanoparticles and their exploitation in cancer theranosis

# International nanomaterials for biomedicine projects reaching success with support of EU Research and Innovation Staff Exchange (RISE) programme

### Dr. Amanda Jane OZIN-HOFSAESS<sup>1</sup>

<sup>1</sup>Research Executive Agency, Brussels, Belgium

amanda.jane-ozin.hofsaess@ec.europa.eu

### What is MSCA and what is RISE?

The Marie Skłodowska-Curie Actions (MSCA) are part of Horizon 2020 (H2020), the European Union's Framework Programme for Research and Innovation (2014-2020).

The **MSCA** support researchers in all scientific domains, promote collaboration between the academic, scientific and business communities, boost the careers of scientists at all stages and develop excellent doctoral training in Europe and beyond through international and intersectoral mobility.

The current budget (2014-2020) under Horizon 2020 is 6.2 billion euro and represents around 8% of the overall H2020 budget. Since 1994, the programme has trained around 130,000 researchers — including 35,000 doctoral candidates —throughout their career [1].

RISE stands for "Research and Innovation Staff Exchange" and it is part of the Horizon 2020 family of **MSCA**. The budget for the next call (opening Dec 5<sup>th</sup>, 2019) is set for 80 million Euro.

### What does RISE offer?

RISE funds short-term international and intersectoral exchanges of staff members involved in research and innovation to develop sustainable collaborative projects between different organisations. It helps people develop their knowledge, skills and careers and ensure the transfer of knowledge.

RISE enables staff mobility and also contributes in a flexible way to research and administrative costs. The administration is quite simple for our coordinators as the programme works by "unit costs" (Figure 1).

### Who applies?

International networks of research organisations from the academic and non-academic sectors.

A RISE consortium consists of at least three independent participants in three different countries

(two must be EU Member States or Associated Countries).

### Who is funded?

Researchers, technical administrative and managerial staff of the participating organisations, of any nationality and at all career levels.

### What type of research project proposals?

The work can be basic research and/or applied research leading to publications, patents, software tools, training materials, prototypes ready for market, etc....

Exchanges (secondments) are open to all countries and nationalities. Within Europe, the special feature of RISE is that exchanges eligible for funding need to be between academia and industry.

Proposal applications are made within one of eight specific panels (i.e. Physics, Mathematics, Life Science, Engineering, Chemistry, and Economic and Social Sciences).

Within the research projects proposals the applicants also show how their work will meet the more general objectives of MSCA and RISE [1]

### Which types of organisations?

All organisations involved in research and innovation activities, academic and non-academic (e.g. SMEs, NGOs, museums, hospitals, etc.), are potential participants.

RISE funds exchanges of research staff between academic and non-academic organisations (intersectoral secondments) and between EU Member States / Associated Countries and other organisations located in the rest of the world (international secondments). The projects are normally lasting 4 years with a maximum number of exchanges of ~540 person months (~2.5 million EUR).

# Examples of Success Stories in field of nanomaterials and biomedicine?

Three recently funded MSCA-RISE projects [2-4] will be highlighted in the presentation. The projects are in under the "Physics" panel and focus on nanomaterial applications in biomedicine (dental implants and cancer detection and therapies). The consortia consist of ~33 organisations from Austria Czech Republic, Estonia, France Italy, Latvia, Lithuania, Poland, Spain, Portugal, United Kingdom, Argentina, Chile, Belarus, Brazil, Ukraine, United States. One third of these organisations are SMEs.

The science is exciting! From the perspective of the Marie Sklowdowska-Curie programme what is also important about these projects is the difference they make to the career development of the researchers involved and the special collaborations between
industry and academia, within Europe and across the globe.

These projects are a proof of concept that innovation comes from mobilizing scientists between countries, between sectors, and between the fields of physics, chemistry, biology, and medicine.

#### How to apply?

Submit your application in response to a call for proposals through the Funding & Tenders Portal – where you will find the Work Programme and the Guide for Applicants. Designated National Contact Points are there to support you to make a successful application [6]

#### Discussion for NanoBio&Med participants

In this presentation, Dr. Ozin-Hofsaess – MSCA RISE Research Programme Administrator/ Panel Coordinator for Physics and Mathematics projects will share her experience working with these scientists to reach their goals and the aims of the MSCA RISE programme.

She will inform and inspire the audience how they can make a strong application in the next and last RISE call - *opening Dec 5<sup>th</sup> and close date April 28<sup>th</sup>, 2020* - of the programme as part of the Horizon 2020 framework programme of the European Commission.

Also the other MSCA opportunities for funding (Figure 2). A preview of what is in store for RISE in the next framework programme, Horizon Europe, will also be presented.

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- [6] National contact points https://www.net4mobilityplus.eu/msca-ncp/

### **Figures**



**Figure 1.** Summary of budget for MSCA RISE projects. For each month that the researcher staff is mobilized they received funds for travel/accommodations, research, training, and networking and also management overheads.



**Figure 2.** The MSCA are highly relevant and attractive, as shown by a growing number of high-quality proposals. However, many cannot be funded due to a lack of funding: proposals submitted under Co-funding of Regional, National and International Programmes; Research and Innovation Staff Exchange and European Researcher's Night are most likely to be funded, whilst there is a high demand for Individual Fellowships and Innovative Training Networks [1].

# 3D multiplex, paper-based rapid diagnostic tests using plasmonic gold nanoprobes

#### Tomás Pinheiro<sup>1</sup>,

Ana C. Marques<sup>2</sup>, Patrícia Carvalho<sup>2</sup>, Rodrigo Martins<sup>1</sup> and Elvira Fortunato<sup>1</sup>

<sup>1</sup>CENIMAT|i3N, Departamento de Ciência de Materiais, Faculdade de Ciências e Tecnologia, Universidade NOVA de Lisboa and CEMOP/UNINOVA, Campus da Caparica, 2829-516 Caparica – Portugal <sup>2</sup>SINTEF Materials and Chemistry, PB 124, Blindern, NO-0314, Oslo, Norway

tp.pinheiro@campus.fct.unl.pt

#### Abstract

Plasmonic properties of gold nanoparticles are a promising tool to develop sensing alternatives for the traditional, but disadvantageous, enzyme catalyzed reactions and other biological recognition elements in biosensors. The need for sensing alternatives, especially in under developed areas of the world, has given rise to the application of non-enzymatic sensing and quantification approaches to biochemical analysis. Because of environmental and cost disadvantages of enzymatic reagents, metallic nanoparticles, with higher focus on the gold ones, have been synthesized and modified with the purpose of achieving sensitive probes for relevant health biomarkers over the years. The integration of these new recognition elements into versatile platforms, such as paper, gives the opportunity for the development of new, easy-to-use, low-cost, sustainable diagnostic tools. More specifically, the pairing of paper ufluidics and gold nanoparticles is a promising approach for the development of point-ofcare devices, which can be used together with information technologies, such as smartphone embedded cameras and cloud computing, to develop complete systems to be used in under developed areas, for various health applications. Here, we present three individual, low-step, wetchemistry assays, for each of the target health markets (free cholesterol, glucose and uric acid), and the fabrication and calibration of a µfluidic, multiplex, paper-based device, to serve as a platform for said assays. We found that the optical properties of differently produced AuNPs are influenced by the presence of the target analytes, by changes in size, conformation and interparticle distance, both in colloidal gold mixtures and in AuNPs immobilized in a chromatography paper substrate. The direct influence of glucose, in different quantities, towards the reduction of a gold salt, in alkaline medium, is used as a sensing approach [1], while for uric acid and cholesterol sensing, the introduction of molecules with thiol for surface modification moieties, and functionalization, was the approach. The use of

digitonin [2] and 2-thiouracil (2-TU) [3], which present affinity towards cholesterol and uric acid, respectively, allows us to tune optical properties of AuNPs, depending on analyte concentration. In the case of glucose and uric acid, the interaction between nanoparticles and increased concentrations of the analytes cause a blue-shift, related to diminishing sizes of AuNPs, resulting in optimal sensitivity ranges of measurement (1.25 - 50 mM for glucose, 0 - 5 mM for UA, both including the clinical measuring range), while for cholesterol, interactions produce an increase in interparticle distance and consequent decrease of optical density. UV-Vis spectrophotometry, dynamic light scattering (DLS) and transmission electron microscopy (TEM) were used to determine the influence of the biomolecules in the plasmonic properties of AuNPs and the changes in size and conformation, in addition to applying Raman spectroscopy and other characterization techniques to study AuNP properties.

The studied AuNPs were posteriorly translated to the chromatography paper substrate, by two different approaches, for the creation of lab-onpaper applications: (i) consecutive deposition of reagents for direct synthesis of AuNPs into the paper substrate (for glucose sensing); (ii) direct deposition of surface modified and functionalized AuNPs, to serve as gold-based probes (for free cholesterol and uric acid sensing). We found that for the sensing of glucose, direct synthesis of AuNPs result in increasing color intensity of pink/red AunPs, because different amounts of particle are produced. This color intensity can be correlated to glucose concentrations, using digital, colorimetric calibration employing different color spaces, mainly RGB. For uric acid sensing, 2-TU functionalized AuNPs deposited into the paper substrate are influenced by the introduction of UA by color change indicative of anti-aggregation effects (from blue/purple to red), resulting in digital color calibration with a linear correlation and a sensitivity range between 71/87.5 µmol/L (depending on the color space used for calibration) and 1 mmol/L, which includes the clinical range of measurement. For cholesterol sensing, digitonin functionalized AuNPs (DAuNPs) interact with cholesterol in the paper substrate, to cause a decrease in color intensity, correlated to cholesterol concentrations using the HSV color space.

With the purpose of developing a platform to host the paper-based, colorimetric assays, a µfluidic, multiplex device is presented, for simultaneous, multiparametric sensing of the target health markers, resulting in a low-cost, low-complexity tool for diagnostics in low-resource areas of the world.

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Figure 1. Real-size image of paper-based, 3D multiplex platform for screening of glucose, cholesterol and uric acid.



Figure 2. Schematic Illustration for assembly and operation of 3D  $\mu\text{PAD}.$ 



Figure 3. Paper-based assay of uric acid colorimetric behavior and color calibration.

# Ultra-sensitive and multiplexed detection of protein biomarkers using Mecwins technology

**V. Pini**<sup>1</sup>, A. Thon<sup>1</sup>, V. Cebrián<sup>1</sup>, A. Salvador-Matar<sup>1</sup>, C. Rodríguez<sup>1</sup>, A. Diaz<sup>1</sup>, N. Marina<sup>1</sup>, T. Ramon<sup>1</sup>, O. Ahumada<sup>1</sup>

<sup>1</sup>Mecwins SA, Ronda de Poniente 15 2D, Tres Cantos, Madrid, Spain

vpini@mecwins.com

AVAC technology is an innovative biosensing platform for the ultra-sensitive and multiplexed detection of protein biomarkers. The fundamental principle of this innovative technology is based on the optical detection of plasmonic nanoparticles amplified by the multi-dielectric substrate underneath [1,2].

The immunoreactions take place on a multi-dielectric substrate coated with antibodies specific to the biomarker of interest. Once the sample has been incubated, a specific antibody tethered to the surface of plasmonic nanoparticles recognizes the biomarkers of interest (see Figure 1). As each plasmonic nanoparticle binds specifically to the biomarker of interest, counting the number of nanoparticles allows to quantify the number of biomarkers immobilized on the surface.

The nanoparticle detection is performed with the AVAC scanner, a proprietary platform that allows the simultaneous measurement and analysis of plasmonic nanoparticle with ultra-high throughput [3,4]; the complete measurement and analysis of a 96-well plate takes less than 5 minutes. The plasmonic nanoparticles are first optically identified, and then the scattering spectrum of each individual nanoparticle is analyzed in order to characterize, classify, and finally count the particles. The combination of different nanoparticle parameters such as brightness, spectral information or polarization state allows a very high specificity, and results in a very low limit of detection in the femtogram range, and provides the capability of detecting several biomarkers within the same sample (multiplexing). In combination with the biosensing platform, Mecwins has developed a cartridge prototype, which is compatible with sample handling systems routinely used in hospitals and analytical laboratories.

Our proprietary detection technology is up to one million times more sensitive than ELISA technology, which has been the standard for protein detection for over forty years. This innovative AVAC technology provides a solution for those diagnostic situations where ultra-sensitive detection is needed; moreover, this technology is also suitable for point-of-care (POC) applications. AVAC technology has proven extraordinary sensitivity with many established biomarkers in clinical use for diagnosis, monitoring, and prognosis, with applications in oncology, myocardial infarction, rheumatoid arthritis, and infectious diseases. An example of the extraordinary capabilities of the technology is demonstrated with the p24 immunoassay (Figure 2), which exhibits a sub-femtogram sensitivity in human serum samples.

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Figure 1. Workflow of the entire AVAC assay process.



**Figure 2.** Calibration curve for Mecwins' p24 immunoassay in human diluted serum; data are represented as ratio sample/control.

# In vivo biodistribution of siRNA-supported by polymer nanoparticles using Positron Emission Tomography (PET) imaging

Cristina Simó<sup>1,2</sup>,

Patrizia Andreozzi<sup>2</sup>, Vanessa Gómez-Vallejo<sup>1</sup>, Luka Rejc<sup>1</sup>, Jordi Llop<sup>1</sup>, Sergio Moya<sup>2</sup>

<sup>1</sup> Radiochemistry and Nuclear Imaging Group, CIC biomaGUNE, 20014 San Sebastian, Spain <sup>2</sup> Soft Matter Nanotechnology Group, CIC biomaGUNE, 20014 San Sebastian, Spain

#### csimo@cicbiomagune.es

After the emergence of nanotechnology, many different types of nanoparticles (NPs) are being used in the biomedical field to encapsulate drugs that are not suitable for direct delivery. Several strategies have been used for the encapsulation of drugs using NPs, where the drugs can be linked to the core or surface of the NP by covalent, electrostatic or hydrogen bonding interactions. In recent years, small interfering RNA (siRNA) has emerged as a promising treatment strategy for various genetic diseases. However, siRNA is readily degraded after administration into the blood stream. Such degradation can be retarded by using appropriate drug delivery systems. One possible strategy is the use of NPs based on the self-assembly of polyamines and phosphate ions. Here, we describe the use of poly(allylamine hydrochloride) (PAH) as a carrier of siRNA and the application of radiollabelling followed by Positron Emission Tomography (PET) imaging to study its biodistribution *in vivo*. The <sup>18</sup>F-labelled SiRNA was prepared by the reacting the amino group-modification of siRNA with 6-[<sup>18</sup>F]fluoronicotinyl-2,3,5,6-tetrafluorophenyl ester ([<sup>18</sup>F]FPy-TFP), which was prepared as previously reported [1]. *In vivo* PET Imaging studies in rodents after intravenous administration clearly showed a different biodistribution between free [<sup>18</sup>F]-siRNA, which was rapidly eliminated via urine, and PAH/[<sup>18</sup>F]-siRNA nanoformulations, which showed significant accumulation in the liver, the spleen and the lungs (Fig. 1).

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## **Figures**



**Figure 1.** In vivo biodistribution studies of a) [18F]siRNA, and b) PAH/[18F]SiRNA in healthy mice using PET-CT. Images show the biodistribution after intravenous administration at time 30 min.

# Photometric-based biosensor for PKU and control unit miniaturization for point-ofcare diagnostics

#### Morgane Valles<sup>1</sup>,

Paul Eduardo David Soto Roodriguez<sup>1</sup>, Agostino Romeo<sup>1</sup>, Rafael Artuch<sup>3</sup>, Samuel Sánchez <sup>1,2</sup>

<sup>1</sup>Institute for Bioengineering of Catalonia, Barcelona, Spain
<sup>2</sup>Institució Catalana de recerca i Estudis Avancats
(ICREA), Passeig Lluís Companys 23, 08010 Barcelona, Spain
<sup>3</sup>Inborn Errors of Metabolism Unit, Gastroenterology, Hepatology and Nutrition Paediatric Department, CIBERER, Hospital Sant Joan de Déu, Barcelona, Spain
mvalles@ibecbarcelona.eu

Phenylketonuria (PKU) is a metabolic disease resulting from a deficient enzyme (phenylalanine hydroxylase) and consequent build-up of dangerous levels of an amino acid, L-Phenylalanine (L-Phe), in the blood.<sup>1</sup> If left untreated, PKU can lead to neurodegenerative symptoms, which can be prevented by following a diet low in L-Phe.<sup>2</sup> Thus, early detection of PKU in newborns is essential. Screening and monitoring of the disease is currently centralized at the site of patient care, which generally requires specialized and costly equipment, as well as gualified personnel to perform the diagnostics.<sup>3,4</sup> In this work, we present an enzymephotometric based qualitative strategy to accurately diagnose PKU. It consists of an assay performed in a 96 well microplate, previously functionalized to specifically detect L-Phe. Measurements are performed by a microplate reader, which allows the samples of up to 48 patients to be analyzed simultaneously within a matter of hours and at the site of patient care. The measurements are fast, versatile, low-cost and easy to carry out. The presented diagnostic system has been validated with anonymous real plasma samples provided by the hospital Sant Joan de Deu (HSJD), accurately discriminating healthy from diseased patients.

Moving forward, a more portable point-of-care (POC) device is also envisaged which aims to miniaturize the control unit for electrochemical detection or integrate a smartphone with the photometric sensor. With this goal in mind, we are developing a compact stand-alone benchtop photometric sensor with wifi and bluetooth connectivity, allowing real-time plotting on a mobile phone. In addition, a low-cost miniaturized potentiostat has been designed and assembled for a more wearable/portable electrochemical sensing platform with state-of-the-art performance.

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#### **Figures**



Phenylalanine dehydrogenase (PDH) + BSA + Nafion

**Figure 1.** Schematic representation of the detection mechanism of the photometric platform for phenylalanine detection. The bottom of the microplate wells is modified with a mixture containing phenylalanine dehydrogenase (PDH), an enzyme that catalyzes the conversion of phenylalanine into phenylpyruvate in the presence of NAD<sup>+</sup> cofactor. The production of NADH (the reduced form of the cofactor) is monitored by measuring the absorbance at 340 nm.

# Natural proteinaceous nanoparticles for theranostic purposes

**Carmen Yuste-Calvo**, María Garrido-Arandia, Flora Sánchez, Araceli Díaz-Perales, Fernando Ponz

Centro de Biotecnología y Genómica de Plantas, Universidad Politécnica de Madrid - Instituto Nacional de Investigación y Tecnología Agraria y Alimentaria (CBGP, UPM-INIA), Campus Montegancedo, Autopista M-40, km 38. Pozuelo de Alarcón, 28223 Madrid, Spain

fponz@inia.es

Natural protein nanoparticles are presented as a great alternative for the development of tools in the biomedical field, providing advantages in terms of biosafety and biocompatibility. This kind of These nanomaterials has been are being used as diagnostic tools, drug delivery systems, vaccination vehicles, among others; so they are considered as a new set of theranostic tools. In this context, viralderived nanoparticles, specifically those derived from plant viruses, offer an extra of biosafety because they are not human or animal pathogens, as well as interesting structural characteristics for tool development, and also cost-economy by plant molecular farming. This is the case of Turnip mosaic virus (TuMV), a potyvirus with whose particles exhibit a flexuous elongated structure which allows the development of functionalized nanoparticles with up to 2000 copies of different compounds with a biomedical interest.

Derivatization by chemical conjugation to different amino acid residues, located in specific regions of the particle surface [1], has allowed a designed functionalization of these particles depending on the application. This functionalization pathway strategy has allowed to conjugate different compounds, such as:

- Peptides with a diagnostic value, in this case related with an autoimmune inflammatory disease.

- Small proteins, like PruP3, a peach allergen with a molecular weight of 9 kDa [2].

- Fluorophores, for bioimagen diagnosis.

- Natural compounds with biomedical properties: antimicrobial, antitumoral and/or antiviral. These functionalizated VNPs would be are used in different applications, such as antitumor treatments, antimicrobial systems, diagnosis of autoimmune diseases, or theranostic tools for food allergies.

Other approaches consisted of functionalization through genetic fusion of peptides to the virus coat protein (CP), rendering peptide-coated nanoparticles, deployable as tools for immunization [3], or for high sensitive diagnosis [3,4]; or the development of nanonets with immobilized enzymes, which has been shown as a possible potential useful tool in the pharmaceutical industry [5], allowing greater yields, for example, in racemic mixtures resolution.

All these advances are opening doors to the multifunctionalization of viral nanoparticles, where different functionalities are presented together and simultaneously in the same nanoparticle.

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## **Figures**



#### TuMV VNPs AS THERANOSTIC TOOLS

**Figure 1.** Functionalization and application of TuMV VNPs in the biomedical field as theranostic tools.



# Mechanical properties of aligned PCL nanofibers made by electrospinning

#### **Reyda Akdemir**<sup>1</sup>, Havvagul Ermis<sup>1</sup>, Silvia de la Flor Lopez <sup>2</sup>, Joan Rosell Llompart<sup>1,3</sup>

 <sup>1</sup> Department of Chemical Engineering, Universitat Rovira i Virgili, E-43007 Tarragona, Spain
 <sup>2</sup> Department of Mechanical Engineering, Universitat Rovira i Virgili, E-47007 Tarragona, Spain
 <sup>3</sup>Catalan Institution for Research and Advanced Studies - ICREA, E-08010 Barcelona, Spain

reyda.akdemir@urv.cat

#### Abstract

The importance of mechanical properties of artificial scaffolds for cell growth is particularly obvious in tissues such as for bone, cartilage, blood vessels, tendons and muscles. Polycaprolactone (PCL) is a very convenient polymer for such purpose due to its low degradation rate and good mechanical properties.<sup>[1]</sup> Here we report on the preparation and mechanical characterization of aligned PCL nanofibers produced by electrospinning stabilized with a co-flow jacket of solvent vapor.<sup>[2]</sup> The electrospinning setup is shown in Figure 1. By using aligned nanofibers,<sup>[3]</sup> mechanical properties of a single fiber were computed. The dissolution of PCL was done in a chloroform-methanol (3:1,v/v)mixture.<sup>[4]</sup> The average diameter of the PCL nanofibers was determined from their sizing in Scanning Electron Microscopy (SEM) images. Dynamic Mechanical Analysis (DMA) was carried out on samples containing thousands of identical nanofibers. As the fibers are aligned and identical, the mechanical tests performed on each sample can be used for computing single fiber average properties. The aligned fibers and the methodology which was followed are shown in Figures 2 and 3. The elastic modulus was obtained by computing the stress for a single PCL fiber. The average tensile elastic modulus and ultimate tensile strength for our neat-PCL nanofibers (Figure 4) was determined as 139 and 41 MPa, respectively. This elastic modulus value lies between that for bulk PCL (343.9 to 363.4 MPa) and the value previously reported for electrospun PCL nanofibers (27.3±3.1 MPa).[1],[5] Given the broad material versatilitv of electrospinning, the proposed method can be extended to many other nanofiber compositions.

## Acknowledgements

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Figure 1. Electrospinning setup



Figure 2. SEM images of aligned PCL nanofibers.



Figure 3. Mechanical testing of the aligned nanofibers. Assembly on DMA clamps (a) and (b) ; DMA test (c).



Figure 4. Tensile Test Curves of aligned PCL fiber mats.

# Design of multivalent polymersomes for range-selective binding

#### Azzurra Apriceno<sup>1</sup>,

Meng Liu<sup>2,3</sup>, Miguel Sipin<sup>1</sup>, Edoardo Scarpa<sup>1</sup>, Laura Rodriguez-Arco<sup>1</sup>, Alessandro Poma<sup>4</sup>, Stefano Angioletti-Uberti<sup>3,5</sup>, Giuseppe Battaglia<sup>1,6,7,8</sup>

<sup>1</sup>Department of Chemistry, University College London, London, UK

<sup>2</sup>Beijing Advanced Innovation Centre for Soft Matter Science and Engineering, Beijing University of Chemical Technology, Beijing, P.R. of China

<sup>3</sup>Institute of Physics, Chinese Academy of Science, Beijing, P.R. of China

<sup>4</sup>Division of Biomaterials and Tissue Engineering, Eastman Dental Institute, University College London, London, UK <sup>5</sup>Department of Materials, Imperial College London, London, UK

<sup>6</sup>Institute of Bioengineering of Catalonia (IBEC), The Barcelona Institute for Science and Technology (BIST), Barcelona, Spain

> <sup>7</sup>Catalan Institution for Research and Advanced Studies (ICREA), Barcelona, Spain <sup>8</sup>The EPSRC/Jeol Centre for Liquid-Phase Electron Microscopy at UCL

> > a.apriceno@ucl.ac.uk

The success of nanomedicine is nowadays strictly associated to the ability of selectively targeting the site of interest: the more specific a therapy is, the more likely it is to be efficient.

The use of multiple ligands, i.e. multivalency, with low affinity for their receptors has proved to successfully address this 'selectivity' requirement [1]. In fact, thanks to the ligand-receptor simultaneous interactions, the collective binding (avidity) compensates for the low affinity and generates a switch-like behaviour where the binding occurs only above a certain receptors density [2].

This mechanism, widely spread in nature for the mediation of several aspects in cell biology [3,4], has recently inspired the design of several drug delivery polymeric nano-constructs functionalized with suitable ligands to guide the carriers according to the level of receptors expression and to deliver their cargos where most needed [5].

Polymersomes, self-assembled amphiphilic diblock copolymer vesicles, have been widely used as nano tools for drug delivery purposes thanks to their versatility and increased stability within biological environments. A recent research carried out on pegylated polymersomes has shown, through cellular uptake studies, that these nanovesicles can display a superselective behaviour by tuning the effective contribution, in terms of chemical potential, of different parameters including the polymer brush length, particle sizes, ligands number [6].

Taking inspiration from these results, the main purpose of the present study was to explore a new type of selectivity where multivalent polymersomes only bind targets when the receptor density is within a certain range. To this aim, a statistical mechanical modelling study was firstly carried out in order to characterise the region where to expect the range selective targetin. Then, Angiopep2-decorated polymersomes were prepared by a solvent switch approach. The formulations were characterised by DLS and TEM and binding studies between functionalized polymersomes and highly-expressing LRP1 FaDu cell line were carried out through fluorometer and laser confocal scanner microscopy.

Understanding the behaviour of the modelled system will significantly improve the design of precise nanodevices with the ability of performing *ad hoc* selective transport and site targeting within cellular environment.

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# Antifungal effect of pegylated graphene oxide and silver nanoparticles against candida albicans

#### Mariana P. Arce<sup>1</sup>,

Arisbel Cerpa<sup>1\*</sup>, Yuen-Ki Cheong<sup>2</sup>, Etelka Chung<sup>2</sup>, Isabel Lado-Touriño<sup>1</sup>, Noemi Luengo Crisóstomo<sup>1,2</sup>, Guillermo Rodríguez<sup>1,2</sup>, Guogang Ren<sup>2\*</sup>

<sup>1</sup>School of Architecture, Engineering and Design. Universidad European de Madrid, Spain<sup>2</sup>School of Engineering and Technology. University of Hertfordshire. Hatfield. U.K.

mariana.arce@universidadeuropea.es

#### Abstract

Due to the global concern over antimicrobial resistance,<sup>1</sup> advanced materials are being studied possible antimicrobial properties. for their Nanoparticles (NPs) have been shown to have antimicrobial effect against certain pathogens. In our study, an initial antimicrobial screening of 13 different NPs standard materials against a series of harmful micro-organisms was carried out. Along with Copper (Cu) and Silver (Ag) NPs, certain Graphene oxides NPs were found to effectively counteract a fungal species, called Candida albicans.<sup>2</sup> With an aim to improve colloidal stabilities of this Graphene oxides (GO), hence to provide better opportunities to microbial exposure, surface modification of GO NPs was performed. As shown in Figure 1, new PEGylated products GO-PEG was synthesised via amide bond formation after the coupling reaction of GO and 4-arm-PEG5K-NH<sub>2</sub> in the present of 1-ethyl-3- (3-dimethylaminopropyl)carbodiimide hypochlorite (EDC HCI).

The physiochemical properties of both GO and GO-PEG were investigated using pH, zeta potential and Nanoparticle Tracking Analysis (NTA).<sup>3</sup> During the initial antifungal screening, all treated *C. albicans* cultures were visualized using an inverted microscope with an aim to capture interactions between the cells and nanoparticles. Biological staining and fixation techniques were applied prior studying morphological changes of affected cells using Scanning Electron Microscopes (**Figure 2**).

MIC values were obtained using broth dilution method where each absorbance was measured at  $\lambda$  490 nm (XTT) in 96 well plates. Four different ratios of GO-based and Ag NPs combinations were used to determine synergistic anti-fungal effects. The results obtained shown the antimicrobial effect depend of GO-based materials /different Ag NPs ratio.

In addition, Molecular Dynamic (MD) simulations of the adsorption of Ag clusters on pristine GO and GO-PEG surfaces were carried out. The calculated adsorption energies from these models demonstrated that the introduction of PEG chains on the GO NPs strengthens the interaction between the surface and the Ag cluster.

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**Figures** 



Figure 1. Synthesis of GO-PEG via coupling reaction



**Figure 2.** SEM images of (a) C. albicans control and (b) affected cell after NP treatment.

# Intrinsic Enzymatic Properties Modulate the Self-Propulsion of Micromotors

#### Xavier Arqué<sup>1</sup>,

Adrià Romero-Rivera<sup>2</sup>, Ferran Feixas<sup>2</sup>, Tania Patiño<sup>3</sup>, Silvia Osuna<sup>2,4</sup>, Samuel Sánchez<sup>1,4</sup>

<sup>1</sup>Institute for Bioengineering of Catalonia (IBEC), BIST, Barcelona, Spain <sup>2</sup> Institut de Química Computacional i Catàlisi (IQCC), Universitat de Girona, Girona, Spain

<sup>3</sup>University of Rome Tor Vergata, Rome, Italy <sup>4</sup>Institució Catalana de Recerca i Estudis Avançats (ICREA), Barcelona, Spain

#### xarque@ibecbarcelona.eu

Bio-catalytic micro- and nanomotors self-propel by the enzymatic conversion of substrates into products.<sup>1</sup> Enzymes offer a combination of biocompatibility, bioavailability and versatility. making it a promising tool for certain biomedical applications.<sup>2</sup> Despite the advances in the field, the fundamental aspects underlying enzyme-powered active motion have rarely been studied, and need to be addressed to make implementations more feasible. We focus our research on the study of the fundamental aspects that rule the active motion of enzymatic micro- and nanomotors,<sup>3</sup> such as the role of the enzyme intrinsic properties.4

We explore the versatility of such systems by studying the powering capacity of a library of enzymes to propel silica-based micromotors: urease, acetylcholinesterase, glucose oxidase and aldolase. We study how their turnover number and conformational dynamics affect the self-propulsion, combining both an experimental and molecular dynamics (MD) simulations approach. Results show that the motion behavior is strongly dependent on the enzyme type.

We conclude that the conformational changes are a precondition for urease catalysis, and that the rate of catalysis is essential and directly related to active motion. Future research will be focused on studying the effect of extrinsic parameters such as the media properties and composition.

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**Figure 1.** (A) TEM micrograph of a microcapsule colored depending on thickness. Hole detection (arrows) and silica bulks (arrowheads) detection. (B) Speed vs. turnover number ( $k_{cat}$ ) of different enzymatic micromotors (urease, acetylcholinesterase, glucose oxidase and aldolase). Inset: Trajectories of the enzymatic micromotors. (C) Molecular dynamic simulation (MDS) of urease with acetohydroxamic acid (AHA) stabilizing the flap in wide-open state (teal). (D) Speed of UR-HSMM and enzymatic activity (Abs 670 nm) vs AHA concentration in 500 mM urea. Inset: linear correlation of speed and enzymatic activity.

# Curcumin-loaded PVP particles produced by electrospray

#### Elena Barbero<sup>1</sup>,

Antonio J. Carrasco-Muñoz<sup>1</sup>, Eszter Bodnár<sup>1</sup>, Jordi Grifoll<sup>1</sup>, Joan Rosell-Llompart<sup>1,2</sup>

 <sup>1</sup> Department of Chemical Engineering, Universitat Rovira i Virgili, Tarragona, Spain
 <sup>2</sup> Catalan Institution for Research and Advanced Studies, Barcelona, Spain Elena.barbero@urv.cat

Electrospray, also known as electrohydrodynamic atomization (EHDA), is a robust technique for producing uniform polymeric particles with controlled morphology and size. In this technique, a liquid pumped through a nozzle is electrically charged by applying high voltage. The electrified liquid adopts a conical shape (called Taylor cone) with a thin jet at its end. This jet then breaks up into highly charged droplets, which form a charged spray plume as they drift towards an oppositely charged substrate, where they are collected as solid particles after the solvent has evaporated from them. One of the advantages of EHDA over other liquid atomization methods is its ability to produce much smaller particles (in the fewmicrons and nano-metric size ranges) [1].

From the point of view of biomedical and pharmaceutical applications, it is desirable to produce size-monodisperse particles. Such particles are used as vehicles for drug delivery, where the release profile of an encapsulated drug is strongly influenced by the particle size; thus the importance to control particle size in the production method [2]. Whereas it is possible to produce homogeneous particles by electrospray, the droplets in the spray often undergo Coulombic instabilities, resulting in particles with non-ideal shapes, commonly elongated or pointed particles with nano-filaments attached [3].

The objective of this work is to produce homogenous polyvinylpyrrolidone (PVP) particles by electrospray. Particles with well-controlled morphologies and sizes of up to a few microns were imaged by scanning electron microscopy (SEM) (Figure 1).

We observed that the particle size is influenced strongly by the infused liquid flow rate. The initial polymer concentration and polymer molecular weight (MW) remarkably affect the morphology of the particles. With Mn 360 kDa MW, as the polymer concentration in the solution increases we observed a progression in particle morphology from filamented particles (due to Coulombic instabilities) to nonfilamented particles, to filamented morphology (due to incomplete jet breakup). The solvent system can also affects the particles morphology and size. In the case of PVP 40kDa, less spherical (more corrugated) particles with larger sizes were obtained when we used a solvent mixture of solvent (ethanol/acetone 50/50) than when we used ethanol as solvent.

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## **Figures**



**Figure 1.** SEM images of PVP-curcumin microparticles of different morphologies collected on a silicon wafer.

(a) PVP 40 kDa and curcumin (0,1 %w) in EtOH at different polymer concentrations (by wt.): 1% (a.1), 5% (a.2), 10% (a.3).

(b) PVP 360 kDa and curcumin (0,1 %w) in EtOH, at polymer concentrations (by wt.): 1% (b.1), 1.5% (b.2), 3% (b.2).
(c) PVP 40 kDa and curcumin (1:1) in ethanol/acetone (50/50)

(c) PVP 40 kDa and curculatin (1.1) in ethanol/acetone (50/50 v/v) at polymer concentrations (by wt.): 0.6% (c.1), 5% (c.2), 10% (c.3).

# Water elimination by CO<sub>2</sub> cryospraying technology to obtain dry microparticles from biphasic, lipid dispersed systems

## Jesús Caramés<sup>1,2</sup>,

Caroline Carrié<sup>3</sup>,Hana Danan<sup>1</sup>,Pierandrea Esposito<sup>1</sup>

<sup>1</sup>Sitec Pharmabio, Barcelona, Spain <sup>2</sup>USC – University of Santiago de Compostela, Spain <sup>3</sup>UCA- Université Clermont Auvergne, France

j.carames@sitec-pharmabio.com

#### Introduction

Variosol<sup>®</sup> cryospraying technology exploits the physical properties of rapidly expanding liquid or dense  $CO_2$  [1] to perform as cryogenic agent (Joule-Thomson effect), while providing mechanical energy through a rapid pressure drop. This rapid expansion can induce phase change, solidification and atomization in a sprayed fluid, forming a dynamic mixture with the expanding  $CO_2$  and transforming the liquid product into a micronized, dried powder. The main advantage of this technology is that it operates at relatively low temperatures and pressures, and does not require supercritical  $CO_2$ , thus reducing the use of energy-consuming elements, and making the process simple and efficient.

One peculiar feature of the expanding CO2 cryospraying is the capability to eliminate significant amounts of water from biphasic disperse systems, during fluid atomization at low temperatures. This "dewatering" effect occurs when the product is sprayed under certain conditions of CO<sub>2</sub> pressure and temperature [2]. Presumably, the water contained in the atomized fluid product is rapidly cooled down and micronized with very high specific surface, and subsequently eliminated in the surrounding atmosphere (phase equilibria) leaving the spray tower with the exhaust gas. Therefore, it is possible to obtain solid, dry microparticles with a residual moisture of about 0.5 to 3%, and diameters below 100 µm, after atomization under dense CO<sub>2</sub> expansion [2,3]. This feature offers the possibility to formulate and produce lipophilic or amphiphilic micromatrices containing hydrophilic, water soluble molecules. The technology can also directly encapsulate natural extracts containing significant amounts of water, transforming them in formulated, micronized powders [4], without the need to reach supercritical CO2 conditions, as it occurs in PGSS-drying technology [5].

The main objective of this study is to evaluate the impact of different process parameters on particles size, morphology and residual water content.

Parameters such as pressure applied to sprayed fluid, nozzles type, diameters and geometry were investigated using aqueous disperse systems of lipidic excipients with amphiphilic properties. The results obtained could be used to explain and understand the key features of particles formation and dewatering phenomenon by CO<sub>2</sub> cryospraying technology. This will help us to optimize the physical properties of the microparticles and process water elimination capability.

#### Materials and methods

Mono, di- and triglycerides with medium to long chain fatty acids, and their amphiphilic derivatives (e.g. poly-hydroxylated fatty esters) were used for these studies. These materials were selected because of their known function in pharmaceutical preparations as solubilization or absorption enhancers, and as controlled release excipients. In addition, their relatively low melting point (typically ranging from 35 °C to 75 °C), combined with the rapid solidification properties at low temperatures, makes them suitable to formulate thermolabile molecules, and processable with the CO<sub>2</sub> cryospraying technology. Different operating conditions were applied in these studies. Gas pressure applied to sprayed material ranged between 1 to 4 bar, and fluid product temperatures were maintained between 55 °C and 85 °C, depending on the formulations. Nozzles producing capillary flow, with diameters between 0.36 to 0.85 mm were used to spray the fluid product. Two different types of dense CO<sub>2</sub> nozzles - full cone flow geometry or swirling flow pattern, were tested and compared. Dense CO<sub>2</sub> pressure was maintained between 48 and 55 bar. Microparticles were characterized by particles size analysis, Optical Microscopy, SEM and residual moisture content by Karl-Fisher Analysis or TGA.

#### **Results and discussion**

Spherical or spheroidal microparticles, with a matrixtype morphology were obtained at all the conditions studied. Depending on applied process conditions, the average diameters varied between 20 to 100  $\mu$ m approximately, with narrow particle size distribution and good powders flowability. Optical Microscopy and SEM observation indicated that different surface features could be obtained, depending on excipients combinations and on applied processing conditions. Porosity and water residual areas observed by SEM suggest that the "dewatering" phenomenon is likely generated from water rapid freezing and subsequent evaporation during the spraying in the presence of CO<sub>2</sub>.

Applying different conditions of pressure, temperature, nozzles diameter and geometry, we observed that effective water elimination to obtain dry microparticles can be achieved when the formulations to be sprayed contain up to about 35% water. Therefore, it is possible to produce dry microparticles by spraying, for instance, drug – containing emulsions, microemulsions, and other complex systems such as fractions of natural extracts. Water elimination capacity and residual moisture in the particles also depend on the nature of the sprayed materials and their affinity to bind and retain water molecules or moisture. In fact, we observed how microparticles containing more hydrophilic excipients (e.g. polyhydroxylated - lipid derivatives) tend to retain more moisture. The dewatering effect may be enhanced by generating high surface area within the sprayed material, during the liquid CO<sub>2</sub> expansion. This can be achieved by introducing modifications in equipment design, while formulating disperse systems with smaller inner-phase droplets.

#### Conclusions

Cryospraying technology exploits the physical properties of rapidly expanding liquid-dense CO<sub>2</sub> to perform as cryogenic agent while providing mechanical energy through a rapid pressure drop. Such features allow to produce dry microparticles from biphasic dispersed systems, facilitating the elimination of water directly during the atomization at low temperatures.

Formulations including up to about 35% of water can be sprayed using the existing equipment design. It is thus possible to manufacture amphiphilic, composites microspheres containing combinations of different drugs or moieties, in a simple, one step process.

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## Figures



Figure 1. Scheme of dense CO2 Cryospraying technology



Figure 2. SEM Images of formulated microparticles with porous and not porous morphology



Figure 3. Residual moisture (%w) in microspheres (TGA) vs. water content in formulated emulsions before spraying

# Coarse-grained model for water and water-protein interfaces.

Luis E. Coronas<sup>1,2</sup>, Valentino Bianco<sup>3</sup>, Arne W. Zantop<sup>4</sup>, Giancarlo Franzese<sup>1,2</sup>

<sup>1</sup>Department of Condensed Matter Physics, University of Barcelona, C. Martí I Franquès 1 08028, Barcelona, Spain <sup>2</sup>Institute of Nanoscience and Nanotechnology (IN2UB) University of Barcelona, C. Martí i Franquès 1 08028, Barcelona, Spain <sup>3</sup>Department of Chemical Physics, University Complutense of Madrid, Plaza de las Ciencias, 28040 Madrid <sup>4</sup> Institut für Theoretische Physik, Technische Universität Berlin, Hardenbergstr. 36, D-10623 Berlin, Germany

 ${\tt lcoronas@ub.edu, gfranzese@ub.edu}$ 

We study, by Monte Carlo simulations, a coarsegrained model for nanoconfined water that includes many-body interactions associated to water cooperativity, originally introduced by Franzese and Stanley (FS) [1]. The FS model is computationally efficient [2] and allows us to equilibrate water at extreme low temperatures T in a wide range of pressures P [3,4]. Moreover, it can be easily extended to include proteins, so we can analyze the behavior of the water-protein interface and how the solvent affects the protein configuration [5,6]. Here, we focus on the phase diagram of the FS model, showing that it reproduces, at least qualitatively, the experimental water phase diagram both in confinement and in bulk [7], a prerequisite for using it as a proper solvent in protein solutions. Our results compare well with atomistic simulations and show, for both confined (Figure 1) and bulk water, the presence of a low-density liquid and a high-density liquid water phases, separated by a liquid-liquid phase transition ending in a liquid-liquid critical point. Our results clarify fundamental properties of hydration and bulk water and are potentially useful for better understanding the effects of T and P on nano-bio-interactions among proteins and other species or interfaces.

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**Figure 1.** Schematic representation of water multilayers under nanoconfinement. We consider a system of 20 layers corresponding to a separation between walls of 6 nm.

# Silver foams with hierarchical pores for antibacterial activity

**F.Ç. Durmus<sup>1</sup>**, J.M. Molina Jordá<sup>1,2</sup>

<sup>1</sup> Instituto Universitario de Materiales de Alicante, University of Alicante, Ap. 99, E-03080 Alicante, Spain

<sup>2</sup> Departamento de Química Inorgánica de la Universidad de Alicante, University of Alicante, Ap 99, E-03080 Alicante, Spain

#### cagla.durmus@ua.es

Filters are mainly used to physically block objects or substances, to remove impurities such as dirt, bacteria or oil from the flow. Since open-celled foams have high specific surface area and permeability property, they are often preferred for flow-through applications as filters in where these internal surface properties can be exploited. Foams can be used in virtually any filtration field as wet or dry filters thanks to their excellent active surface area and porous structure. [1, 2] It is very important that the foams have good mechanical properties as well as they allow for a highly stable flow during the filtration. [3] Especially open cell metallic foams, have received considerable attention in recent years as materials that find use in various engineering applications. They are also suitable for use in the field of filtration to reduce the concentration of undesirable ions dissolved in water. [4] In applications intended to reduce the concentration of dissolved ions in water, open cell metallic foams with high liquid / gas permeability are used which allow liquid flow through micro and macro pores. [2, 3] Foams have been regarded as a convenient candidate for air filtration, drinking water purification, antibacterial purposes and for industrial and environmental filtration applications and previously many studies have been made for these purposes. [5] Microbial contamination from microorganisms causes various problems in human life. It is completely impossible to create а sterile environment to prevent infections, but it is possible to take precautions to prevent the increase in the number of microorganisms. Bacterias are the most serious infections common and most of microorganisms. As is known, ions of metals such as copper, zinc and silver have a strong antibacterial effect. [6] In order to combine and take benefit of these advantages of ionic silver and cellular structure of foam, researchers have also been focused on studies to obtain materials which have uniform microstructures with micro and macropores and large internal surface area. Since the cellular structure of the foam can be controlled by porosity, there are several methods that can be used for the fabrication of open celled silver foams having micro and macro pores throughout the foam. [7, 8] The primary objective of this study is to produce antibacterial effective foam structures with replication method following by chemical dealloying. For this purpose, production was started with alloying aluminium and silver metal, and then it was used to manufacture foams. Two different route were used as 5% HCl and 20% NaOH solution in order to observe the effect of dealloying environment on the microstructure and pore size distribution [9]. The codes were used to define samples as: AgAl is the foam resulting from infiltration of a packed bed of preforms with liquid AgAl alloy, after dissolution of the NaCl particles (with no further chemical treatment); Ag-HCl is the foam after HCl treatment; Ag-NaOH is the foam after NaOH treatment; Ag-sint is a foam resulting from sintering. Foams were analyzed by SEM, interconnected-bicontinuous structures with hierarchical pore sizes ranging from nanoscale to micron scale were obtained with both dealloying route. XRD analysis was carried out to determine phases the samples contain after the dealloying processes. With the detailed pore size distribution study, the contributions of the different scale pores to the foam porosity which sourced from alloy microstructure, infiltration process and the dealloying process were determined. Nitrogen adsorption/desorption isotherms were used to determine surface area, pore volume and nano pore size distribution. Multi point BET method was used to measure surface area of the samples. Pore volume and nanopore size distribution was carried out by Quantochrom software. In addition to characterisations were mention above, to evaluate the performance of the foams as a filter, antibacterial efficiency was investigated according to ASTM E2149 against Gram Positive (S. aureus) and Gram Negative (E. coli) bacterias. The effect of dealloying process and pore size distribution on antibacterial performance of the foam were investigated. After 24 hours, the foam dealloyed with NaOH exhibited a superior performance compared to the other foams, providing 99.99% reduction in both bacteria species. These promising results have shown that this process combination allows to tailor the pore size, distribution and porosity according to the intended area of use.

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Figure 1. Contribution of micro and meso pores to total volume



**Figure 2.** Experimental results for antibacterial activity were displayed as log reduction versus exposure time for AgAI, Ag-HCI, Ag-NaOH and Ag-Sint samples against E.Coli and S.Aureus.



Figure 3. Experimental results for antibacterial activity were displayed as % reduction versus exposure time for AgAI, Ag-HCI, Ag-NaOH and Ag-Sint samples against E.Coli and S.Aureus.

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# Insights into the synthesis of Bi<sub>2</sub>S<sub>3</sub> nanostructures for Computed Tomography

#### M. Escoda-Torroella<sup>1</sup>,

C. Moya<sup>1</sup>, D. Doblas<sup>1</sup>, A. Fraile Rodríguez<sup>1</sup>, A. Labarta<sup>1</sup> and X. Batlle<sup>1</sup>

<sup>1</sup> Departament de Física de la Matèria Condensada, Institut de Nanociència i Nanotecnologia (IN2UB), Universitat de Barcelona, 08028 Barcelona, Spain

mariona.escoda@ub.edu

Computed tomography (CT) is an X-ray based whole body imaging technique widely used to enhance the contrast among human body tissues because it allows deeper tissue penetration and higher-resolution imaging [1]. Currently, clinically approved CT contrast agents are iodinated molecules or barium suspensions, but to provide a good contrast large doses are needed, and their short circulation time limits their applications. Nanoparticles (NPs) show several advantages in comparison with these small molecules such as high residence times, potentiality for cell-tracking and imaging applications due to their targeted functionalizable surface [2],[3]. In particular, Bi<sub>2</sub>S<sub>3</sub> NPs are a good choice because bismuth shows a large X-ray attenuation coefficient which enhances the contrast for small variations of the X-ray voltage. In addition, it is less expensive and also exhibit lower toxicity than other metals with similar X-ray attenuation coefficient. However, there is a lack in the literature of methods enabling a good control over the NP structure.

Here, we show a 2-step method to obtain  $Bi_2S_3$  NPs with tunable shape and size based on the high temperature decomposition of bismuth (III) neodecanoate using different high boiling-point solvents, 1-octadecene and benzyl ether [4]. We have monitored the particle size and shape by tuning the duration of the last step of the reaction from 1 to 120 minutes. After that, we have stabilized the samples in aqueous media by a ligand exchange process.

After the first reaction stage, crystalline 5 nm spherical nanoparticles are obtained. Rod-like-shaped NPs can be grown by further increasing of the reaction time, which yields elongated NPs with 5 nm in width and from 5 nm to 50 nm in length. Despite the good control found in the particle size distribution, particles show poorer crystalline quality as they become elongated, which may be due to a faster growth process. By EELS analysis, we have discarded the presence of any parasitic phase of bismuth oxide. These nanoparticles may pave the way to enable the combination with other materials

to achieve multifunctional systems for diagnosis or theranostics.

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**Figure 1.** High-resolution transmission electron microscope images of the NPs obtained changing the duration of the last step of the reaction from 1 min to 120 min.

# Metal-enzyme nanocomposites with bactericidal and antibiofilm efficacies

Guillem Ferreres <sup>1</sup>,

Kristina Ivanova<sup>1</sup>, Juan Torrent-Burgués<sup>1</sup>, Tzanko Tzanov<sup>1</sup>

<sup>1</sup>Molecular and Industrial Biotechnology Group, Department of Chemical Engineering, Universitat Politècnica de Catalunya, Rambla Sant Nebridi 22, Terrassa 08222,

guillem.ferreres@upc.edu

Antimicrobial resistance (AMR) is causing 50 thousand deaths per year in Europe and North America, with a concomitant heavy economic burden. Bacteria have developed different specific mechanisms conferring antibiotic resistance altering or destroying the antibiotic molecules, decreasing the membrane permeability to the antibiotic or expulsing it through efflux pumps.<sup>1</sup> Besides these resistance mechanisms, the ability of bacteria to proliferate adhered to inert surfaces or living tissues forming biofilms aggravates the appearance of AMR. Bacteria encased in these structures avoid the immune system response and makes them highly tolerant to high concentrations of antimicrobials.<sup>2</sup> Furthermore, conventional antibiotics do not remove biofilms thus, despite a successful antibiotic treatment; remaining sessile cells may lead to an infection relapse.

Metallic nanoparticles (NPs) are increasingly used to target pathogenic agents as an alternative to antibiotics. Metallic NPs offer a platform against bacteria, viruses, fungus and protozoa, these nanoparticles present multiple biocidal mechanisms that occur at the same time<sup>3</sup> (oxidative stress induction, metal ion release, or non-oxidative mechanism) reducing and hindering the appearance of the microbial resistance. On the other hand, among anti-biofilm strategies, different enzymes can be applied to prevent the biofilm formation or its eradication once established.

In this study, we integrate metallic particles with antibiofilm enzymes in the same nano-entity to combine synergistically different antimicrobial agents. The enzymatic component disrupts the bacterial communication pathways, through the hydrolysis of small molecule signals that govern the biofilm formation.<sup>4</sup> On the other hand, the biocidal activity of the nano-composite is supplied by the metallic particles while functions as an active template for the grafting of the enzyme. This antimicrobial approach could be applied in the form of coatings on surfaces such as hospital textiles, water treatment membranes and implantable medical devices, ensuring a safer environment for both patients and healthy population.

Silver-chitosan NPs (AgCh NPs) were synthesised by silver ions reduction, using chitosan as a reducing and capping agent. After washing the particles, UV-vis spectrometry reveal the pick at 420 nm corresponding to the formation of Ag NPs. TEM images revealed spherical NPs of 25-30 nm of diameter. After that, the AgCh NPs were functionalized with the quorum quenching enzyme (QQE) acylase I. The TEM analysis showed that the AgCh NPs were embedded in a protein matrix-like structure forming a silver-chitosan-acylase I (AgChAcyl) composite. The particles containing acylase were able to hydrolyse N-acetyl-Lmethionine during the ninhydrin assay, indicating that the enzyme maintained part of its activity after the cross-linking between the chitosan and the acylase I.

The antimicrobial efficacies of AgCh NPs and AgChAcyl NPs were tested towards Psuedomonas aeruginosa. Silver and chitosan are well-known antimicrobial agents.<sup>5</sup> However, the antimicrobial assay showed that the presence of acylase I enhanced the antimicrobial activity of AgCh NPs (Fig. 1A). In addition, the time-killing assay reveal that AgCh NPs and AgChAcyl NPs displayed a rapid antimicrobial effect. After 20 minutes incubation of the NPs with P. aeruginosa, the bacterial concentration was drastically reduced. Nonetheless, this reduction was faster when the nanoparticles contained the QQE enzymes acylase I (Fig. 1B). Acylase I by itself did not presented any antimicrobial effect, which indicated that there is a synergistic effect between the QQE and the antimicrobial agent.

*P. aeruginosa* was exposed to AgCh NPs and AgChAcyl NPs to test the capacity of composites to disrupt the biofilm formation. The biofilm was washed to remove the NPs and the non-attached bacteria. The establishment of the extracellular matrix was assessed by crystal violet assay and livedead staining. Both assays confirmed that the presence of acylase I in the nanoparticles inhibits the formation of biofilm (Fig. 2). Acylase I is able to hydrolase N-butyryl-I-homoserine lactone, a quorum sensing molecule of *P. aeruginosa*, hindering the quorum sensing and affecting the processes that are related with this communication, such as the production of virulence factors and the biofilm formation.

Finally, the biocompatibility of the particles was assessed using different human skin cell lines. The toxicity towards these cell lines was reduced when the enzyme was present on the surface of the NPs reduced the toxicity of the composites towards mammal cells.

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13. 28 ppm of silver and the bacteria surviving the treatment were estimated after 15, 30, 60 and 180 min.

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**Figure 1.** A) Evaluation of the antimicrobial activity of AgCh NPs, AgChAcyl NPs and AgChBSA NPs. The particles were tested using the same silver content. Acylase I was tested at the initial concentration of the synthesis of the particles. *P. aeruginosa*  $t_0$  indicates the initial bacterial concentration of the test and *P. aeruginosa* value indicates the final concertation of bacterial without treatment B) Time-kill curves of AgCh NPs (dark grey) and AgChAcyl NPs (light grey) towards *Pseudomonas ae*ruginosa. *P. aeruginosa* was incubated with





**Figure 2**. Evaluation of the biofilm inhibitory activity of AgCh NPs and AgChAcyl NPs. A) Assessment by crystal violet assay of *P.aeruginosa* biofilm inhibition, incubated for 24 h with AgCh NPs and AgChAcyl NPs. B) Fluorescence microscopy images of *P. aeruginosa* biodfilm after the treatment with C) AgCh NPs and D) AgChAcyl NPs.

# When and Where: Microfluidic Cancer-on-a-chip platform for real-time imaging of drug delivery systems stability and extravasation

#### Adrianna Glinkowska Mares<sup>1</sup>,

Natalia Feiner-Gracia<sup>1,2</sup>, Marina Buzhor<sup>4</sup>, Josep Samitier<sup>1</sup>, Roey J. Amir<sup>3-5</sup>, Silvia Pujals<sup>1</sup>, Lorenzo Albertazzi<sup>1,2</sup>

<sup>1</sup>Institute for Bioengineering of Catalonia, C. Baldiri Reixac 10-12, 08028 Barcelona, Spain <sup>2</sup>Department of Biomedical Engineering, Institute for Complex Molecular Systems (ICMS) Eindhoven University of Technology, 5612AZ Eindhoven, The Netherlands <sup>3</sup>Department of Organic Chemistry, School of Chemistry, Faculty of Exact Sciences, Tel-Aviv University, Tel-Aviv 6997801, Israel. <sup>4</sup>Tel Aviv University Center for Nanoscience and

Nanotechnology, Tel-Aviv University, Tel-Aviv 6997801, Israel. <sup>5</sup>BLAVATNIK CENTER for Drug Discovery, Tel-Aviv

University, Tel-Aviv 6997801, Israel

aglinkowska@ibecbarcelona.eu

Drug vehicles confront multiple delivery physiological barriers after injection into the human body. Their performance strictly depends on the stability in that complex environment. Effective nanocarriers should be stable enough to successively overcome the encountered barriers avoiding premature drug release, while being smart enough to free the cargo once the target is reached. Ideally, the performance of a drug nanocarrier should be evaluated in an environment mimicking human physiology, to reduce and refine the number of preclinical and clinical trials. Commonly used 2D cell culture models do not reflect the dynamic and complex organization of a human body, meanwhile animal models are ethically arguable, expensive, time-consuming and still lack direct translation due to the differences between species. Those challenges in drug delivery screening, together with the emerging era of microfluidic technology are the driving forces for the creation of new solutions [1,2].

In our work we present a perfusable 3D cancer-ona-chip platform, where we study time- and spaceresolved stability of potential drug delivery nanocarriers. In the microfluidic chip we recreated a part of tumor microenvironment, where we focus on essential barriers challenging drug delivery systems stability (Figure 1). The microfluidic model recapitulates present *in vivo* perfusable blood vessel lined with organized Human Umbilical Vein Endothelial Cells (HUVECs), that create the cellular wall between the vessel lumen and the extracellular matrix, in which 3D HeLa cancer cells spheroids are distributed [3].

From the different drug delivery systems, we chose to evaluate supramolecular structures. We perfused the microfluidic platform with three amphiphilic PEGdendron hybrids (previously studied in 2D cell culture), that change their fluorescent properties upon assembly into micelles [4]. Thanks to the compatibility of the microfluidic model with confocal spectral imaging we could register real-time stability and extravasation of the introduced nanostructures interacting with the 4 defined barriers (blood vessel, extracellular endothelial wall. matrix. tumor spheroid). This special property of the micelles allows us to follow their stability in correlation with the barrier they encountered, by real-time monitoring of changes in their fluorescence emission.

We observed a difference in extravasation of nanostructures depending on the leakiness of the endothelial barrier (studying healthy blood vessel and tumor blood vessel models), what correlates to the Enhanced Permeability and Retention (EPR) effect found in vivo. Interestingly, we could observe how the number and proximity of cancer cells affects the integrity of endothelial wall. Furthermore, we were able to identify most and least stable formulations by following their fluorescence emission. We registered decreased micelle internalization comparing to previously investigated 2D cell culture.

Our results demonstrate the applicability of the cancer-on-a-chip microfluidic platform in bridging the gap between 2D and *in vivo* studies. The vision of fast screening of a drug nanocarrier candidates in a 3D cell culture that could use patient derived cancer cells provides knew knowledge in the field of

nanomaterials' performance and brings us one step closer to the personalized nanomedicine.

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**Figure 1.** Cancer-on-a-chip platform. From left to right: A. HeLa cells spheroid confocal microscopy image (Green: live cells stained with Calcein, Red: dead cells stained with Propidium lodide), spheroid diameter in vertical line: 240 µm. B. Transmission image of the cancer-on-a-chip platform. C. 3D reconstruction of HUVECs monolayer creating an interface between the extracellular matrix and the perfusable vessel lumen. Image acquired using confocal microscopy in Z-stack mode, in red: Phalloidin, blue: Hoechst, image height: 280 µm.

# Hybrid fibrous microenvironments for muscle tissue engineering

**B.** Hermenegildo<sup>1</sup>,

Daniela Correia<sup>2,3</sup>, Leyre Pérez-Álvarez<sup>1,4</sup>, José L. Vilas<sup>1,4</sup>, Senentxu Lanceros-Méndez<sup>1,5</sup>

<sup>1</sup> BCMaterials, Basque Center for Materials, Applications and Nanostructures, UPV/EHU Science Park, 48940 Leioa, Spain
<sup>2</sup> Department of Chemistry and CQ-VR, Universidade de

Tras-os-Montes e Alto Douro, 5000-801 Vila Real, Portugal

<sup>3</sup> Centro/Departamento de Física, Universidade do Minho, 4710-057 Braga, Portugal

 <sup>4</sup> Macromolecular Chemistry Research Group, Department of Physical Chemistry, Faculty of Science and Technology, UPV/EHU, Leioa, Spain
 <sup>5</sup> IKERBASQUE, Basque Foundation for Science, 48013 Bilbao, Spain

#### bruno.hermenegildo@bcmaterials.net

To mimic the natural environment of tissues, in-vitro, support structures are necessary in order to allow for healthy cell and tissue development. Hydrogels have become popular materials to develop these support structures due to their substantial water content and the simplicity in tailoring their physical, biological or chemical characteristics. However, hydrogels alone cannot provide all the necessary stimuli and microenvironment for cell development and, therefore, hybrid materials are currently being developed.

Cells and tissues also require more than a suitable biochemical environment to successfully develop and differentiate [1]. Specifically, electrical and mechanical stimuli are extremely important for tissues such as skin, cartilage, bone and muscle. Scaffolds can be functionalized with nanomaterials, so they can deliver these stimuli to improve the viability of the new tissue [2].

Muscle is an electromechanical material, highly responsive to these stimuli [3], and it is known that negatively charged surfaces improve cell adhesion and proliferation and that the directional growth of the myoblast cells can be achieved by using aligned fibers [4].

Therefore, incorporating electroactive polymers in a hydrogel scaffold, and stimulating these polymers externally so that they can in turn stimulate the incorporated cells, allows for in-vitro mimicry of the normal conditions of muscle cell growth and differentiation [5].

In this context, the present work focuses on the development of electrospun electroactive polymer fibers [6], to fabricate functionalized hybrid hydrogel scaffolds for muscle tissue engineering.

Oriented and non-oriented fibers, based on polymers that are electroactive, biocompatible, biodegradable and biostable, have been processed and characterized. They were further modified with ionic liquids and magnetic particles to allow electro and mechanotransduction to be applied to the cells. This resulted in fibers with diameters between 0.5-3  $\mu$ m, crystallinity between 45-60%,  $\beta$ -phase content around 90%, and magnetic properties suitable for use in a magnetic bioreactor, with the thermal stability of the polymer being unaffected by the inclusion of these materials.

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Figure 1. Non-aligned PVDF fibers



Figure 2. Aligned PVDF fibers with magnetic particles



Figure 3. Photo of a fiber at the start of the electrospinning process

# Controlling Cellular Trafficking by Nanoparticle Avidity: From Endocytosis to Transcytosis

#### Diana M. Leite<sup>1</sup>,

Xiaohe Tian<sup>2</sup>, Edoardo Scarpa<sup>1</sup>, Joseph Forth<sup>1</sup>, Diana Matias<sup>1</sup>, Loris Rizzello<sup>3,4</sup>, Manish R. Vuyyuru<sup>5,6</sup>, Andela Šarić<sup>5,6</sup>, Giuseppe Battaglia <sup>1,3,4</sup>

<sup>1</sup>Department of Chemistry, University College London, London, United Kingdom; <sup>2</sup>School of Life Sciences, Anhui University, Hefei, Peo-

ple's Republic of China;

<sup>3</sup>Institute for Bioengineering of Catalonia (IBEC), The Barcelona Institute for Science and Technology (BIST), Barcelona, Spain;

<sup>4</sup>Institució Catalana de Recerca i Estudis Avançats (ICREA), Barcelona, Spain; <sup>5</sup>Department of Physics and Astronomy;

<sup>6</sup>Institute for the Physics of Living Systems, University College London, London, United Kingdom.

#### diana.leite@ucl.ac.uk

Drug delivery to the brain is hindered by the presence of the blood-brain barrier (BBB), which consists in specialised endothelial cells that line brain capillaries restricting movement of molecules from bloodto-brain. Nonetheless, brain endothelial cells (BECs) rely on endogenous transport mechanisms (such as, receptors) that allow certain molecules to transverse the BBB. By using Angiopep-2(AP2)-decorated pHsensitive polymersomes, we previously demonstrated the ability to specifically target lipoprotein receptor-related protein-1 (LRP-1) at the surface of BECs, and trigger transcytosis allowing the delivery of macromolecules into the brain parenchyma [1]. Here, we explore the mechanism of transcytosis of the polymersomes as a function of the number of AP2 ligands (i.e., avidity) using an established in vitro BBB model as well as in vivo.

AP2-poly(oligo(ethylene glycol) methyl ether methacrylate)-block-poly((diisopropylamino) ethyl methacrylate) (POEGMA-PDPA) polymersomes showed binding to LRP-1 in BECs, and significantly higher levels of apparent permeability (2.5-folds) compared to unfunctionalised polymersomes. When decorated with different numbers of AP2 ligands (I = 16 to 82), the rate of transport across a bEnd3 monolayer is affected, with the highest efficiency observed for 16 AP2 per polymersome. At the density of l = 16, the overall affinity of the nanoparticle triggers transcytosis by the formation of tubular structures, as demonstrated by live cell imaging and molecular dynamic modelling simulations. Cellular trafficking of AP2 polymersomes, I = 16 and I = 82, illustrated that, depending on the number of ligands, polymersomes undergo distinct intracellular sorting in BECs. After a tail vein administration of the polymersomes, 3.82% of the injected dose was obtained in the brain for the polymersomes with I = 16 which is significantly higher than unfunctionalised polymersomes, I = 80 AP2-functionalised polymersomes and AP2.

Together, these results elucidate the impact of the density of AP2 ligands on the intracellular trafficking of POEGMA-PDPA polymersomes at BECs. Hence, our work offers a new insight into the mechanism of transcytosis that could be explored when engineering nanoparticles for drug delivery to the delivery.

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# STORM characterization of enzyme powered micro- and nanomotors

#### Joaquin Llacer Wintle<sup>1</sup>, Tània Patiño, Sílvia Pujals, Lorenzo Albertazzi, Samuel Sánchez<sup>2</sup>

<sup>1, 2</sup> Institute for Bioengineering of Catalonia (IBEC), Baldiri i Reixach 10-12, 08028 Barcelona, Spain jllacer@ibecbarcelona.eu

Self-propelled enzyme micro- and nanomotors are promising in the biomedical field as a drug delivery platform. This kind of self-propelled motors make use of enzymes to transform the environmental chemical energy into active motion. Despite the recent advances in the field, a deeper understanding of fundamental aspects is required for an efficient implementation in biomedicine. For example, in order to achieve active motion, an asymmetry on the distribution of the particles has traditionally been claimed. Herein, we study the quantity and distribution of urease molecules around the surface of our different motors, including mesoporous silica nanomotors, polystyrene and core-shell polystyrene silica micromotors, in order to understand key parameters such as the enzyme coverage, the number of enzymes needed to power motors, or the impact of an asymmetric enzyme distribution to the motion. Moreover, given the applicability of nanomotors in the nanomedicine field, we also provide a study of the interactions between the nanomotors and biological fluids. The motion of the motors was measured with optical tracking software and the distribution of single molecules (urease and other physiologically relevant molecules) around them was observed and quantified using Stochastic Optical Reconstruction Microscopy (STORM). Interestingly, observed asymmetric we an distribution of enzymes around the motors surface regardless of particle composition and size, suggesting the stochastic asymmetric distribution is enough to break force symmetry and produce motion. These results provide deeper knowledge on the fundamental aspects underling enzyme-powered motors and might help to establish more efficient designs for better applicability in the near future.

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## **Figures**



Figure 1. Urease molecules conjugated to the surface of a micromotor viewed with STORM. Scalebar is 2  $\mu m.$ 

# Label-free nanosensing platform for breast cancer exosome profiling

#### A. Marques<sup>1</sup>,

N. Ferreira<sup>1</sup>, R. Martins<sup>1</sup>, C. Bodo<sup>2</sup>, M. G. Sales<sup>3</sup>, B. Costa-Silva<sup>2</sup>, E. Fortunato<sup>1</sup>

 <sup>1</sup>i3N|CENIMAT, Faculdade de Ciências e Tecnologia, Universidade NOVA de Lisboa, Campus de Caparica, 2829-516 Caparica, Portugal
 <sup>2</sup>Champalimaud Research, Champalimaud Centre for the Unknown, 1400-038 Lisbon, Portugal
 <sup>3</sup>BioMark/CEB, ISEP, R. Dr. António Bernardino de Almeida, 431, 4200-072 Porto, Portugal

accm@campus.fct.unl.pt; emf@fct.unl.pt

Cancer constitutes the second leading cause of mortality worldwide, only surpassed bv cardiovascular disease. Based on GLOBOCAN estimates, about 18 million new cancer cases and 9.6 million deaths occurred in 2018 worldwide. Breast cancer is the most frequently diagnosed form of cancer and the leading cause of cancer death among females worldwide. It totalizes 11.6% of the global registered cases in both genders. The diagnosis of breast cancer in the current scenario is made by mammography and its spectroscopy, and breast biopsy test. All these detection techniques are usually expensive, invasive and time-consuming. Thus, the development of simple, reliable, cost effective and non-invasive detection methods for early cancer diagnosis and posterior follow-up is particularly important, due to the disease's prevalence and potential lethality.

Exosomes are small (50-100 nm in diameter) extracellular vesicles secreted by all cells into body fluids such as blood, saliva and urine. These extracellular vesicles show potential for cancer diagnostics, as they transport several molecular contents of the cells from which they originate. Additionally, exosome' analyses are minimally invasive and afford relatively unbiased readouts of the entire tumour burden, less affected by the scarcity of the samples or intra-tumoral heterogeneity. The essential first step of current purification exosome analysis is by ultracentrifugation. Afterwards, exosomes may be western blot, analvsed using enzyme-linked immunosorbent assay, flow cytometry and other analytical methods. Though robust and effective, these strategies are expensive, time-consuming and rely heavily on the sample handling skills. Thus, the development of sensor technologies for rapid, inexpensive, simple and on-site exosome screening is necessary. Some exosomes-based sensors have already been reported, such as label-free exosome assay utilizing transmission surface plasmon resonance (SPR), mass-sensitive sensors aptamerbased sensors magneto-electrochemical sensors, among others. [1,2,3]

Surface Enhanced Raman Spectroscopy (SERS) has emerged as a highly sensitive and rapid analytical technique with wide application regimes, from biological analysis to environmental monitoring. At the most basic level, SERS is a way to significantly increase the signal from the weak yet structurally rich technique of Raman scattering. A SERS-active substrate is generally based on a platform coated with a roughened or nanostructured metallic surface (silver, gold, etc.) that enhances the Raman signal due to the Localized Surface Plasmon Resonance (LSPR). However, the commercially available SERS-active substrates come with a high cost and low shelf-life. Cellulose is the most abundant polymer on earth and meets several interesting properties. Being a biocompatible, biodegradable, flexible, recyclable and low-cost material draws the scientific community attention in several applications, from biosensors to electronics. In this work [4], low-cost SERS-active substrates were produced based on silver nanoparticles (AgNPs) grown in situ into bacterial cellulose (BC) coming from commercial nata de coco, providing a low-cost and simple alternative to the conventional production methods (Figure 1). The AgNPs were grown by hydrothermal synthesis assisted by microwave radiation, that allows well-controlled and fast synthesis. Two routes were followed: one using silver citrate as precursor and another using silver citrate and ammonium citrate dibasic, to induce alkaline environment. A systematic study on the synthesis time and precursor concentration, temperature was performed in order to obtain a good SERS enhancement factor (EF). Ultimately, it was possible to achieve EF from 10<sup>4</sup> to 10<sup>5</sup>, detecting rhodamine 6G (R6G) with concentrations as low as 10<sup>-11</sup> M, which was used as modelmolecule. Finally, biological tests were performed on the optimized SERS substrate, with exosomes samples coming from MCF-10A (non-tumorigenic breast epithelium) and MDA-MB-231 (breast cancer) cell cultures lineages and the obtained SERS spectra were subjected to statistical Principal Component Analysis (PCA), to analyse variances in each collected spectrum and group the similar ones. This analysis tool was chosen since exosomes segregated by the same cell may have different Raman fingerprints: this is probabilistic and is related to the way the exosomes may be positioned in the SERS substrate. Since exosomes have several surface's proteins, different positions of the exosomes in the SERS platform will show different Raman spectra, thus inducing some intra sample variation. So, by combining PCA with Raman intra and inter variability in exosomal samples, it was possible to differentiate tumoral and non-tumoral exosomes, with a data grouping of 95% confidence. The obtained 95% confidence ellipses (Figure 2) are especially useful in this work final objective, since they can be used as a form of diagnostic: if an analysed sample Raman spectrum is located inside any of the presented ellipses, it's safe to assure with 95% confidence that the sample belongs to the

respective group. As a proof-of-concept, a close-to real time diagnosis was performed. For this, tumoral and non-tumoral sample SERS spectra were collected and analysed in the previously obtained score plots. It was registered that both samples fell within the respective ellipses, proving PCA as a valuable diagnosis tool, being able to distinguish between exosomes segregated by tumoral and nontumoral cell lineages trough SERS while using innovative substrates, with an overall cost of 0.39 € per membrane, which can provide several dozens of different measurements. This approach rendered a simple, label-free and easy-to-perform method for exosomes profiling and shows promising results as far as breast cancer diagnostic by SERS is concerned. Moreover, we believe that this novel exosome's profiling method can provide precious information on both the prognosis of the disease and the predictive outcome of a given therapy.

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## **Figures**



**Figure 1.** A: Schematic workflow of the active-SERS substrate's production: from the source (*nata de coco*) to the

final BC/AgNPs platform; B: SEM imaging and AgNP's diameter histogram of the optimized active-SERS platform using BC/AgNPs composites.



**Figure 1.** Schematic representation of the detection system used in this work. Measurement of exosome's samples, spectra data comparison and PCA profiling: PCA resultant score plot using PC1 and PC2 as the analysed principal components: PBS (control) in black, MCF-10A (green) and MDA-MB-231 (red) exosomes sample analysed.

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## SRs and Cd81 Receptors-mediated endocytosis of PMPC-PDPA polymersomes via dynamin IIindependent manner

**Diana Matias**<sup>1</sup>, Loris Rizzello<sup>1,4</sup>, Edoardo Scarpa<sup>1</sup>, Maria Milagros Avila Olias<sup>2</sup>, Virginia Gouveia<sup>1</sup>, Joseph Forth<sup>1</sup>, Irene Canton<sup>2</sup>, Alessandro Poma<sup>1</sup>, Claudia Contini<sup>3</sup>, Giuseppe Battaglia<sup>1,4</sup>

<sup>1.</sup> University College London, Department of Chemistry. 20 Gordon Street, WC1H 0AJ - London (UK);

<sup>2.</sup> The University of Sheffield, Department of Chemistry. Brook Hill S3 7HF - Sheffield (UK);

<sup>3</sup>. Imperial College London, Department of Chemistry. South Kensington Campus SW7 2AZ - London (UK);

<sup>4</sup> Institute for Bioengineering of Catalonia (IBEC), The Barcelona Institute of Science and Technology, Baldiri Reixac 10-12, 08028 Barcelona Spain

d.matias@ucl.ac.uk

#### Abstract

Polymersomes have been revealed to be an ideal tool for the efficient intracellular delivery of a large diversity molecules. However, the molecular pathways regulating polymersomes uptake by cells remain still poorly investigated, especially regarding the role played by surface membrane receptors such as scavenger receptors and tetraspanin family proteins. This subject has crucial implications in biomedical research applied to payload delivery by polymersomes. Here, we investigated the mechanisms involved in polymersomes interaction with specific cell receptors. PMPCx-PDPAy-based self-assembly of polymersomes was carried out the pH-switch method. using After this. polymersomes were purified through a hollow fiber (tangential flow filtration system) followed by stepgradient centrifugation to isolate several subpopulations of particles having homogenous sizes. Polymersomes concentration was quantified by HPLC, while the size characterised by DLS and TEM analysis. The screening of specific receptors guiding the uptake of polymersomes was evaluated by western blot and immunofluorescence. The cytofluorometric method was used to study the kinetics of polymersomes uptake. siRNA and/or shRNA was used to knockdown the expression of endocytosis proteins and manipulate the uptake of polymersomes by carcinoma cells. The results showed that changes in the polymer lengths of PMPC affected the rate of vesicles uptake.

Moreover, we deciphered an essential correlation between the degree of polymerisation(i.e., the polymer lengths) and the kinetics of polymersomes uptake. We confirmed a key role played in PMPC25-PDPA70 polymersomes uptake by scavenger receptors (SRBI and CD36) and CD81 receptor in cancer cells. Silencing of SR-BI gene using siRNA in FaDu cells decreased PMPC-PDPA polymersomes uptake by 50% in a dynamin-independent manner. Here, we highlighted the dynamics of interaction between polymersomes and plasma membrane receptors, SRs and CD81. We have shown that polymersomes uptake guidance is dynamin-IIindependent.

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**Figure 1.** The SR-BI/CD36 and the tetraspanin CD81 are natural receptors for cellular uptake of PMPC<sub>25</sub>-PDPA<sub>70</sub> polymersomes via dynamin-II independent manner.

# Novel 3d Printed Capacity and pH Buffer Sensor

#### Pouya Mehdrel <sup>1</sup>, Josep Farré-Lladós, Jasmina Casals-Terré<sup>1</sup>

<sup>1</sup>Universitat Politècnica de Catalunya, C/ Colom 7-11,

Terrassa, Spain

Jasmina.casals@upc.edu

#### Abstract

This work presents a novel 3D-printed micromixer capable to not only measure pH also molarity of the buffer. Buffer molarity control is especially sensitive in biological processes[1]. The design takes advantage of the diffusion of the solutions (buffers) and analyzes interaction area and the color change experienced by bromocresol purple (pH indicator). The performance of the proposed solution was evaluated in three different buffer molarities (0.1, 0.5 and 1.0 M ) with three different pH values (6.0, 7.0 and 8.0). The microfluidic channel was designed for a Reynolds number of 1, therefore the diffusion was occurring progressively from the inlet to the outlet. Molarity measurements were done at the intersection of the inlets, while pH measurement (that required complete mixture) was done at the outlet. The results showed that not only the current setup is successful at measuring the buffer molarity and pH, but also the fabrication method is more rapid and flexible in creating microfluidic devices.

#### Methodology

The microfluidic device shown in Figure 1 (a) and (b) was manufactured using a 3d printer based on Digital Light Projection Technique (DLP) [1]. Briefly, the geometry from Figure 1 is modeled in 3D using @Solidworks software and exported to \*.slt format to be introduced to the @MiiCraft Plus printer. The channel's height is also set to 500  $\mu$ m and the top layer to 300  $\mu$ m to ensure that the channel is fully sealed and the chip is printed uniformly. The pH indicator is Bromocresol purple (5',5"-dibromo-o-cresolsulfophthalein), @sigma Aldrich. (4-(2-hydroxyethyl)-1-pi-perazineethanesulfonic acid) HEPES, from @Sigma Aldrich, was used as buffer at different molarities and pH [28].

During the assay the main channel injects the Bromocresol and the buffers are injected into the device, through lateral channels. The injection is done by another syringe pumps (kdScientific 410-CE- @kdScientific, Holliston, MA, US).

#### Conclusions

According to the results, the DLP 3D printed microfluidic mixers can be employed as a flexible process to manufacture pH and molarity buffer The use of 3D printed microfluidics sensor. provides portability to pH measures and the opportunity to control the buffer capacity measuring its molarity/concentration. In the current study HEPES buffer of 3 different concentrations were evaluated showing clearly that BCP advanced further into the lateral channels when the concentration was increasing. In the same magnification scale, BCP penetrated up to 39 pixels in buffers with 0.1 M of HEPES, see Figure 2. Whereas, the indicator marked a 147 pixels advance for the buffers with 1.0 M of HEPES, showing a 2.77 times increase in the diffusion width, while the inlets' discharges were kept constant. Besides, pH measurement, which required a homogeneous mixing, was achieved as well at the outlet of the mixer, See FIGURE 3. This study showed that the 3D printed device could be successfully employed in order to detect buffers in the pH range of 6.0 up to 8.0 as the investigation showed a 21.7% mean blue color difference between buffers with pH 6.0 and 7.0. Although, a 11.2% difference between the buffers with pH 7.0 and 8.0 was reported, but the analysis showed a 35.3% change when buffers with pH 8.0 and 6.0 were compared. Furthermore, the assay showed that the setup could be used as a selfreferencing sensor, when two unknown solutions are being injected into the lateral channels. The results showed that, not only the 3D printed device reproduced the numerically predicted trend, but also it provided 76.3% of homogeneity, which is only 1.3% off the numerically predicted efficiency.

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#### **Figures**



inlet 2

Figure 1. a) shows a 3D view of the investigated device, inlets and measurement zones. i) illustrates the buffer measurement zone and ii) displays the pH measurement zone. b) Inlets, outlet and the channel of the 3D printed device is shown. c) Displays the diffusion phenomena at the intersection of the inlets. The evaluation line, where the buffer diffusion is measured over, is also displayed. d) Shows the numerical simulation of diffusion in one loop mixer with 10% expansion parts, assuming that 0.05 M of a specie is injected into a device while the fluids flow at Re=1.0.



Figure 2. displays the length of reaction at pH 8.0. This level is beyond BCP's capacity to demonstrate the alkalinity of buffers and the color change and reaction lengths are at their maximum. Reactions of BCP and buffers with 0.1, 0.5 and 1.0 M of HEPES are represented in pictures (a), (b) and (c), respectively. Lateral (a), (b) (c) shows the reaction of BCP and buffers with different pH levels at the intersection of the inlets. The upper inlet was dedicated to the buffers with pH 8.0 and through the bottom inlet, the buffer with pH 6.0 was injected. Pictures (a), (b) and (c) show the reaction of buffers with 0.1, 0.5 and 1.0 M of HEPES, respectively.



Figure 3. shows the analysis of the mixture of the BCP and the buffers at the outlet. The transition of color in the range of pH 6.0 to 7.0 is quite obvious, but for the range of pH 7.0 to 8.0 further investigation and accurate measurements are necessary. Pictures (a), (b) and (c) show the final mixture of the BCP and buffers with 0.5 M of HEPES at pH 6.0, 7.0 and 8.0, respectively

Modification of the magnesium corrosion rate in physiological saline 0.9 wt % NaCl via chemical and electrochemical coating of reduced graphene oxide

#### J.M. Molina<sup>1</sup>,

J. Fernández<sup>2</sup>, Y. El Ouardi<sup>2</sup>, J. Bonastre<sup>2</sup>, F. Cases<sup>2</sup>

<sup>1</sup>Departamento de Química Inorgánica de la Universidad de Alicante e Instituto Universitario de Materiales de Alicante, University of Alicante, Ap 99, E-03080 Alicante, Spain

<sup>2</sup>Departamento de Ingeniería Textil y Papelera, Escuela Politécnica Superior de Alcoy, Universitat Politècnica de València, Plaza Ferrándiz y Carbonell, s/n, 03801 Alcoy, Spain

> <sup>1</sup>(J.M. Molina) jmmj@ua.es; <sup>2</sup>(F. Cases) fjcases@txp.upv.es

Abstract (Arial 10)

Different metallic materials have been used as biomaterials for the manufacture of medical implants. Commonly used metallic biomaterials include stainless steel, pure titanium, titaniumaluminum-vanadium-based alloys and cobaltchromium-molybdenum-based alloys [1-5]. The advantages of biodegradable Mg-based implants [6-8] lie in their mechanical and electrochemical properties. Mg is a lightweight metal with a density of 1.74 g cm -3 versus 7.9 g cm -3 for Al and 4.5 g cm -3 for Ti. Moreover, Mg presents an elastic modulus and compressive yield strength closer to those of natural bone [9]. In addition, Mg is a biocompatible material naturally found in the human body (approximately half of the total physiological Mg is stored in the bone tissue) [10]. Setbacks when using Mg as metallic material for biomedical applications are related to its low corrosion resistance under the physiological conditions [9] and the excessively rapid production of hydrogen gas during the in-vivo corrosion [11]. The first issue could lead to both a rapid loss of its mechanical problems properties and severe in tissue regeneration, and the second, to harmful effects during the tissue healing process. One of the most recent studies dedicated to slowing down the dissolution of magnesium in saline conditions was performed on samples of magnesium foam manufactured using the replication method from carbon spheres as a template. The heat treatment in air flow at 540 °C applied to burn the template particles generated a layer of oxide on the surface of the foam which notably slowed down its dissolution at 37 °C in an aqueous solution containing 3 wt % NaCl that had a pH of 7.4 (a pH closed to that of the

human body) [12]. Other surface modifications that were proved to be successful in slowing the corrosion rate of magnesium were fluoride conversion coatings, phosphate treatments or chemical deposition of hydroxyapatite and octacalcium phosphate [13].

Moreover, it has been proved that both graphene oxide (GO) and reduced graphene oxide (RGO) show anti-corrosion properties when coated onto metal substrates [14–19]. The syntheses of the different graphene-metallic substrate specimens were carried out following both electrochemical [20– 22] and chemical [23,24] methods.

The synthesis of reduced graphene oxide onto magnesium discs by electrochemical and chemical methods is presented in this work. The surface morphology and atomic composition were investigated using field emission scanning electron microscopy and dispersive energy X-ray spectroscopy. The corrosion rate of different samples was analyzed in physiological saline 0.9 wt % NaCl solution by potentiodynamic polarization, electrochemical impedance spectroscopy and scanning electrochemical microscopy. As a result of the different treatments, a progressive decrease in the corrosion rate of the magnesium disc in the corroding environment was obtained, reaching up to 80% of reduction for the chemically modified sample.

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## Development and permeability evaluation through BBB-on-achip model of Gold nanorods with therapeutic potential for Alzheimer's disease

#### Sujey Palma-Florez<sup>1</sup>,

Dr. Francisco Morales-Zavala<sup>4,5</sup>, Dr. Anna Lagunas<sup>2,1</sup>, Dr. Mónica Mir<sup>2,1,3</sup>, Prof. Marcelo Kogan<sup>4,5</sup>, Prof. Josep Samitier<sup>2,1,3</sup>

<sup>1</sup> Nanobioengineering group, Institute for Bioengineering of Catalonia (IBEC) Barcelona Institute of Science and Technology (BIST), 12 Baldiri Reixac 15-21, Barcelona 08028, Spain.

<sup>2</sup> Networking Biomedical Research Center in Bioengineering, Biomaterials and Nanomedicine (CIBER-BBN), Madrid, Spain.

 <sup>3</sup> Department of Electronics, University of Barcelona, Martí i Franquès 1, 08028 Barcelona, Spain.
 <sup>4</sup> Nanobiotechnology group, Faculty of Chemistry and Pharmaceutical Sciences, University of Chile, Santos Dumont 964, 8380494, Santiago, Chile.
 <sup>5</sup> Advanced Center for Chronic Diseases (ACCDiS), Sergio Livingstone 1007, Santiago, Chile.

#### spalma@ibecbarcelona.eu

Alzheimer's disease (AD) is а chronic neurodegenerative disorder characterized by a progressive loss of cognitive capacity and memory. AD is mainly associated to two neuropathological processes: hyperphosphorylation of tau protein (Ptau) and the accumulation of toxic aggregates of amyloid  $\beta$  peptide (A $\beta$ ) in the brain. In pathological conditions, AB peptide is synthetized from a transmembrane protein (APP) which is cleavage by the beta and gamma secretase enzymes [1]. Then, the Aβ peptide is aggregated in oligomeric species, fibers and amyloid plaques which produce oxidative stress and neurotoxicity [2].

In the last years, multiple efforts have been performed in order to develop new molecules for AD's treatment based on the disaggregation of AB cumulates [1]. However, most of them do not reach the action site due the strict permeability in the brain by the blood brain barrier (BBB). By the way, nanotechnology is an attractive field that offers several alternatives for the treatment and diagnosis of AD. Specifically, a previous work reported gold nanorods (GNRs) functionalized with polyethylene glycol (PEG), a peptide that acts as a  $\beta$  sheet breaker (D1 peptide) and other one to allow the shuttling through the BBB (Angiopep-2) by LRP1 receptor present in the brain endothelium. The results revealed that the nanosystem (GNRs-PEG-Ang2/D1) performed A $\beta$  growth inhibition *in vitro*. Remarkably, this effect was enhanced by irradiation due GNRs present photothermal properties. In addition, the nanosystem decreased the toxicity of Aß aggregates in a Caenorhabditis elegans in vivo model [2].

Therefore, promising therapy/diagnostic agents are being developed and need to be evaluated quickly and easily for the early provision of new alternatives for AD. BBB-on-a-chip is an interesting alternative due their versatile, controlled, repeatable and lower cost design to mimic both *in vivo* physiological and pathological conditions for the study of drug permeability, disease progression, efficacy of treatment and others [3].

In the present work, we proposed the development of GNRs-PEG-Ang2/D1 and evaluate its permeability in a BBB-on-a-chip model which allows a 3D arrangement closer to the biological structure and tuning different flow conditions.

For this, we synthetized GNRs by a seed-mediated growth method and then were conjugated with PEG, Angiopep-2 and D1. These nanosystems were characterized by dynamic light scattering (DLS), zeta potential, electron microscopy (TEM) and UV-Vis-NIR spectroscopy. On the other hand, for the construction of the BBB-on-a-chip we will use brain endothelial cells and pericytes; therefore, the cytotoxicity of the nanosystems was determined by Annexin V/DAPI assay. Then, we expect to assess the cell uptake by flow cytometry. Finally, we will evaluate the permeability of the GNRs at different conditions in BBB-on-a-chip by atomic flow absorption and Nano tracking analysis (NTA). Also, the integrity of the BBB after GNRs administration will be assessed by immunofluorescence and transendothelial electric resistance (TEER).

From UV-vis-NIR spectroscopy of GNRs and its conjugates showed two absorption peaks about 520 and 710nm, directly regarding to this type of nanoparticles. Also, DLS and zeta potential revealed that the GNRs surface functionalization caused an increase in the hydrodynamic diameter and electrostatic change from positive to negative charge (+40 to -5 mV). Finally, electron microscopy displayed the shape and size of GNRs of length 40nm and 10nm width. On the other hand, these nanosystems did not show cytotoxic effects over endothelial cells and pericytes between 0.05 to 0.4nM for 24 hours.

We conclude that obtained GNRs-PEG-Ang2/D1 in a reproducible manner and they were not toxic for the endothelial and pericytes cells for BBB-on-achip. In future, we will evaluate the permeability of the GNRs at different flow conditions in BBB-on-achip and the integrity of the barrier after GNRs exposure.

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## **Figures**



Figure 1. Electron micrograph of GNRs-PEG-Ang2/D1.

## BBB-targeting liposomes : Design, characterization and *in vivo* evaluation

Panagiota Papadopoulou<sup>1</sup>, Gabriela Arias-Alpizar<sup>1</sup>, Mohammad Moradi<sup>3</sup>, Jeroen Bussmann<sup>2</sup>, Nico A.J. M. Sommerdijk<sup>3</sup>, Frederick Campbell<sup>1</sup>, Alexander Kros <sup>1</sup>

<sup>1</sup>Department of Supramolecular & Biomaterials Chemistry, Leiden Institute of Chemistry, Leiden University, The Netherlands.

<sup>2</sup> Department of Biotherapeutics, Leiden Academic Center for Drug Research (LACDR), Leiden University, The Netherlands.

<sup>3</sup>Materials and Interface Chemistry & Centre for Multiscale Electron Microscopy, Department of Chemical Engineering and Chemistry, TU Eindhoven University, Eindhoven, The Netherlands.

p.papadopoulou@lic.leidenuniv.nl

The blood-brain-barrier (BBB) remains a formidable obstacle for the treatment of brain diseases. Current technologies, characterized by high complexity, rarely achieve delivery of the drug in the brain beyond 1% of the total injected dose [1] and therefore prognoses for brain diseases remain extremely poor.

By using embryonic zebrafish (Danio Rerio) as a model to assess nanoparticle behavior in vivo [2], we report a simple liposome formulation composed of just two lipids, with a significant specificity for the brain endothelium. We demonstrate how the highly unusual morphology of these liposomes, characterized by phase-separation and a single protrusion per liposome, is essential for BBB targeting, as well as our current understanding of the mechanism behind this biological response. Finally, we show the incorporation of a pH sensitive lipid-dye and of a single gold nanoparticle per liposome, which enables the elucidation of the liposome fate using high-resolution imaging techniques.

Ultimately, the unprecedented specificity of this liposomal formulation for brain endothelial cells and our comprehension of its *in vivo* mechanistic behavior, may lead to the development of a novel powerful tool for drug delivery to the CNS.

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### **Figures**



**Figure 1.** 10x fluorescent images of the embryonic zebrafish head (dorsal view), following intravenous administration of BBB-targeting liposomes and control liposomes (liposomes in magenta (left) or white (right)). Arrow indicates the specificity of the liposomes for the BBB, as targeting starts where the brain endothelium begins. Zebrafish embryo is at 3 days post fertilization (3dpf), expressing green fluorescent protein throughout its vasculature (kdrl:GFP).

## Affinity-Targeted Silver Nanoparticles as a Research Tool and a Drug Carrier

#### A. Tobi<sup>1</sup>,

A. M. A. Willmore<sup>1</sup>, K. Kilk<sup>2</sup>, G. B. Braun<sup>3</sup>, U. Soomets<sup>2</sup>, K. N. Sugahara<sup>4</sup>, E. Ruoslahti<sup>3,5</sup>, T. Teesalu<sup>1,3,5</sup>

<sup>1</sup>Laboratory of Cancer Biology, Institute of Biomedicine and Translational Medicine, University of Tartu, Ravila 14b, 50411 Tartu, Estonia.

<sup>2</sup>Department of Biochemistry, Institute of Biomedicine and Translational Medicine, University of Tartu, Ravila 14b, 50411 Tartu, Estonia.

<sup>3</sup>Cancer Research Center, Sanford-Burnham-Prebys Medical Discovery Institute, 10901 North Torrey Pines Road, La Jolla, 92037 California, USA.

<sup>4</sup>Department of Surgery, Columbia University College of Physicians and Surgeons, New York, New York, USA. <sup>5</sup>Center for Nanomedicine and Department of Cell, Molecular and Developmental Biology, University of California, Santa Barbara Santa Barbara, 93106 California, USA.

#### allan.tobi@ut.ee

#### ABSTRACT

We have developed silver nanoparticles (AgNPs) as a model carrier system to study tumor homing peptide-mediated targeting and cellular/tissue interactions of AgNPs in vitro and in vivo. AgNPs loaded with fluorescent dyes can be tracked in cells and tissues by ultrasensitive optical imaging, as the silver cores of the AgNPs plasmonically enhance the fluorescent signal [1]. To allow quantitative internally-controlled cellular uptake and tissue biodistribution studies using AgNPs, we have developed isotopically barcoded AgNPs and optimized their detection by inductively coupled plasma mass spectrometry (ICP-MS) and laser ablation ICP-MS. This approach allows ultrasensitive parallel auditioning of peptide-guided and control AgNPs in the same biological test systems [2,3]. Furthermore, peptide-targeted AgNPs can serve as a carrier for cytotoxic payloads to receptor-positive cancer cells [4].

In addition to the synthesis and characterization of the nanoparticles, we show that AgNPs loaded with a potent anticancer drug, monomethyl auristatin E (MMAE), and targeted with Neuropilin-1-targeting Cend Rule peptide, RPARPAR, accumulate in prostate cancer cells overexpressing the receptor protein and cause selective toxicity in these cells through the release of MMAE by lysosomal cathepsin B (Figure 1). Importantly, the specific cytotoxic activity of RPARPAR-MMAE-AgNPs (vs. non-targeted MMAE-AgNPs) can be potentiated by dissolution of the extracellular nanoparticles with a biocompatible etching solution [1]. mild We demonstrated that the binding and subsequent internalization is Neuropilin-1-dependent (Figure 2),

and quantified the uptake of MMAE, which was delivered to cells on AgNPs, by HPLC-MS. RPARPAR-MMAE-AgNPs were also tested in a mixed culture of target and control cells, where specific elimination of target cancer cells was clearly evident. Several assays were used to evaluate the cytotoxicity of these nanoparticles.

These studies suggest that the AgNP platform can be used for quantitative nanoparticle biodistribution studies and as an anticancer drug carrier *in vitro*, and that elimination of extracellular AgNPs by exposure to etching solution can be used as an endocytosis research tool and as a means to improve the therapeutic index of AgNPs loaded with anticancer payloads. Validation of peptide-targeted MMAE-AgNPs as an effective drug carrier *in vivo* are currently under way.

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**Figure 1.** CendR peptide guided conditional therapeutic AgNPs. [1] RPARPAR-MMAE-AgNPs bind to the b1b2 binding pocket of NRP-1 on the surface of cells. [2] Binding to NRP-1 initiates cellular uptake of particles in the endolysosomal compartment. [3] Intracellular RPARPAR-MMAE-AgNPs are processed by cathepsin B (Cat B) at Val-Cit bond on the linker incorporated into the cytotoxic MMAE (red stars) to release the active MMAE in the cytosol where it binds to tubulin and prevents cell division, eventually causing cell death. [4] The extracellular fraction of the AgNPs can be removed by a mild biocompatible etching solution consisting of hexacyanoferrate and thiosulfate.



Figure 2. Neuropilin-1-dependent binding and RPARPAR-MMAE-AgNPs. internalization of (A) RPARPAR-MMAE-AgNPs bind to the b1b2 domain of NRP-1. Recombinant wild type (wt) and mutant (mut) b1b2 domains of Neuropilin-1 (NRP-1) with a 6xHis-tag were coupled to Ni-NTA magnetic agarose beads. After 1 h incubation with AgNPs (1.5 nM) at 37 °C the unbound AgNPs were removed by washing, bound AgNPs in complex with NRP-1 were released from the beads with imidazole, and absorbance of the eluate in the UV-Vis range was measured. (B) RPARPAR functionalization renders AgNPs and MMAE-AgNPs selective for NRP-1 binding. Cells in suspension were incubated with 1.5 nM AgNPs at 37 °C for 1 h, washed, and resuspended in PBS for flow cytometry to measure AgNP uptake in the cells. Representative data are shown (n = 3). See Fig. S1 for data on the NRP-1 negative control cell line. (C) Representative dark-field image (with DAPI overlay) showing internalization of RPARPAR-MMAE-AgNPs in PPC-1 cells. Attached PPC-1 cells were incubated with 1.5 nM RPARPAR-MMAE-AgNPs (green) at 37 °C for 1 h. Extracellular AgNPs were removed by exposure to 10 mM etchant for 5 min. The cells were fixed with -20 °C MeOH, counterstained with DAPI (1  $\mu\text{g/ml};$  blue), and imaged using an inverted microscope. The image is a composite of dark-field and DAPI images; dotted lines outline the cells, arrows point to internalized AgNPs; scale bar: 20 µm. (D) NRP-1-dependent internalization of RPARPAR-MMAE-AgNPs by PPC-1 cells. PPC-1 cells in suspension were incubated with 1.5 nM AgNPs at 37 °C for 1 h, washed, and analysed by flow cytometry. Optional incubation with etchant prior to flow cytometry for 5 min was used to remove extracellular surface-bound AgNPs. To study the role of the NRP-1 in the cellular interaction of particles, the cells were incubated with 10 µg/mL functionblocking polyclonal rabbit α-NRP-1 antibody at 37 °C for 15 min prior to incubation with AgNPs. Representative data are shown (n = 3).

# Controlling self-assembling and tumor cell-targeting of protein-only nanoparticles through modular protein engineering

**Eric Voltà-Durán**<sup>1,2,3</sup>, Olivia Cano-Garrido<sup>1,4</sup>, Naroa Serna<sup>1,2,3</sup>, Hèctor López-Laguna<sup>1,2,3</sup>, Laura Sánchez-García<sup>1,2,3</sup>, Mireia Pesarrodona<sup>1,2,3#</sup>, Alejandro Sánchez-Chardi<sup>5</sup>, Ramón Mangues<sup>6</sup>, Antonio Villaverde<sup>1,2,3</sup>, Esther Vázquez<sup>1,2,3</sup>, Ugutz Unzueta<sup>3,5</sup>

<sup>1</sup> Institut de Biotecnologia i de Biomedicina, Universitat Autònoma de Barcelona, Bellaterra, 08193 Barcelona, Spain

<sup>2</sup> Departament de Genètica i de Microbiologia, Universitat Autònoma de Barcelona, Bellaterra, 08193 Barcelona, Spain

<sup>3</sup> CIBER de Bioingeniería, Biomateriales y Nanomedicina (CIBER-BBN), C/Monforte de Lemos 3-5, 28029 Madrid, Spain

<sup>4</sup> Nanoligent SL, Edifici EUREKA, Universitat Autonoma de Barcelona, Bellaterra, 08193 Barcelona, Spain

<sup>5</sup> Departament de Biologia Evolutiva, Ecologia i Ciències Ambientals, Facultat de Biologia, Universitat de Barcelona, Av. Diagonal 643, 08028 Barcelona, Spain <sup>6</sup> Institut d'Investigacions Biomèdiques Sant Pau and Josep Carreras Research Institute, Hospital de la Santa Creu i Sant Pau, 08041 Barcelona, Spain

# Present address: Institute for Research in Biomedicine (IRB Barcelona), The Barcelona Institute of Science and Technology, 08028 Barcelona, Spain

eric.voltaduran@gmail.com

#### Abstract [1]

The use of proteins as drug delivery systems is gaining interest in nanomedicine, especially when dealing with targeted therapies which require specific interaction and penetration into target cells [2]. By genetic fusion, proteins with multiple biological activities can be synthetized as singlechain polypeptides. This way, just a unique step of recombinant production is needed to obtain the final modular protein, in which each domain plays a determinant and distinct role [3]. In this context, the combination of both cationic peptides and polyhistidines into a protein structure has been proven as a universal self-assembling protein platform [4]. The paradigmatic example of this is the modular protein T22-GFP-H6, in which the combination of T22 (a potent ligand of the tumoral marker CXCR4) and H6 promote the formation of protein-only nanostructures around 11 nm (above renal filtration cut-off) which selectively bind and internalize CXCR4+ tumor cells in vitro and in vivo [5]. This makes T22-GFP-H6 and its related fusions

appealing vehicles for selective drug delivery. In here, we study the relevance of T22 and H6 positioning inside the modular structure by performing а morphological and functional characterization of alternative fusion proteins in which T22 and H6 have been rearranged in different locations (Figure 1). The results show that swapping modules crucially impacts on protein functionalities. For instance, we prove that positioning T22 at the amino terminus and H6 at the carboxy terminus is crucial for promoting protein self-assembly as oligomers (ten protein units each nanoparticle), whereas the alternative dispositions result in hydrodynamic sizes compatible with those from GFP monomers or dimers. Moreover, T22 must be placed in the amino terminus for allowing CXCR4+ cell binding and specific internalization. Besides this, it has been demonstrated that the ability to oligomerize as regular protein nanoparticles increases cell penetrability in a cooperative way. When T22 is located at the N-terminus, proteins (irrespectively of being assembled as oligomers or not) enter CXCR4<sup>+</sup> cells by endocytosis, showing a punctuated pattern of fluorescence with perinuclear distribution in confocal images (Figure 2). In contrast, when T22 is located in the C-terminus, proteins tend to accumulate in CXCR4+ cell membranes, lacking the ability to internalize them (Figure 2). Taken together, all these data teaches how to design smart multifunctional protein nanocarriers with feasible applications in targeted drug delivery, not simply for the treatment of human cancers but also for the CXCR4<sup>+</sup> development of pharmaceuticals against other diseases in which CXCR4 is a relevant homing marker, such as HIV.

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## **Figures**



**Figure 1.** Modular proteins with alternative arrangements of T22, GFP and H6. Each module owns two key functions in protein functionality.



**Figure 2.** Intracellular location of proteins in protein-exposed cells. Red signal indicates labelled membranes, blue signal labelled nuclear nucleic acids and green signal is the natural green fluorescence of proteins. 2D confocal images and 3D reconstructions. Bars indicate 10<sup>4</sup> nm. Reprinted by permission from Springer Nature Customer Service Centre GmbH: Springer Nature, Science China Materials, Voltà-Durán E, Cano-Garrido O, Serna N et al. Controlling self-assembling and tumor cell-targeting through modular protein engineering (2019), https://doi.org/10.1007/s40843-019-9582-9 ©.



Calle Alfonso Gomez 17 Planta 2 - Loft 16 28037 Madrid (Spain)

info@phantomsnet.net www.phantomsnet.net

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